

Introduction to fMRI

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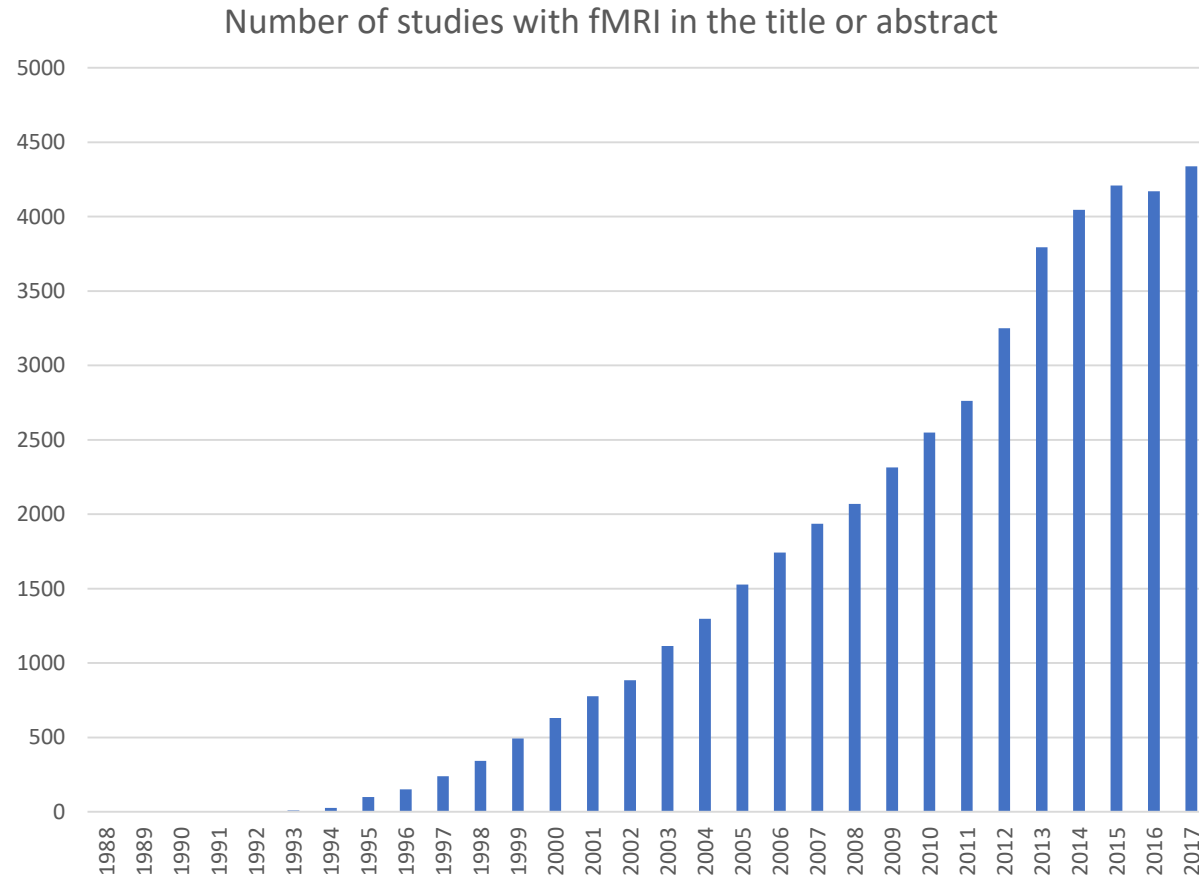


fMRI outline

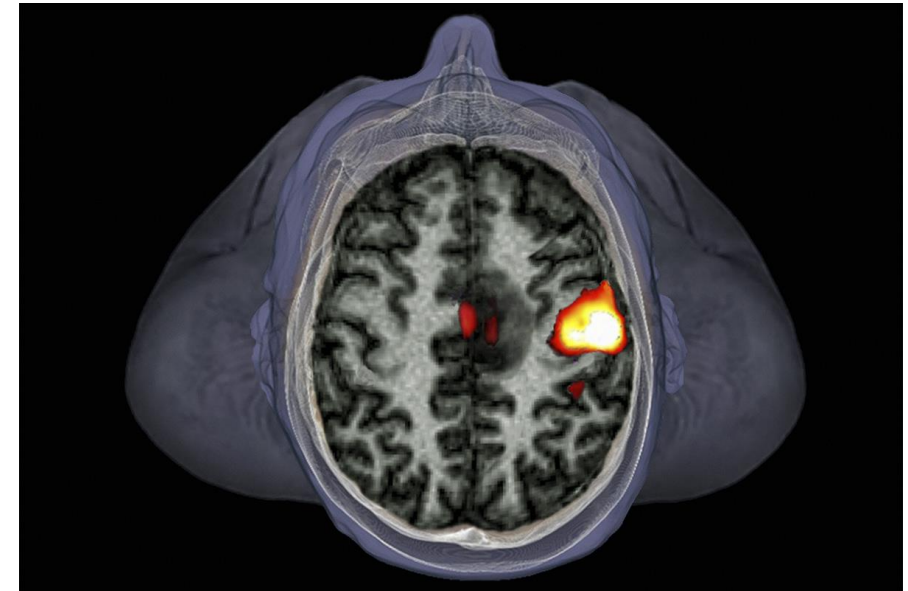
- Advantages
- MRI vs. fMRI
- Basic neurophysiology
- fMRI experiment
- Analysis steps
- Connectivity
- Limitations



Why is it so cool?



Source: PubMed search

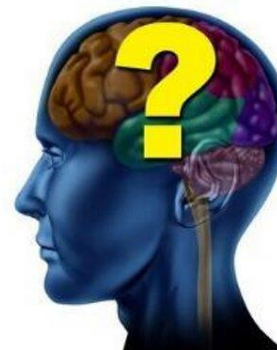
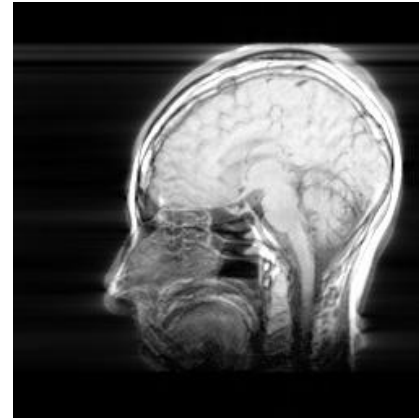


Zephyr/Science Photo Library

- Noninvasive and doesn't involve radiation
- Excellent spatial and good temporal resolution
- Tool for imaging entire network of brain regions engaged when performing particular tasks (cognitive/affective/motor functions)
- Broad application

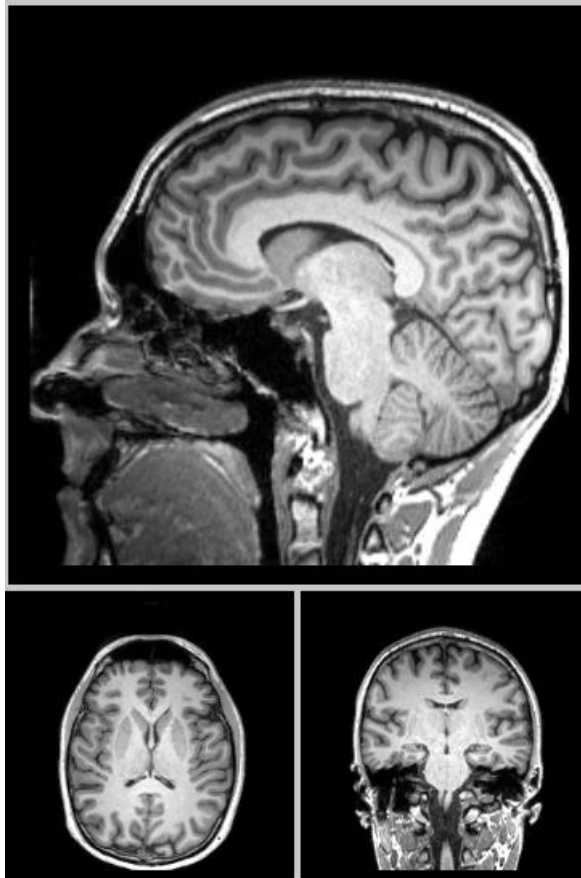
Why it is not so cool?

- Contraindications
- Motion artefacts
- Expensive
- Surrogate signal - indirect measurement of neuronal activity – hard to interpret

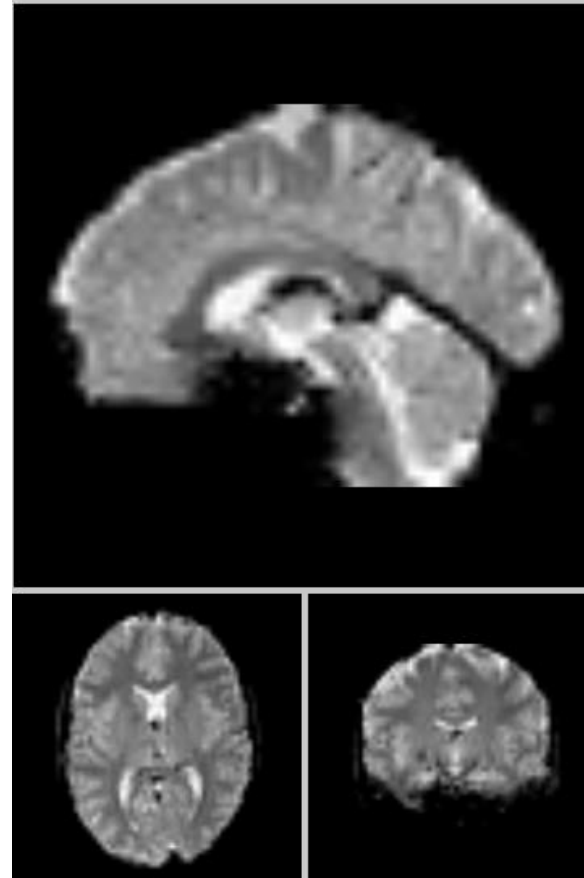


MRI vs. fMRI

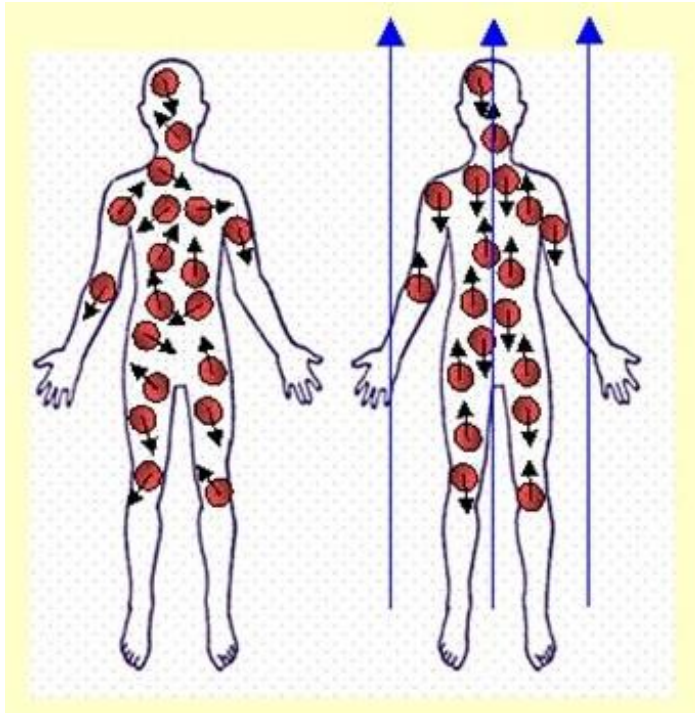
- Anatomic structure
- High resolution (1 mm)
- One image (volume)



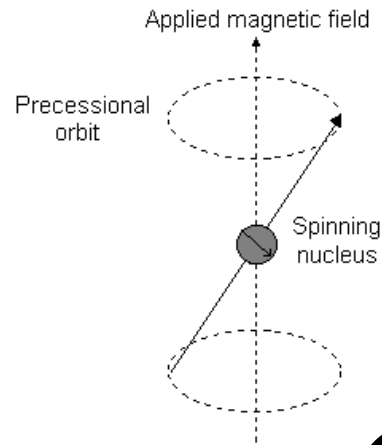
- function
- Low resolution (3 mm)
- Number of images (volumes) in succession



(N)MRI principle in a nutshell



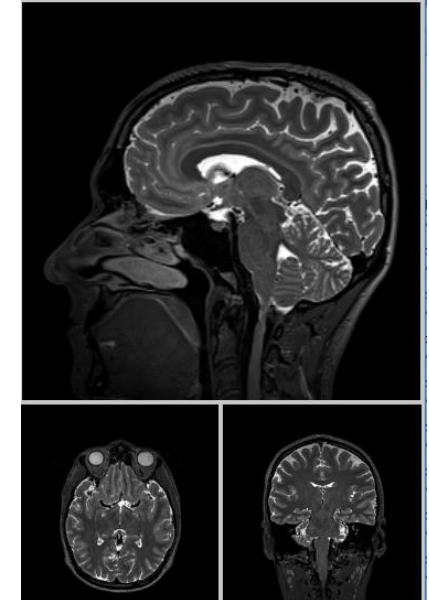
Hydrogen nucleus



T1



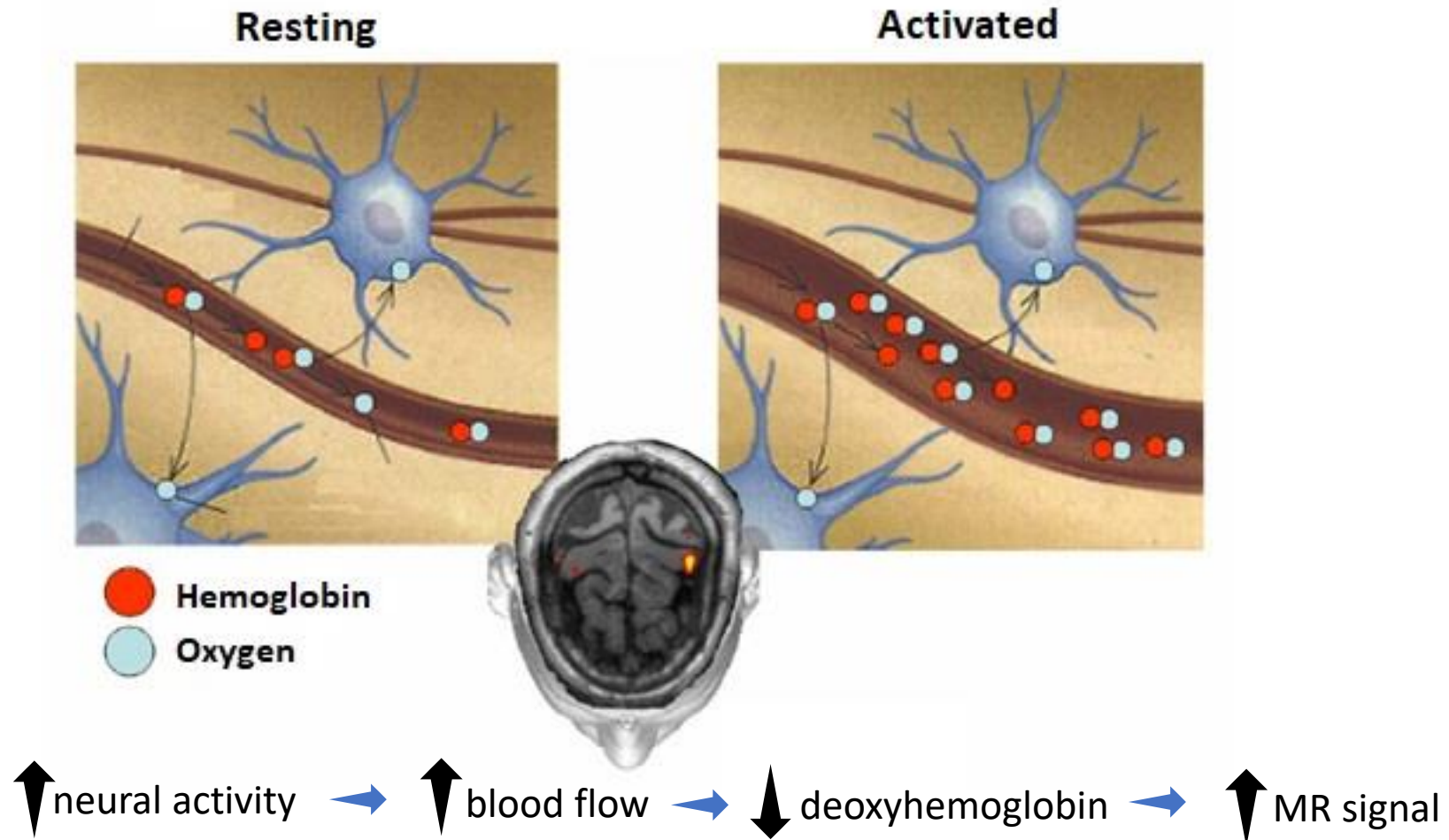
T2



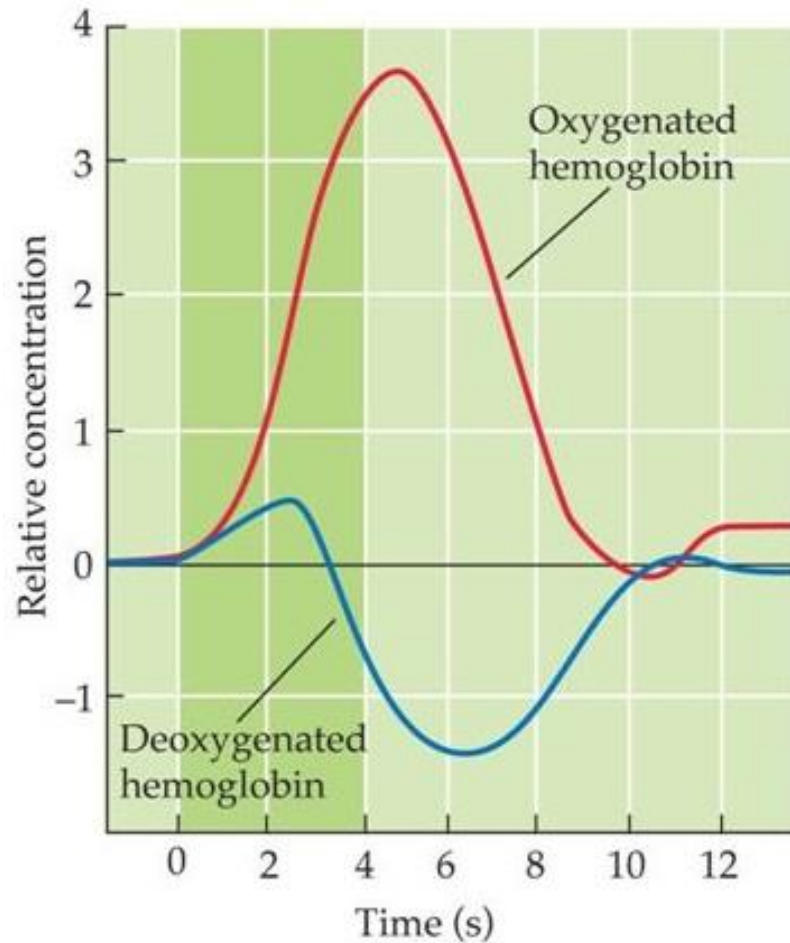
1. Hydrogen nuclei (protons) are aligned by a strong magnetic field
2. Protons can be rotated using radio waves
3. Protons oscillate while returning to equilibrium
4. During realignment the nuclei lose energy and a measurable radio frequency (RF) signal
5. Detected signal is used for detailed images of body tissues

fMRI principle

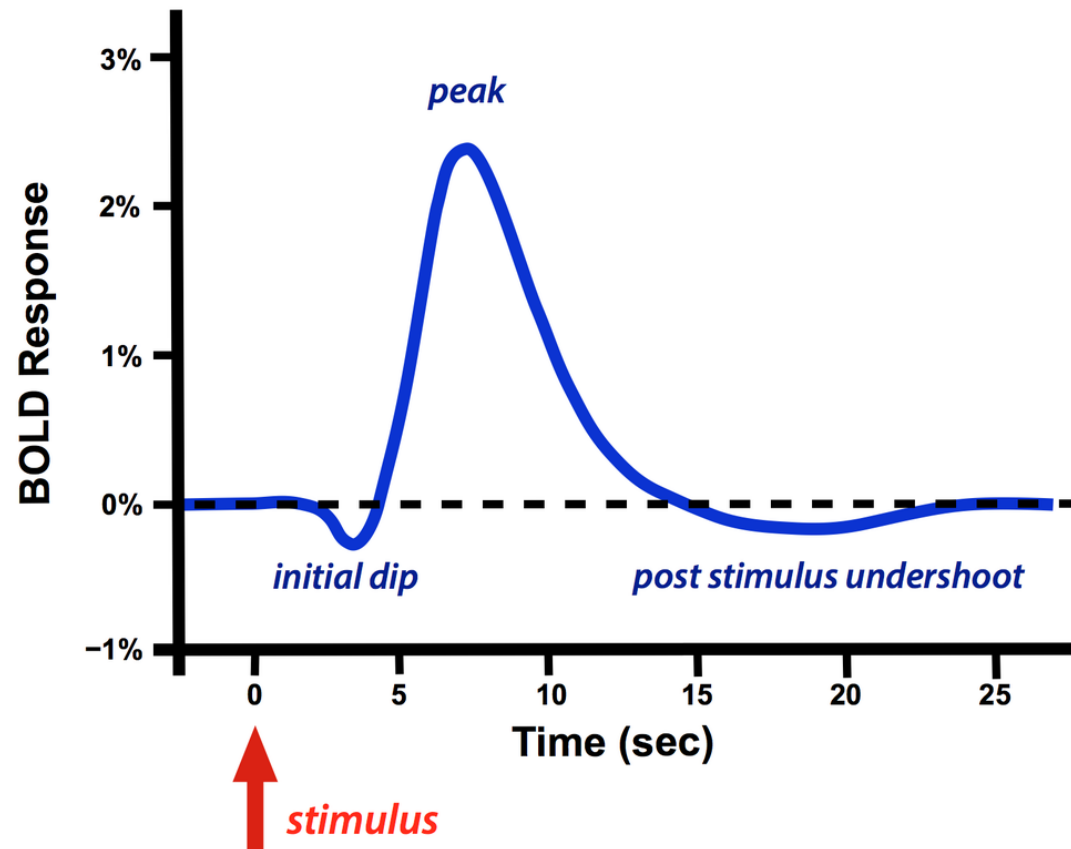
Blood **O**xxygen **L**evel **D**ependent - **BOLD** signal



Hemodynamic Response Function (HRF)



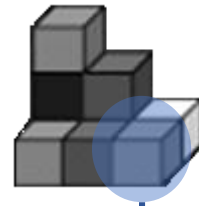
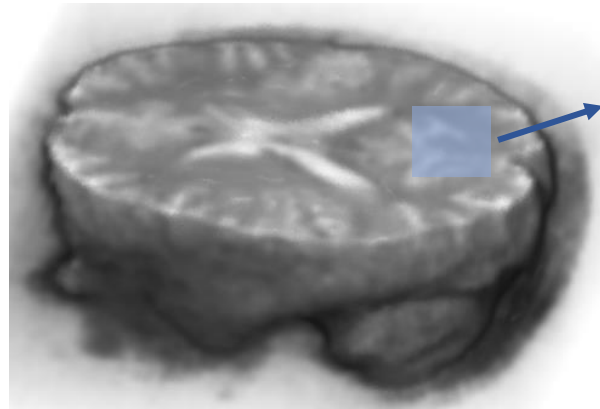
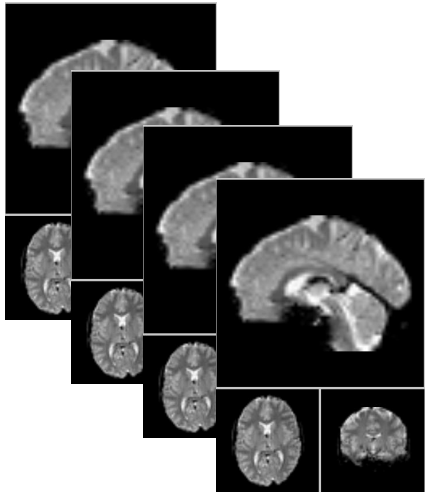
(Malonek and Grinvald, 1996)



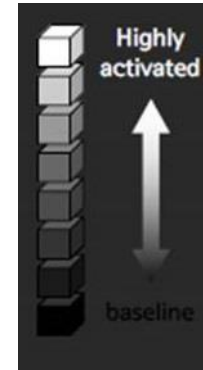
<http://mriquestions.com>

fMRI raw data

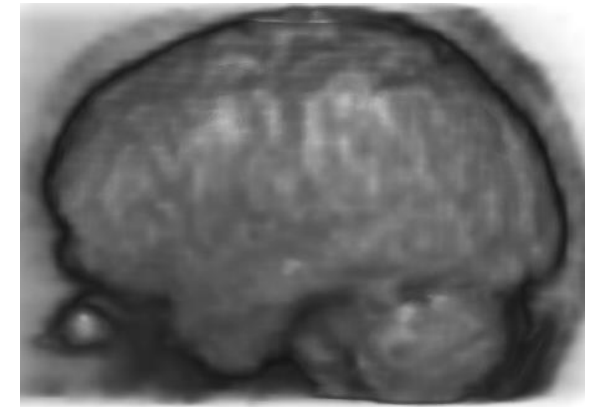
Slices (2D)



One voxel

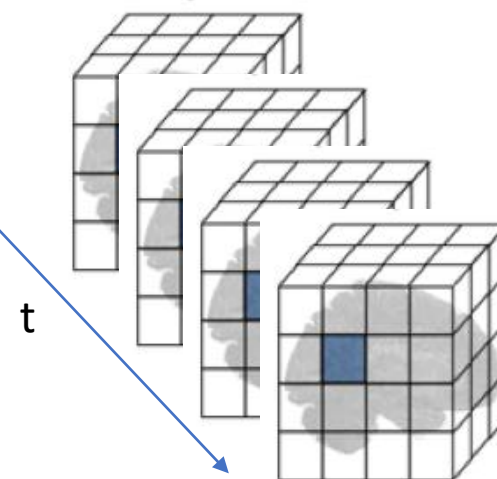
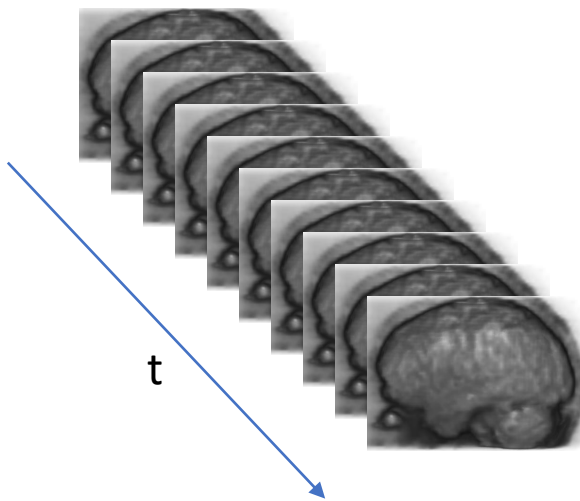


Volume (3D)



Acquisition time 1,5-3 s

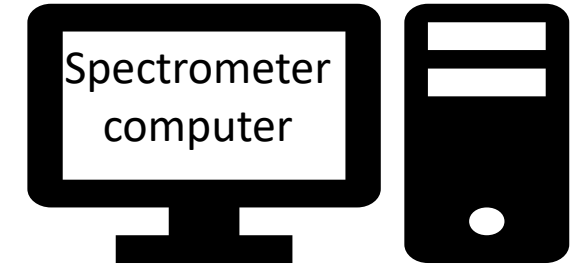
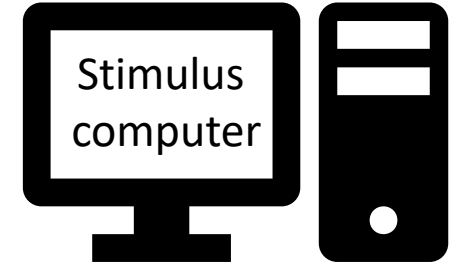
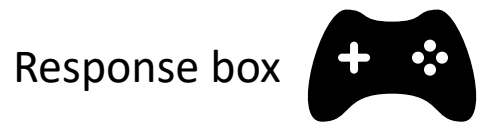
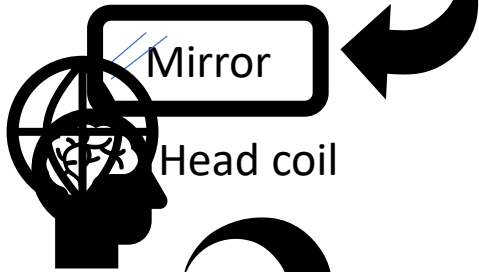
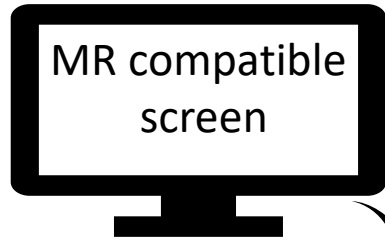
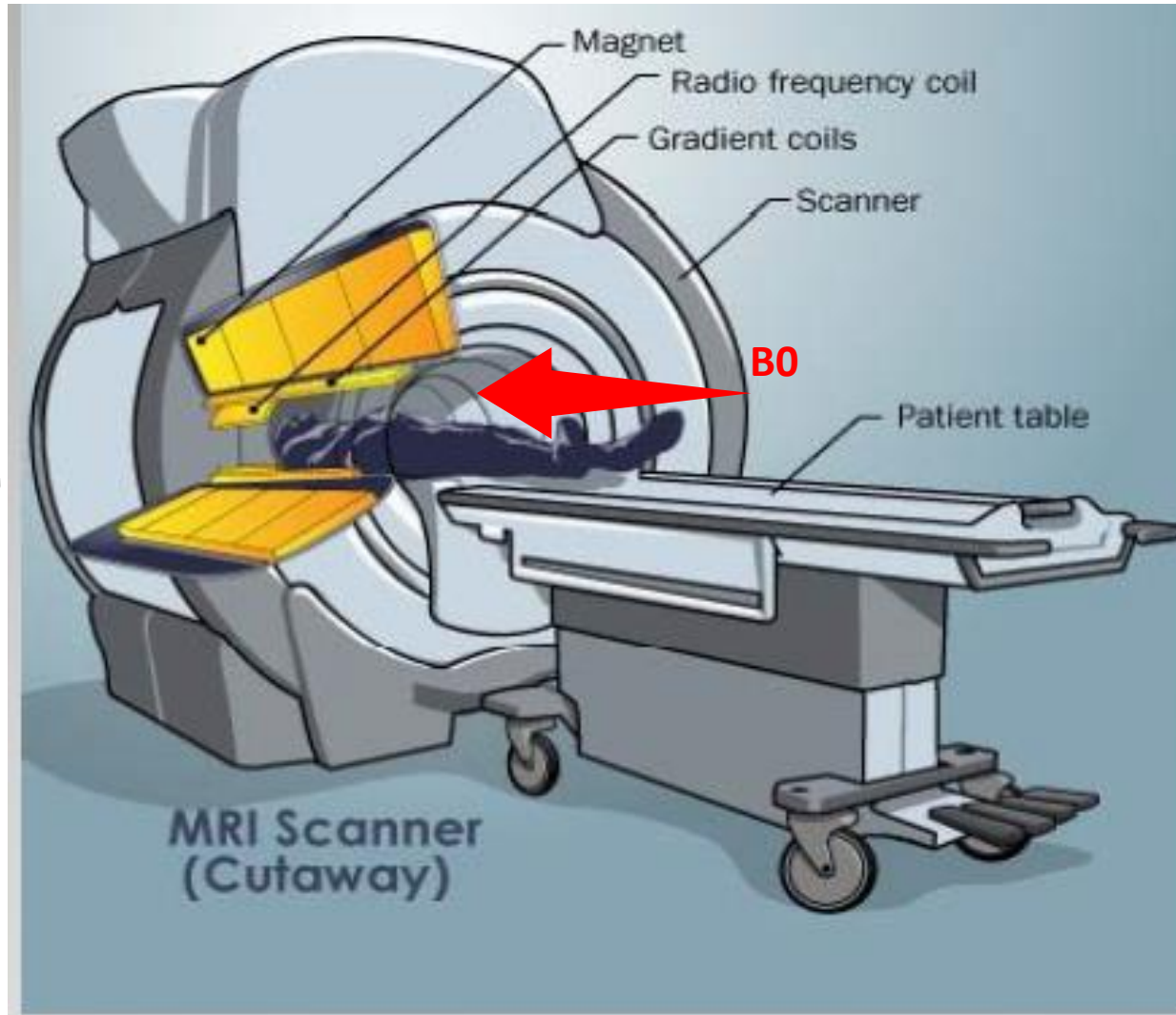
One measuring session
Number of images depending
on measuring time



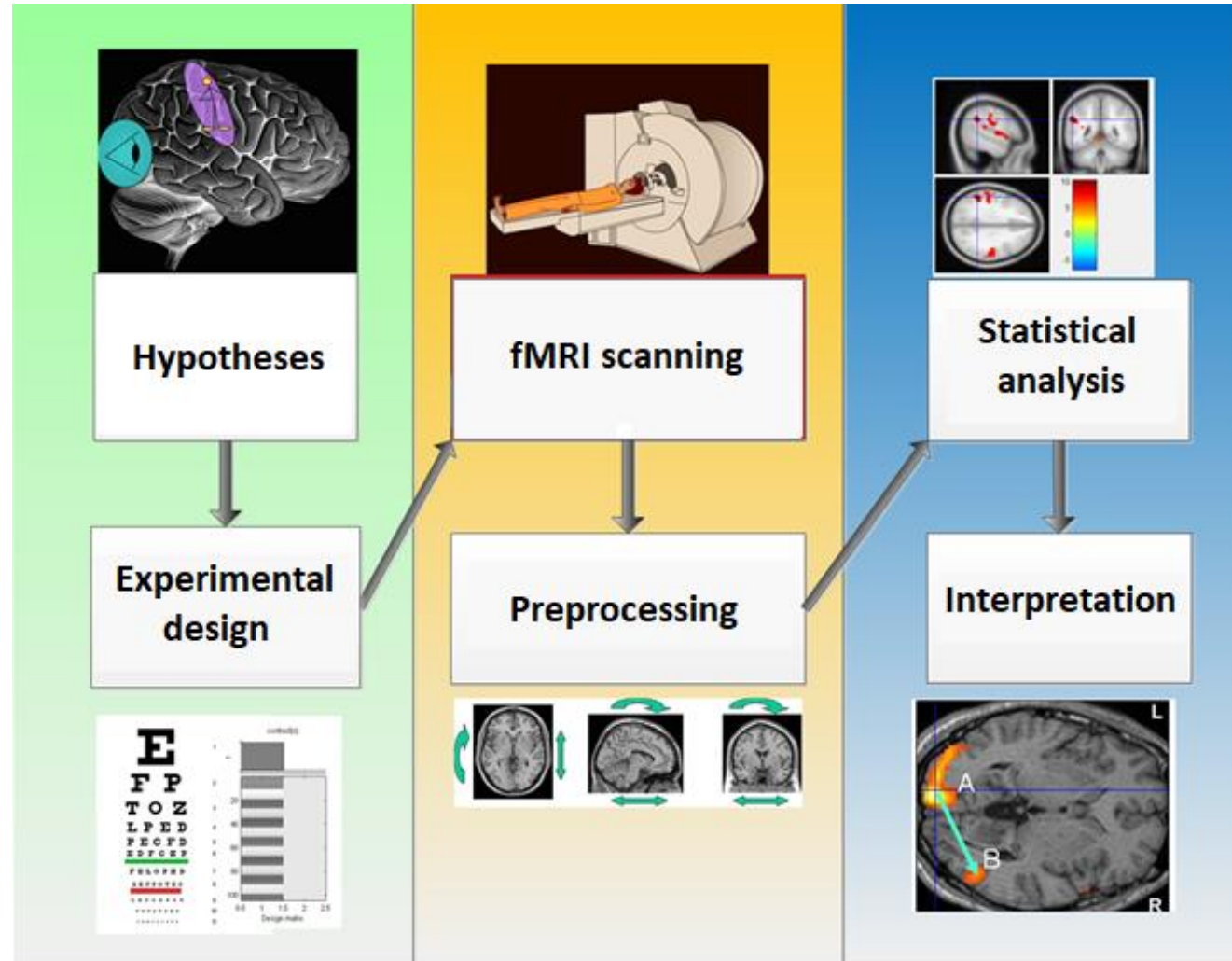
4D matrix



fMRI setup



fMRI experiment



fMRI experiment issues

We don't know the baseline BOLD signal level

➔ measurement of resting state or other control condition

Very small signal change

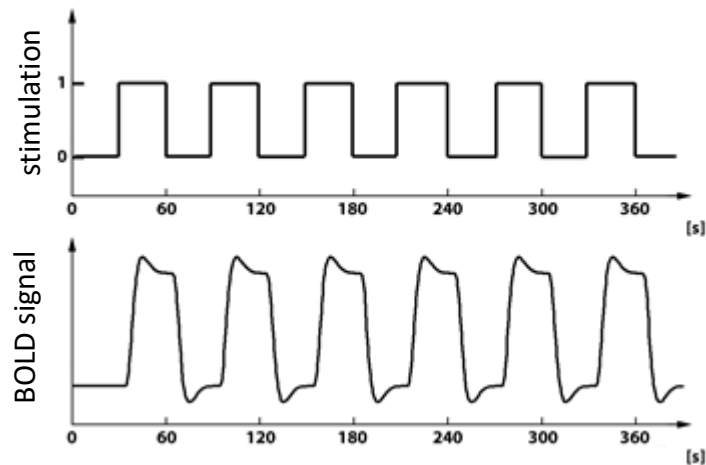
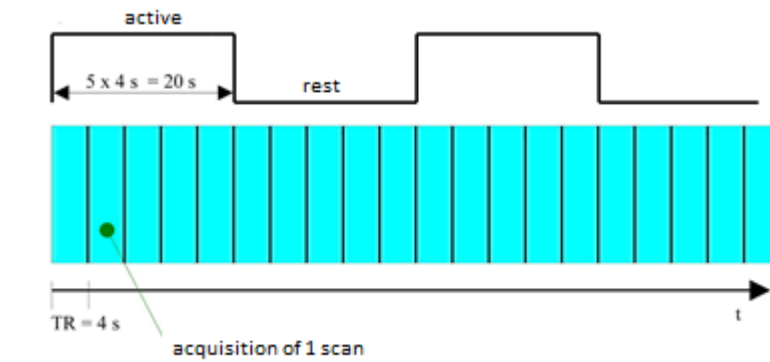
➔ repetition of conditions many times, acquisition of lot of data to detect the difference

Low-frequency fluctuations and BOLD signal drift

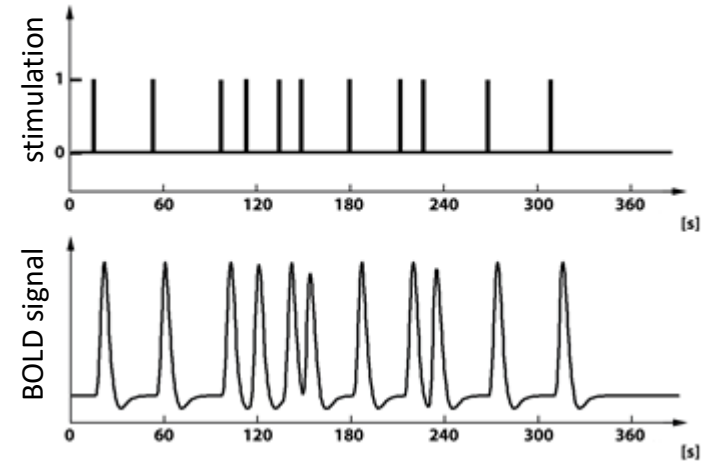
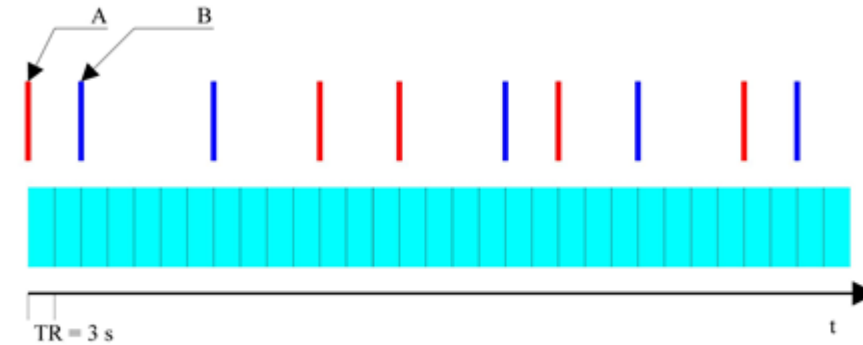
➔ alternations of experimental states during stimulation

fMRI experiments - design

Blocked



Event-related



Experimental design – advantages/disadvantages

Blocked

- Series of stimuli during time epoch(16-60s)
- Simple and powerful
- Easy to analyze
- Very good detection power
- Longer blocks may evoke heterogenous neuronal activity
- Estimating relative changes between tasks

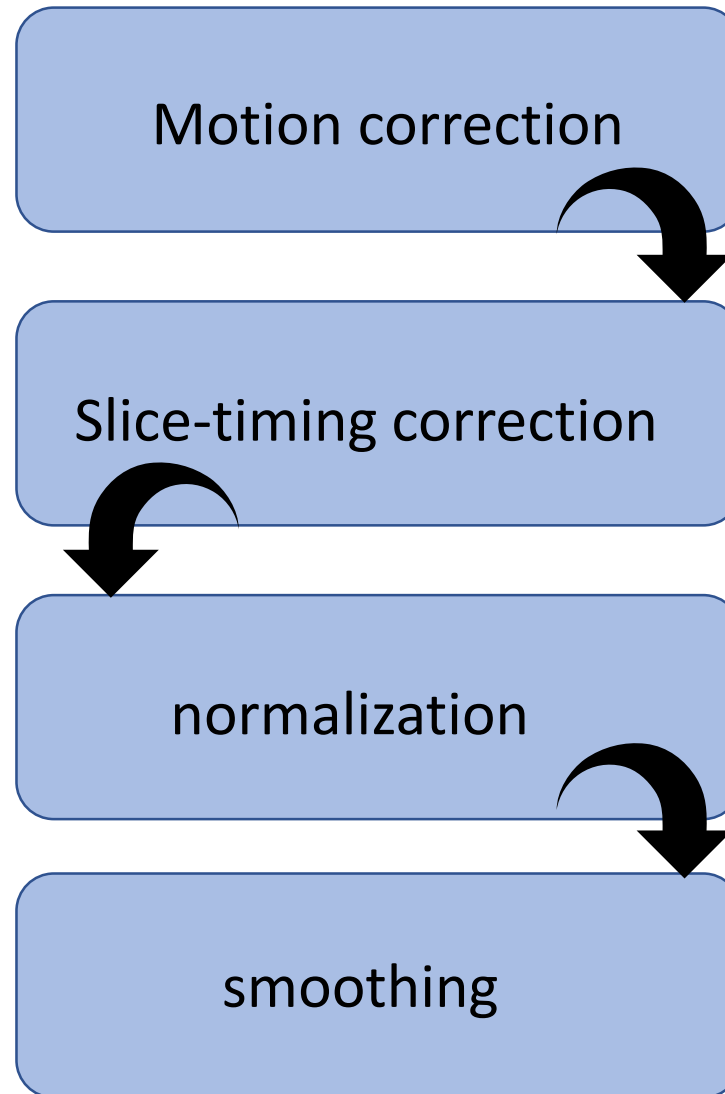
Event related

- Reactions to single stimuli
- Lower statistic power
- Estimation of HRF possible
- Longer measurement necessary
- More complicated data analysis

Sequence parameters

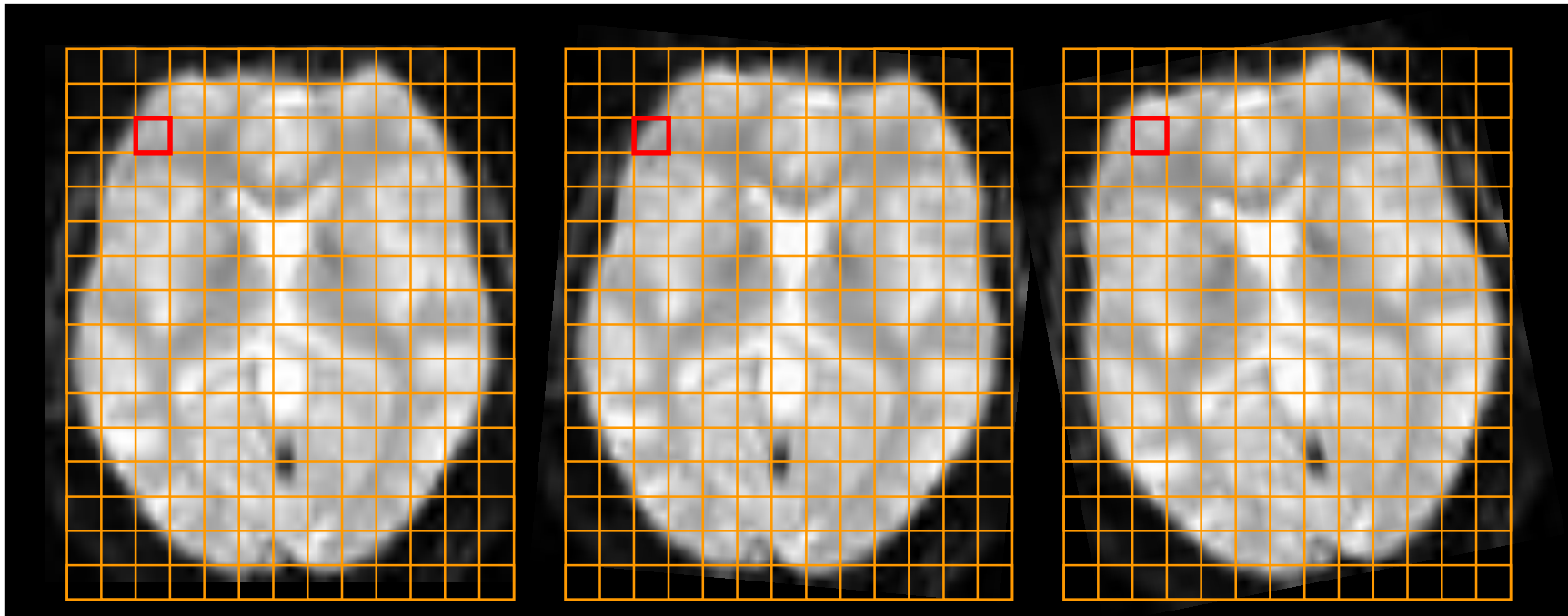
- T2* weighted, echo-planar BOLD images
- Typical parameters on 1,5 T MR:
 - resolution: 64x64 (128x128)
 - FOV = 220 mm \Rightarrow 3,4375 x 3,4375 mm²
 - Slice thickness: 3 - 7 mm
 - Bigger thickness – better SNR
 - Number of slices: 16 - 32
 - Volume acquisition time
 - Repetition time (TR)
 - 1,5 – 4 s
- Stronger fields possible
 - 3T, 7T, (9T, 11T, ...)
 - Stronger field \Rightarrow better SNR X worse susceptibility to artefacts

Preprocessing of the data



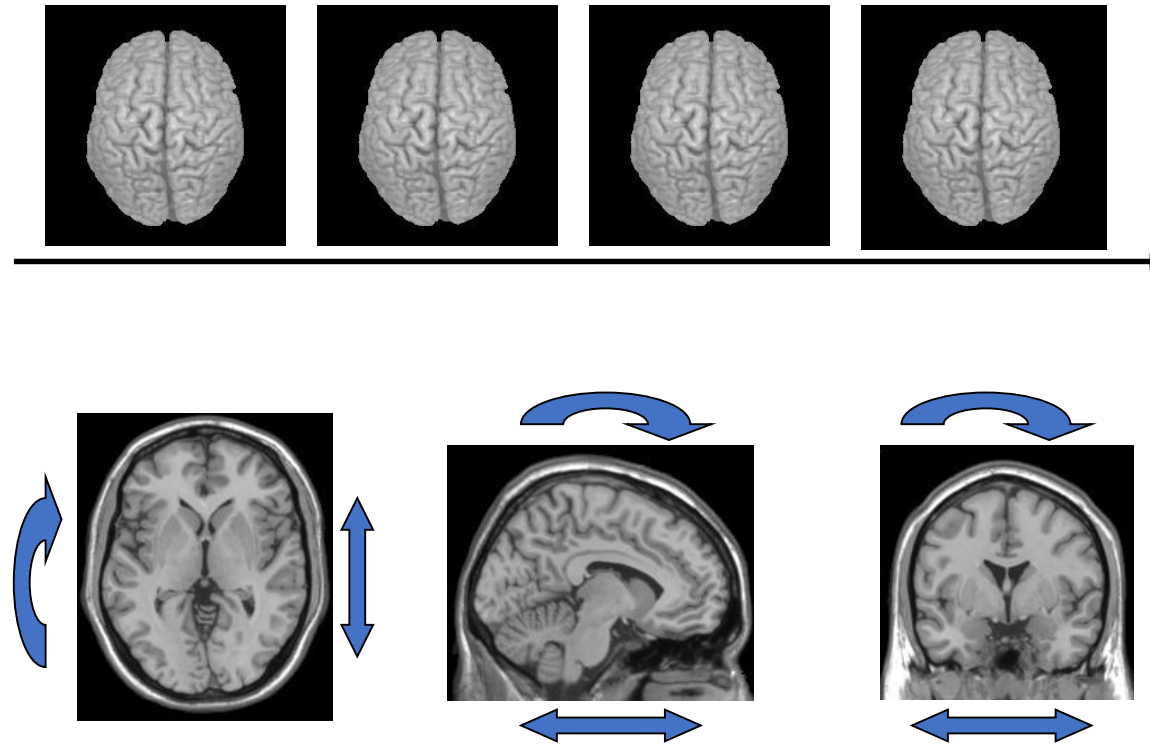
Motion correction

- Motion artefacts are the most problematic in fMRI
- Statistical parametric mapping methods work with single voxels independently
- The same voxel must correspond with the same spot in the brain



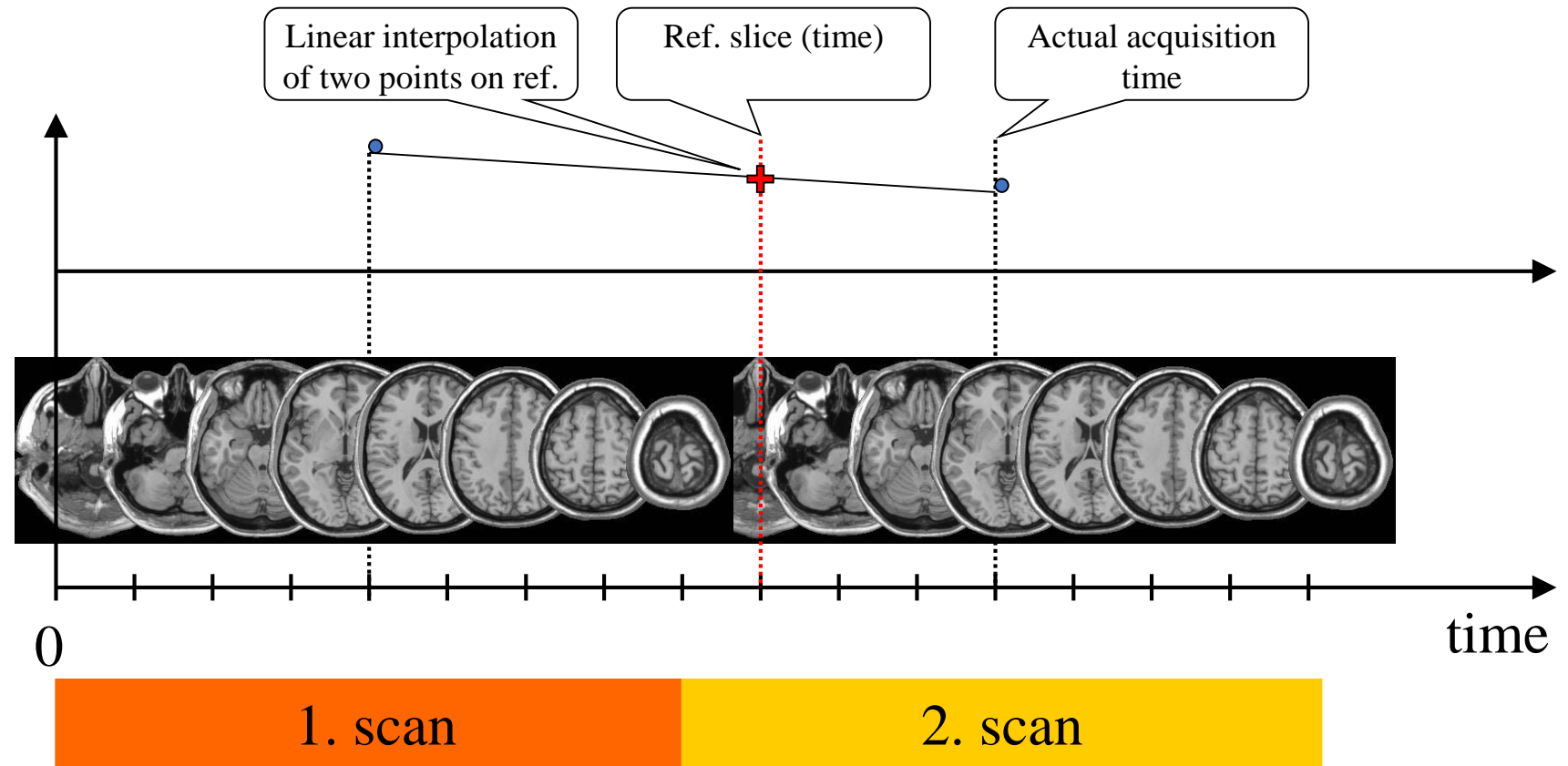
Motion correction

- Realignment to the first (referential) image
- Searching for optimal parameters (translation, rotation)



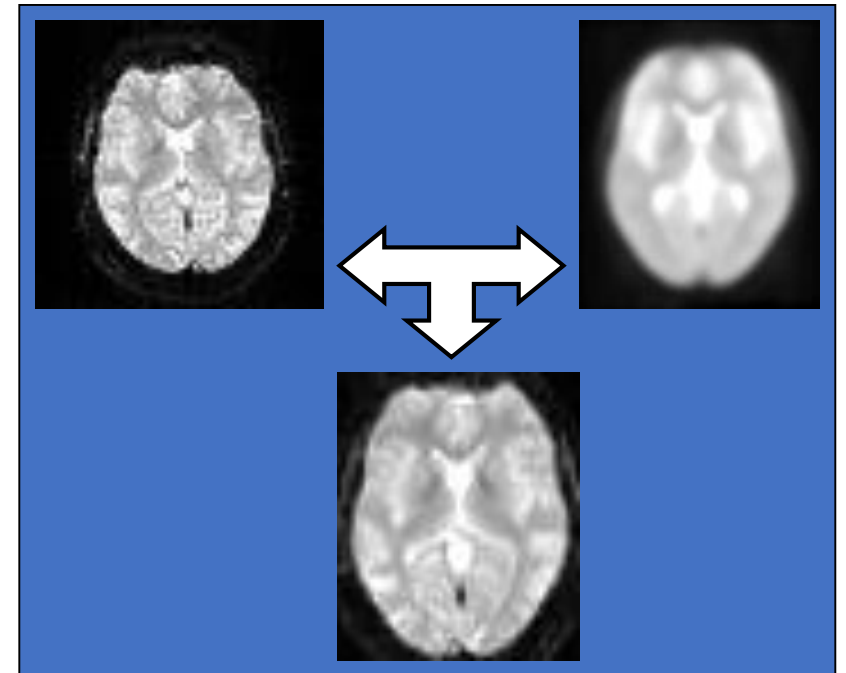
Slice timing correction

- Ideal case – acquisition of the whole brain volume in an infinitely short time
- Scanning of individual slices between 100 and 500 ms
- First and last layer from 2 to 4s apart
- Different slices different HRF
- Can be corrected by weighted distance from referential slice and referential time



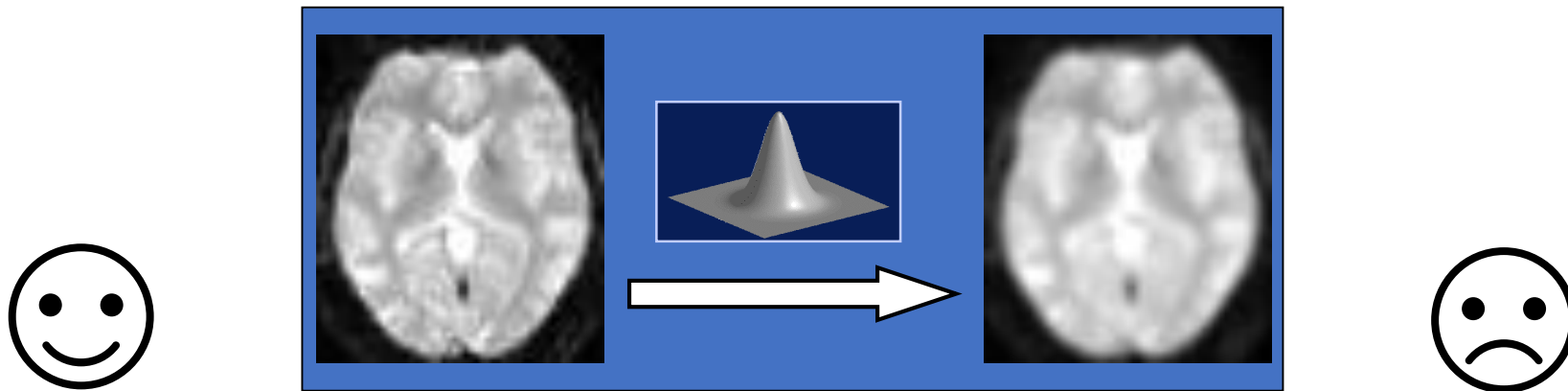
Normalization

- Neuroscience research X clinical application
- Transformation into standardized template (MNI, Talairach)
- Linear transformations
 - Translation
 - Rotation
 - Size change
- Nonlinear deformations



Spatial smoothing

- Filtration of rapid changes in signal intensity
- Various filter shapes – most frequent Gaussian kernel

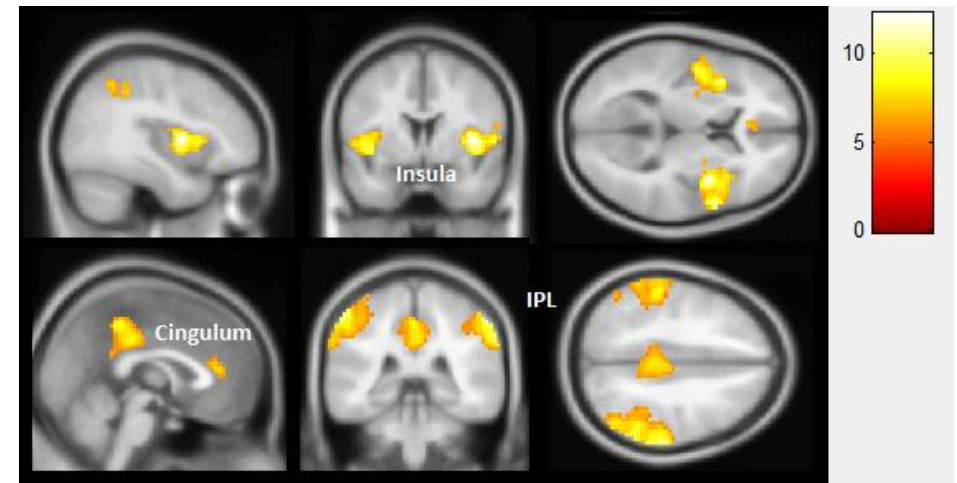
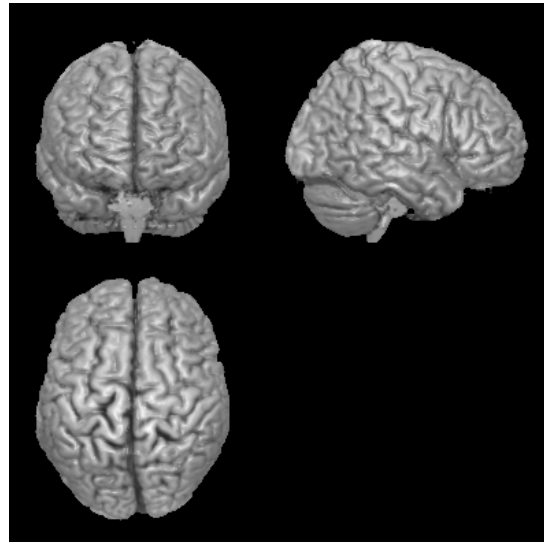
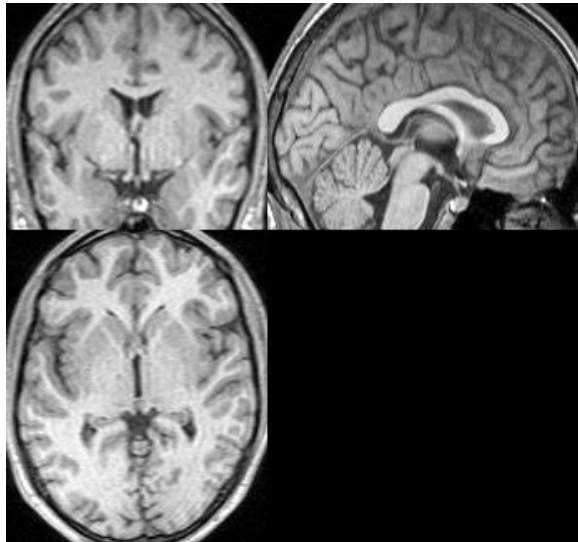
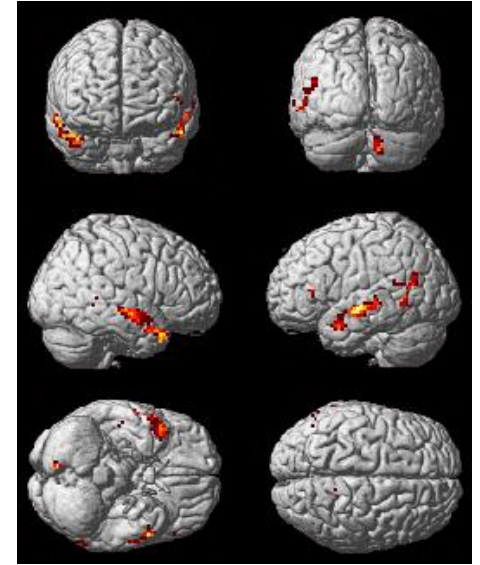


- reduces noise in the image (increase signal to noise ration - SNR)
- improves spatial distribution of the data
- better fit in group comparison

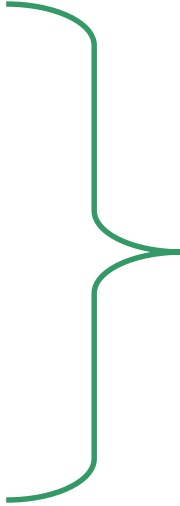
- Risk of loosing activated regions
- data transformation – not working with the raw data

Anatomical images

- Normalization and co-registration with functional scans
- Segmentation and rendering (3D view)
- Used for display of activation maps

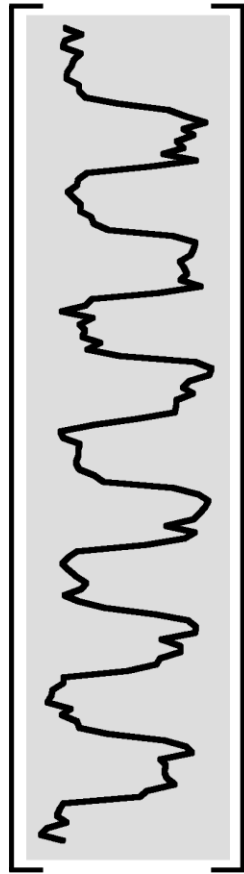
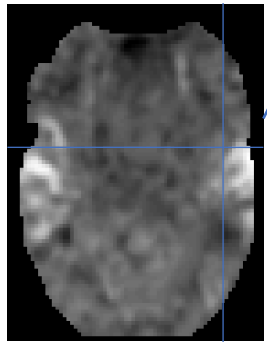


Statistical analysis

- Methods without model
 - ICA/PCA
 - Methods with model (hypothesis about the shape of the BOLD signal)
 - Correlation
 - T-test
 - ANOVA
 - AnCova
 - Linear regression
 - Multiple regression
 - F-test
 - etc..
- 
- Cases of
GLM
(general linear model)

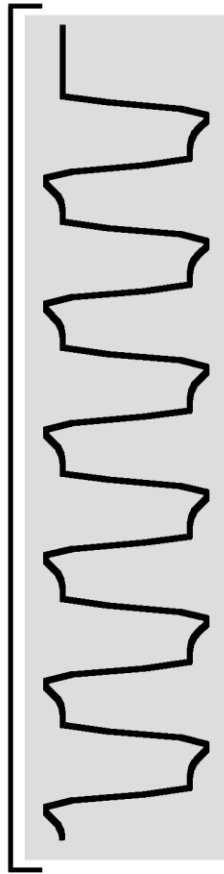
GLM

$$Y = X\beta + \varepsilon$$

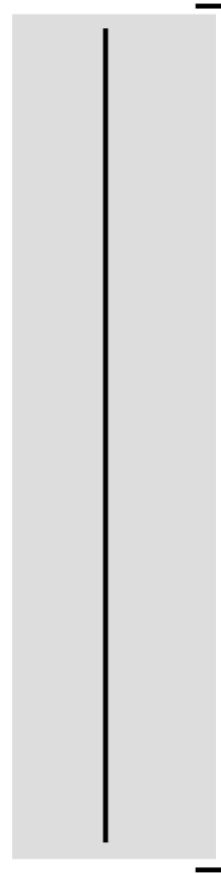


Measured signal

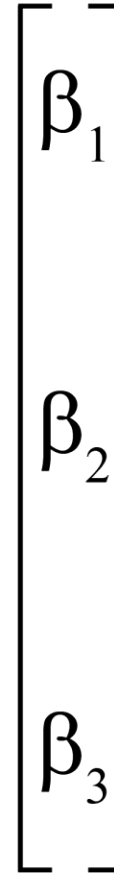
=



Regressors/modeled signals



*



parameters

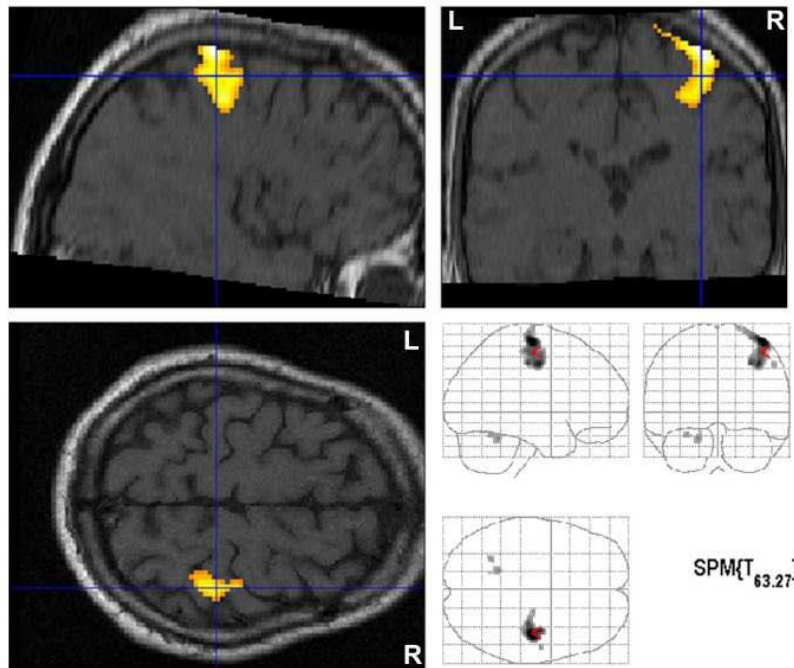
+



residuals

Hypotheses testing

- T-test about β parametres
- T-test is run on every voxel across the brain
- Suprathreshold voxels mark regions where tested effect was significant



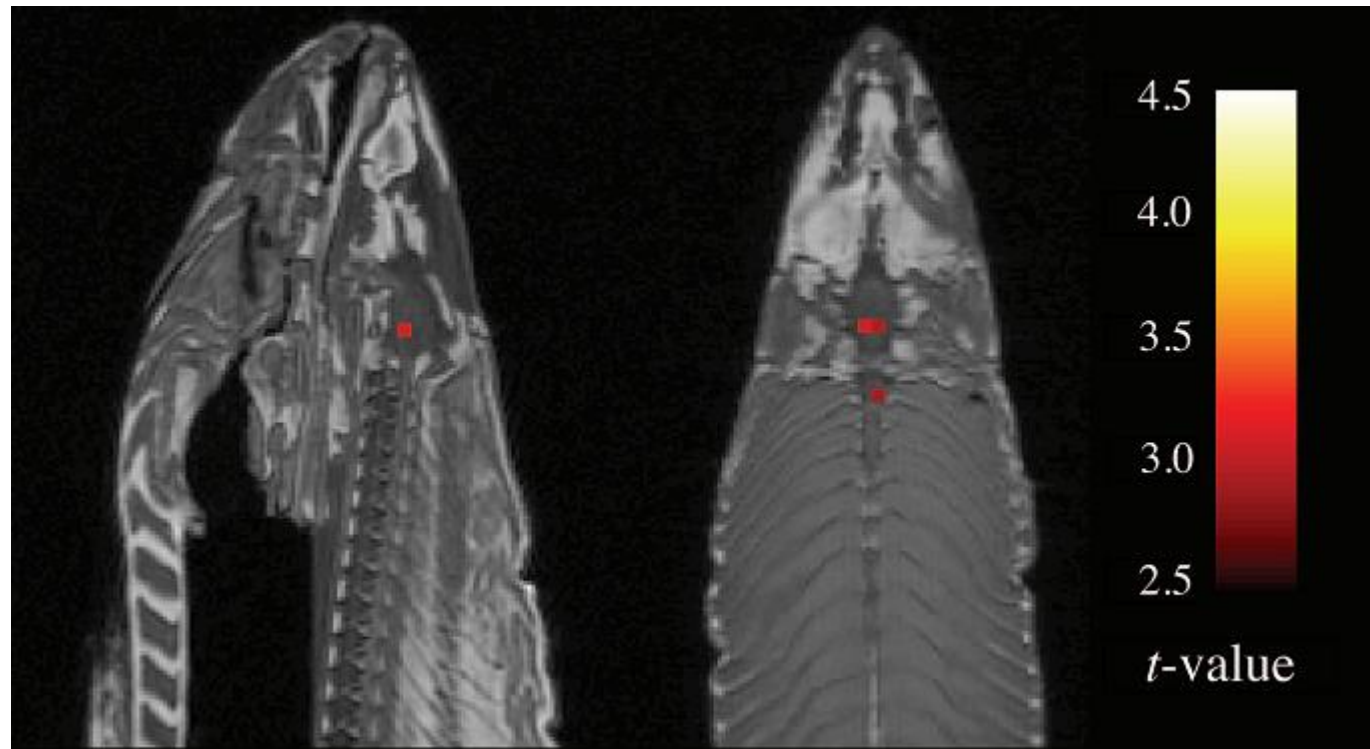
Movement of left hand

$P < 0.001$

$T=3.1$

Multiple comparisons problem

Neural correlates of interspecies perspective taking in the post-mortem Atlantic Salmon:
An argument for multiple comparisons correction (Bennett et al., 2009)

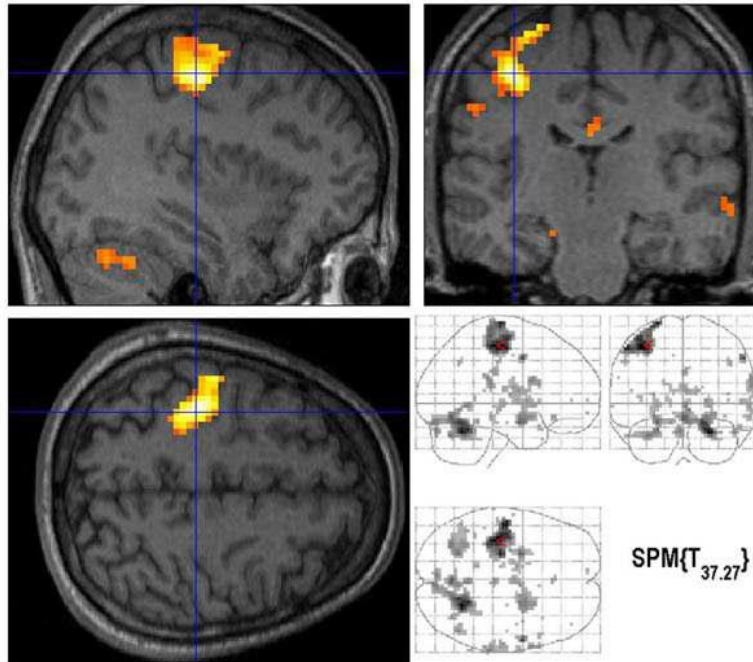


Uncorrected results

Correction for multiple testing

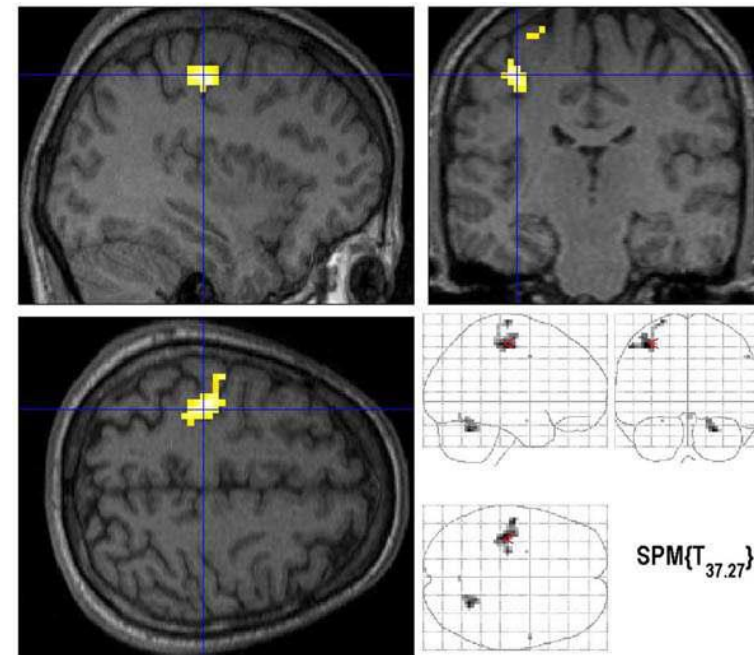
Without correction

- Sig. level for one voxel
 - When n results displayed, probability of false positive results increases n -times!
 - $p < 0.001$



With correction

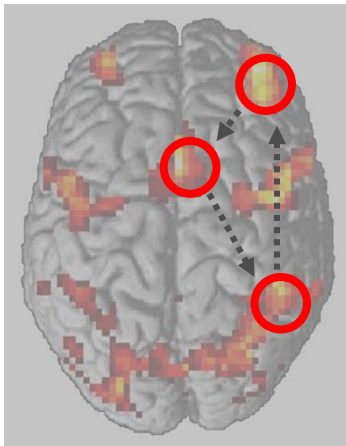
- Sig. level for whole sample
 - FEW – family wise error
 - FDR – false discovery rate
 - $p < 0.05$



Functional organization in the brain

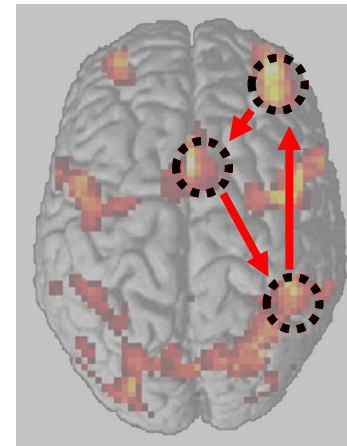
Functional specialization

- Specialized and spatially separated modules
- Regions of interest



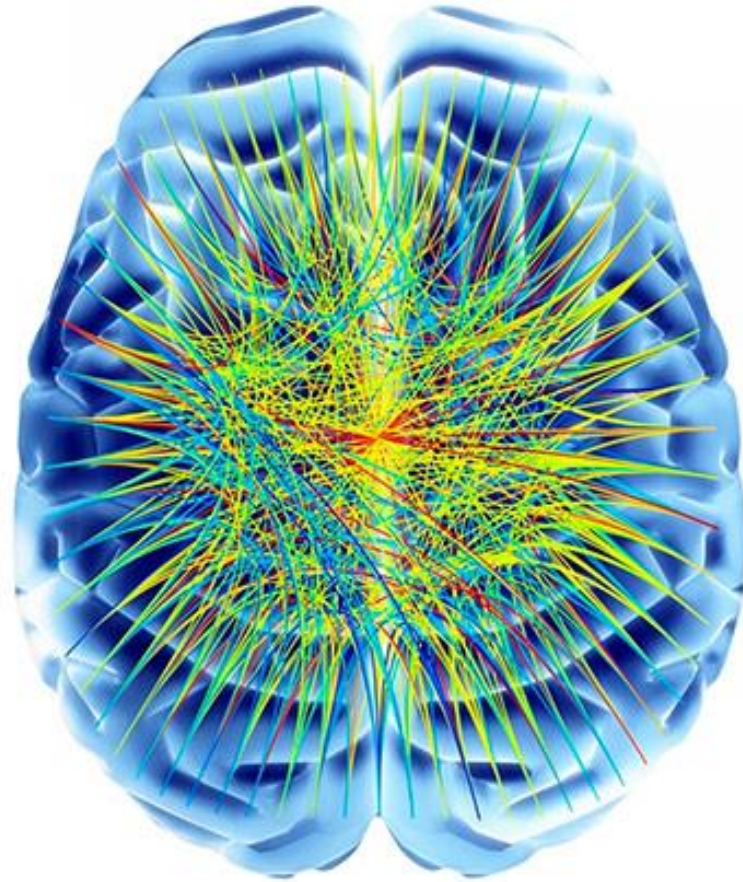
Functional integration

- Specific function is characterized by interconnection of relevant regions
- Large-scale neuroimaging
- networks



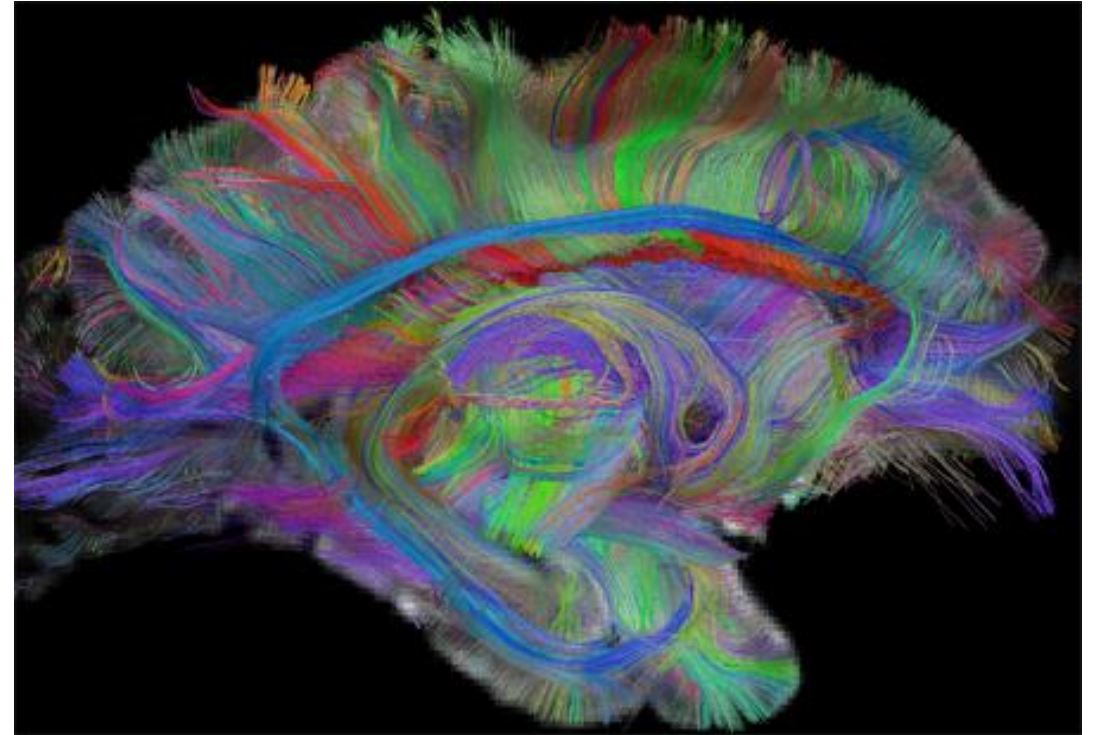
Connectivity

- Structural
- Functional
- Effective



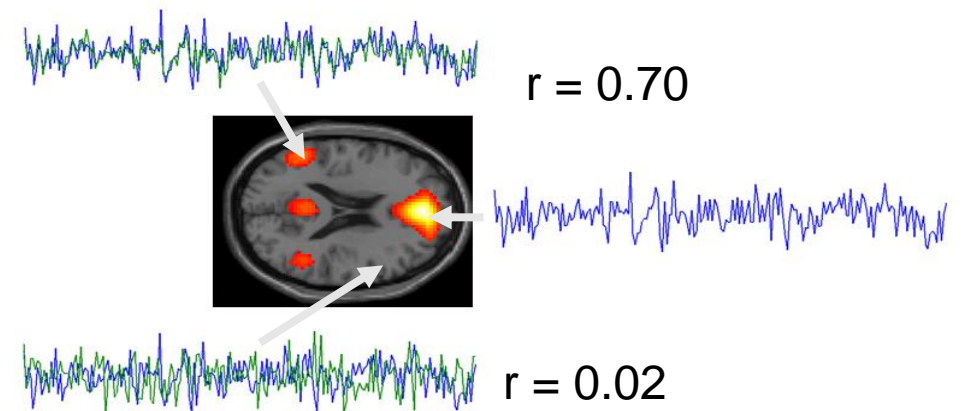
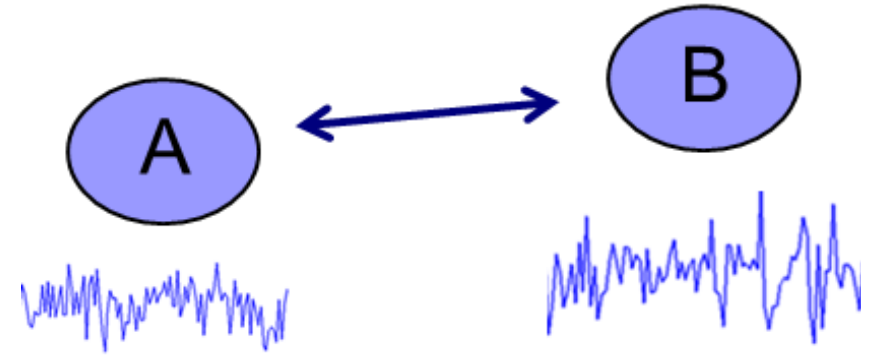
Structural connectivity

- Mapping of anatomical connections between cortical region
- white matter organization
- Diffusion tensor imaging (DTI)
- Static description of the system



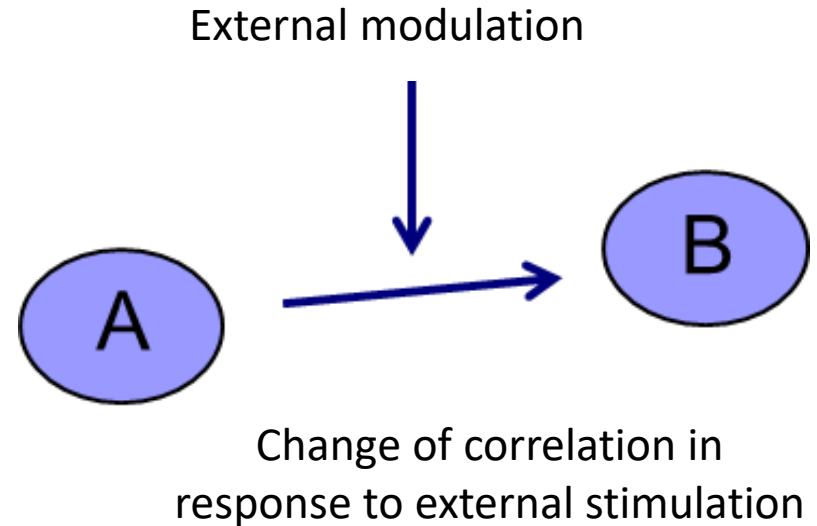
Functional connectivity

- Correlation between large distance neurophysiological events
- Indirect assumption about relationship between the regions
- Seed analysis, ICA



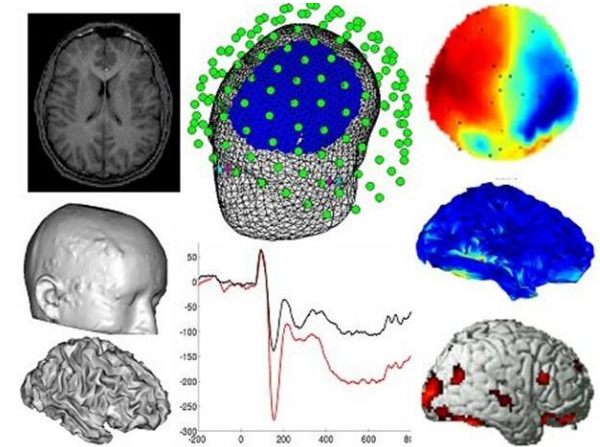
Effective connectivity

- Causal directed influences between neurons or neuronal populations
- Indirect assumption of connection between regions and how these are modulated by external stimulation
- PPI, DCM

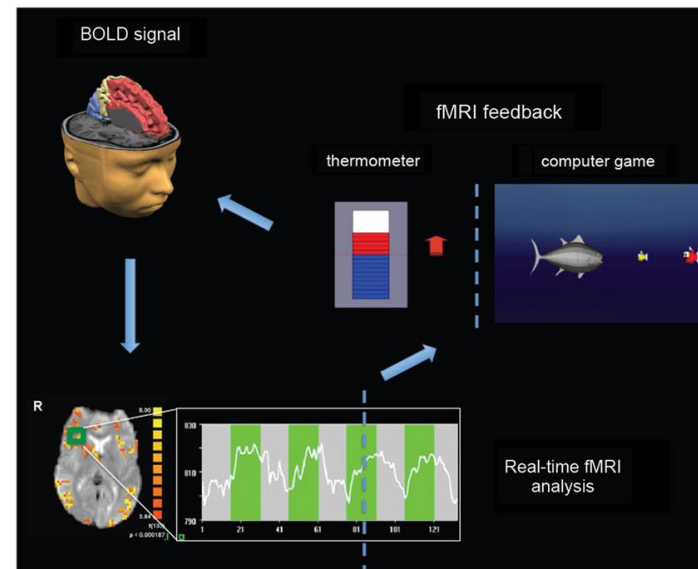


More examples of fMRI applications

- Resting state fMRI – large scale networks
- Real time fmri - neurofeedback
- multimodal imaging EEG-fMRI
- Hyperscanning
- Physiological measurement ECG, breathing, galvanic response...



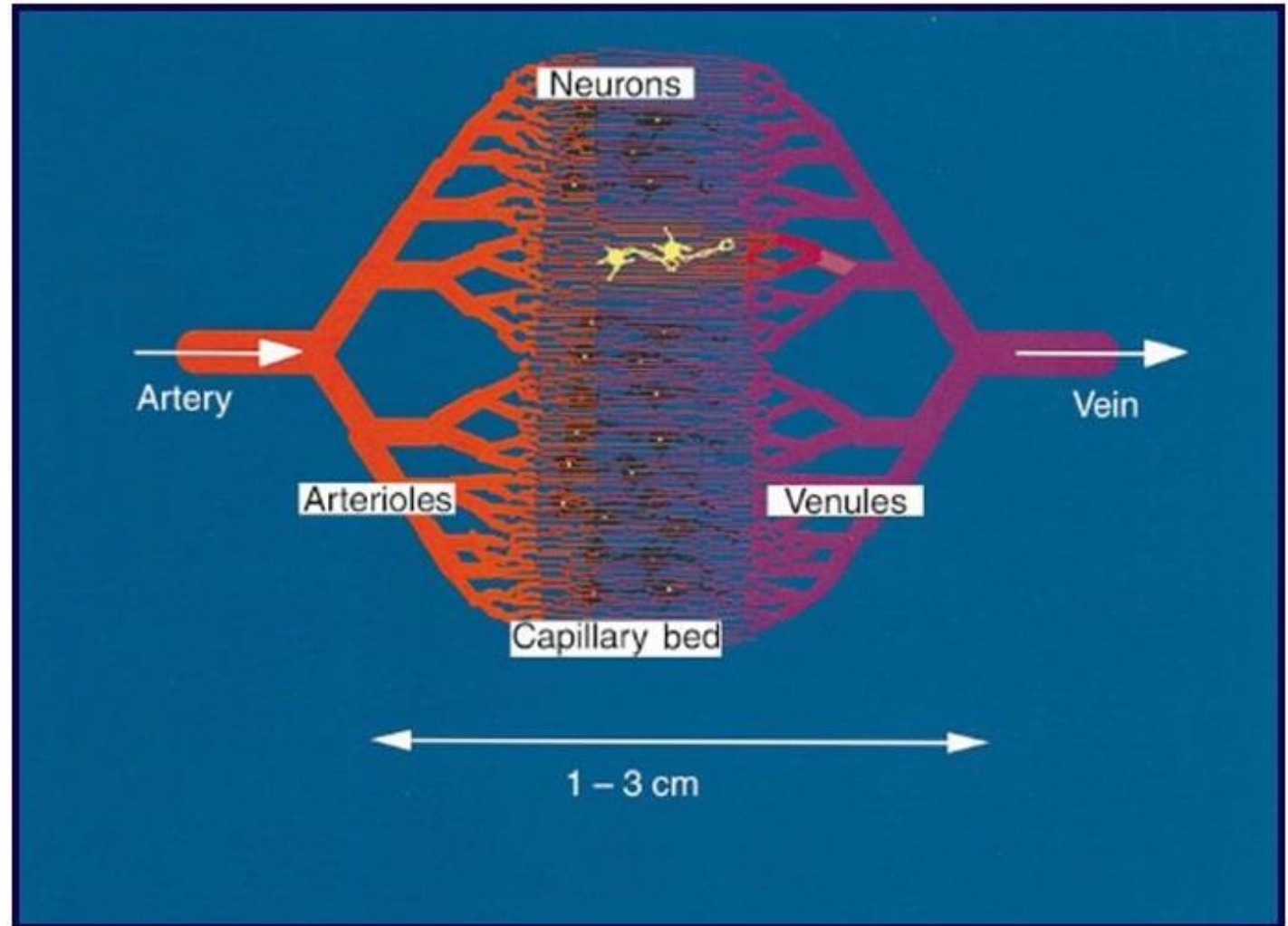
<http://www.neuroscience.cam.ac.uk/directory/profile.php?RikHenson>



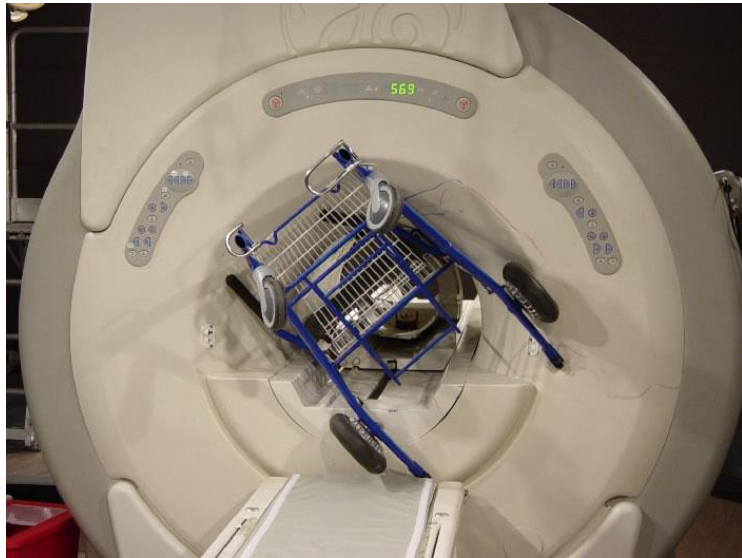
(Carie and de Falco, 2015)

fMRI limitations

- **Artifacts** - misleading BOLD signal changes (head motion, ECG, respiration)
- BOLD response to a stimulus is delayed, which restricts maximum **temporal resolution** achievable
- Vasculature – implications for **spatial resolution**
- **Conceptual limitations**



Beware – the main magnetic field is always ON!



Thank you for attention...