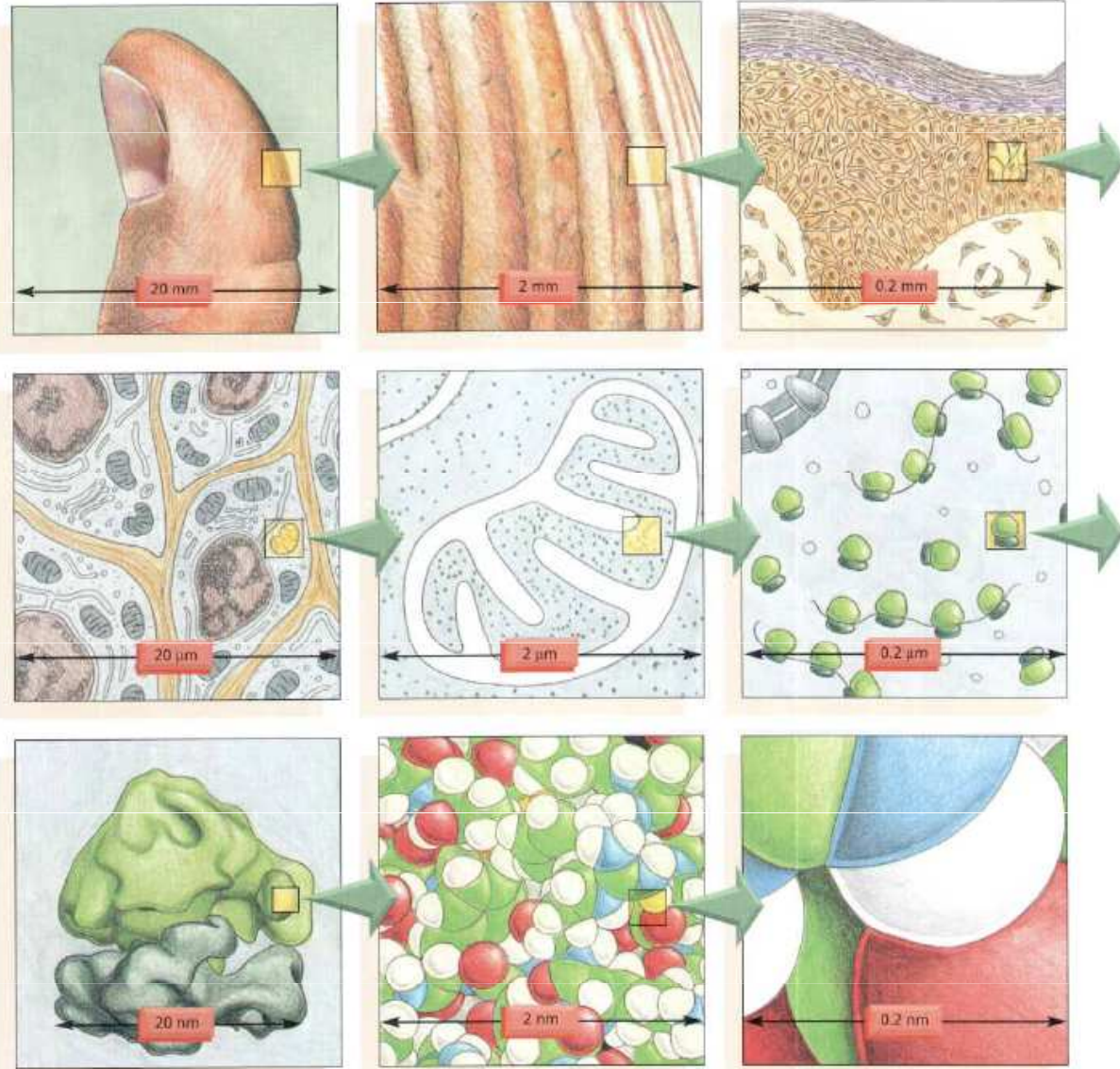


# NMR-based Structural Biology for Studying Biomolecular Interactions

Karel Kubíček

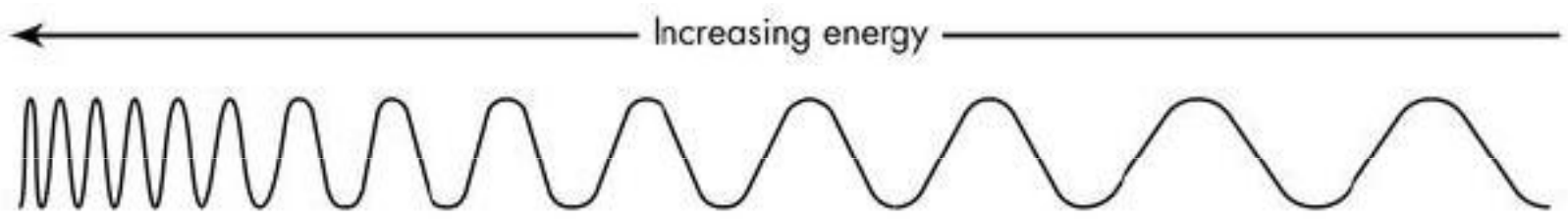


### Composition of the Earth's Crust, Seawater, and the Human Body\*

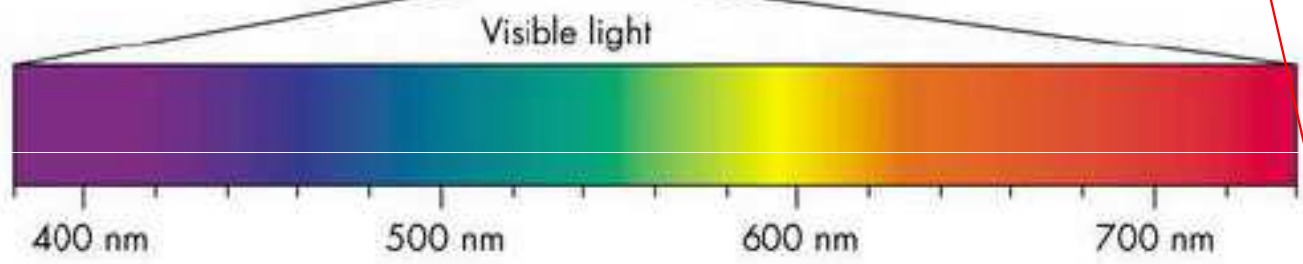
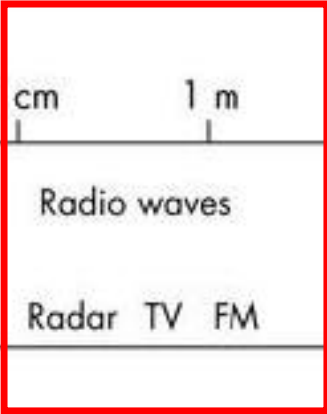
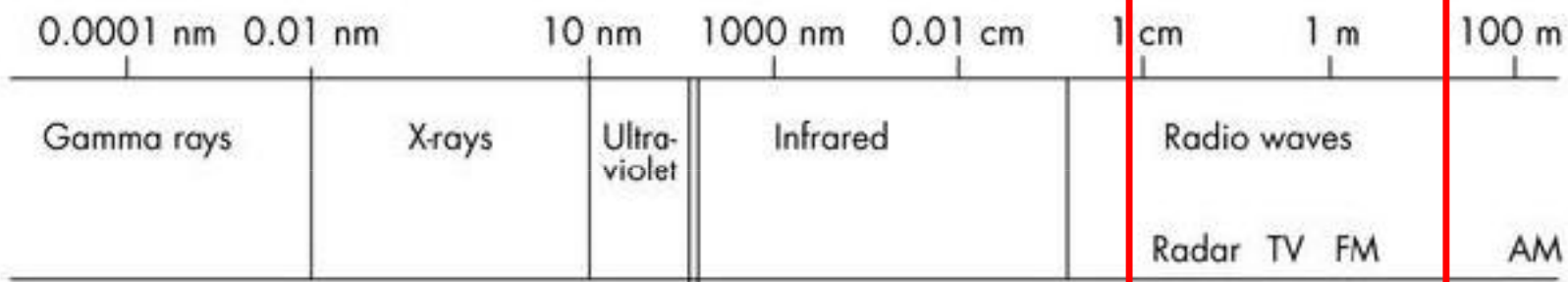
Earth's Crust		Seawater		Human Body <sup>†</sup>	
Element	%	Compound	mM	Element	%
O	47	Cl <sup>-</sup>	548	H	63
Si	28	Na <sup>+</sup>	470	O	25.5
Al	7.9	Mg <sup>2+</sup>	54	C	9.5
Fe	4.5	SO <sub>4</sub> <sup>2-</sup>	28	N	1.4
Ca	3.5	Ca <sup>2+</sup>	10	Ca	0.31
Na	2.5	K <sup>+</sup>	10	P	0.22
K	2.5	HCO <sub>3</sub> <sup>-</sup>	2.3	Cl	0.08
Mg	2.2	NO <sub>3</sub> <sup>-</sup>	0.01	K	0.06
Ti	0.46	HPO <sub>4</sub> <sup>2-</sup>	<0.001	S	0.05
H	0.22			Na	0.03
C	0.19			Mg	0.01

\*Figures for the earth's crust and the human body are presented as percentages of the total number of atoms; seawater data are millimoles per liter. Figures for the earth's crust do *not* include water, whereas figures for the human body do.

<sup>†</sup>Trace elements found in the human body serving essential biological functions include Mn, Fe, Co, Cu, Zn, Mo, I, Ni, and Se.



→ Increasing wavelength →



NMR

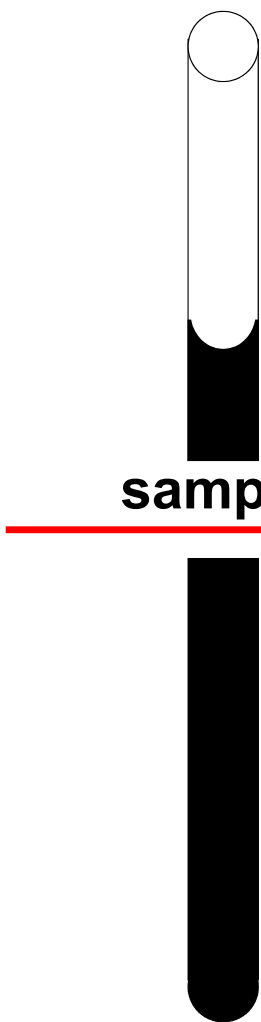


200-500  $\mu\text{l}$  of  
100-1000  $\mu\text{M}$  compound

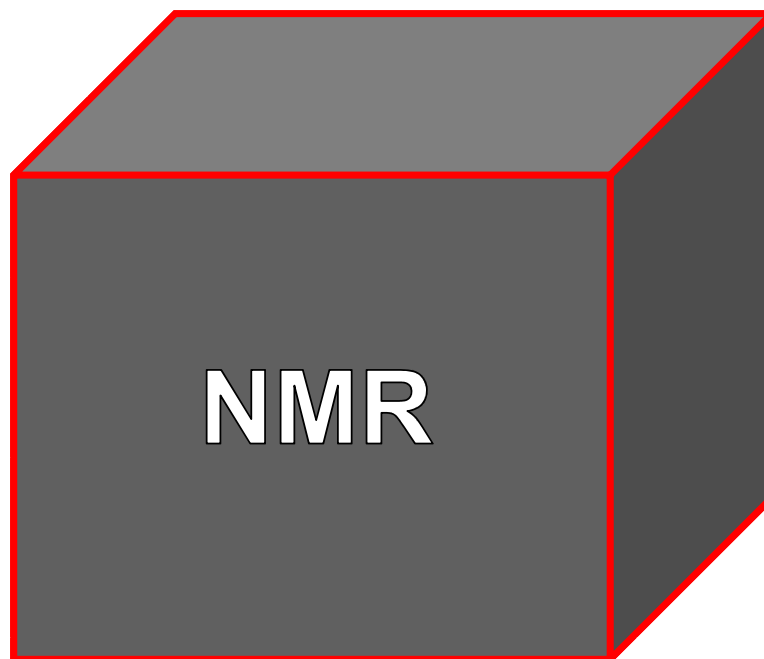
Method of choice

Data to be analyzed

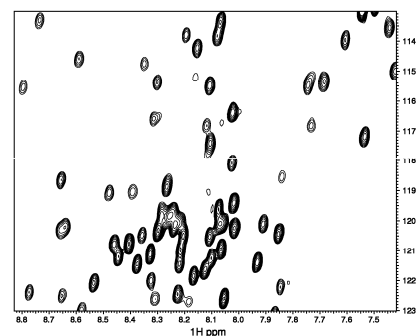
Results



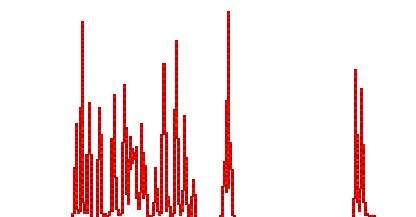
**sample**



**NMR**



**spectrum**



- 1) Structure
- 2) Relaxation properties
- 3) Interaction at atomic level resolution
- 4) Analysis
- 5) Image

# NMR hardware

- 1) Magnet
- 2) Spectrometer
- 3) Control units





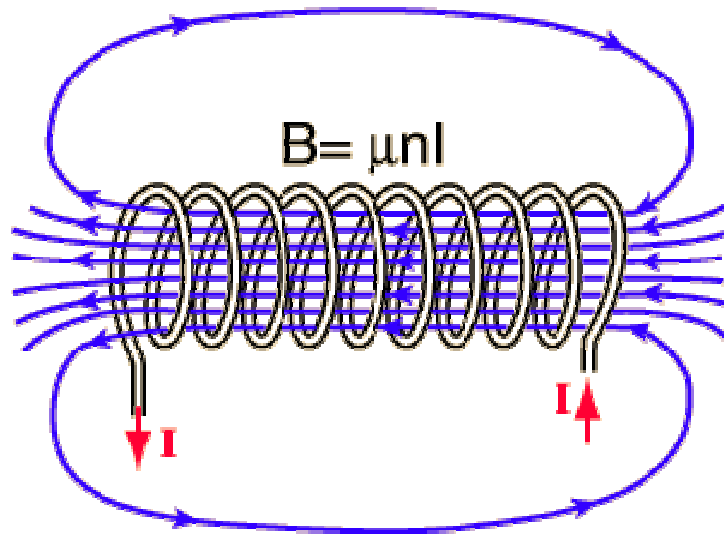
*NMR spectrometer*



Earth's Magnetic Field

$\sim 50\mu\text{T}$

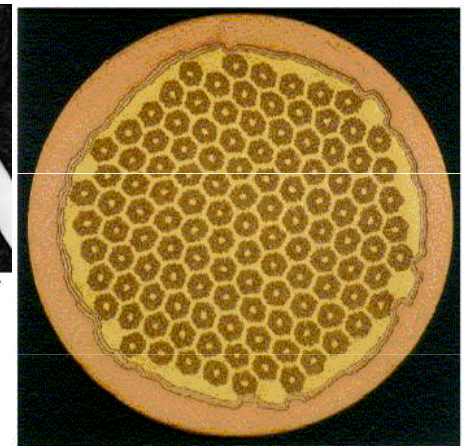
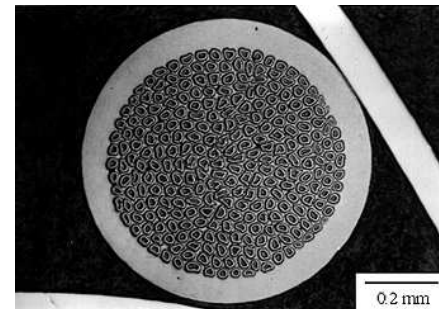
## Ampere's law & solenoid



The magnetic field is concentrated into a nearly uniform field in the center of a long solenoid. The field outside is weak and divergent.

## Magnet

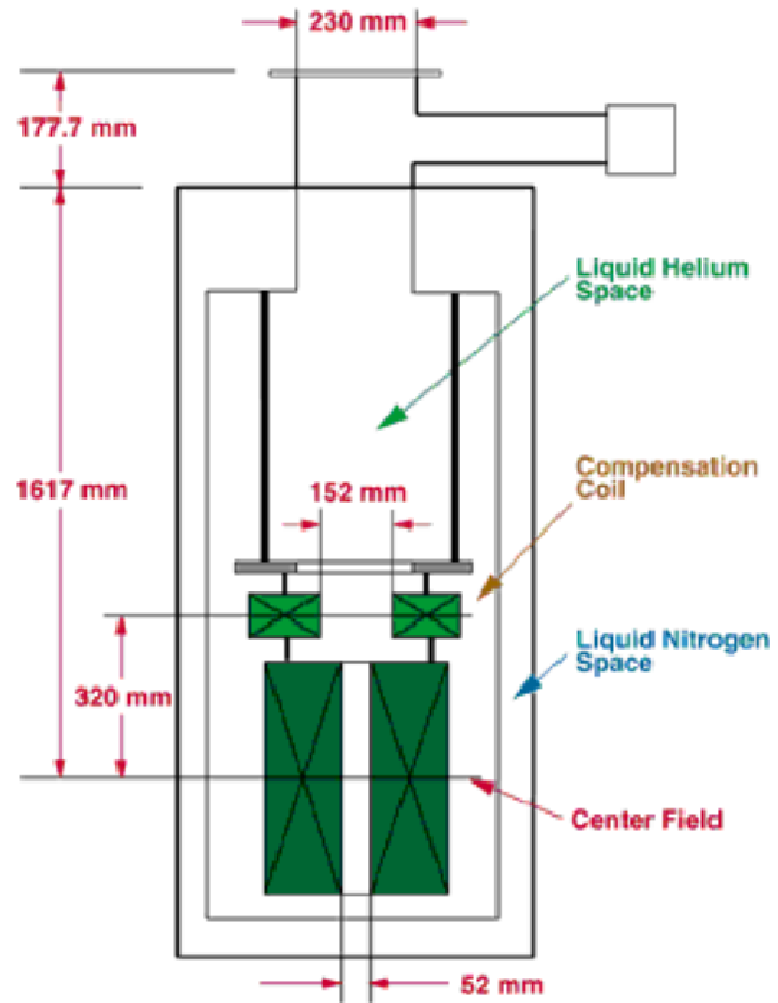
- superconducting solenoids immersed into He bath
- He-bath  $\sim 4$  K further improved to  $\sim 2.1$  K with J-T pump
- field strength 25-28 Tesla
- $(\text{Nb}, \text{Ta})_3\text{Sn}$  superconductor of 0.81 mm with  $\sim 271$  filaments buried in OFHC copper matrix

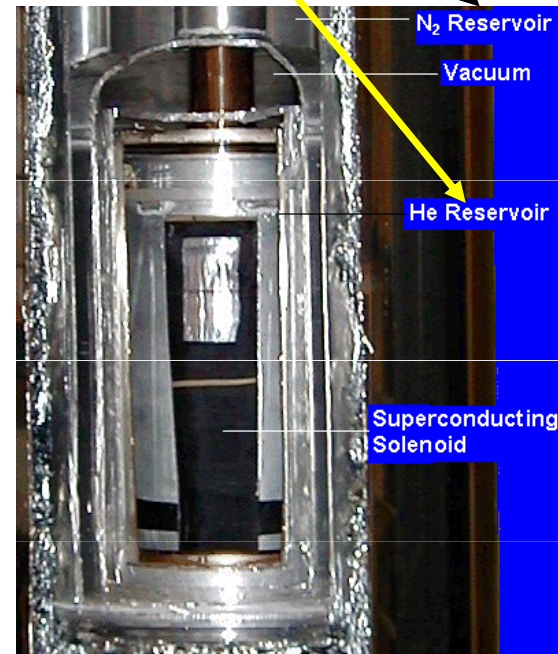
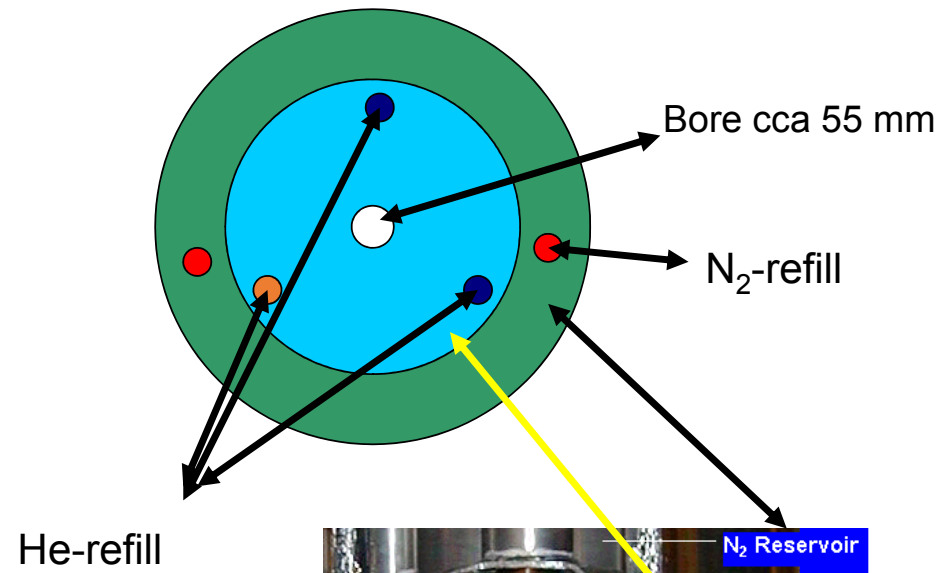




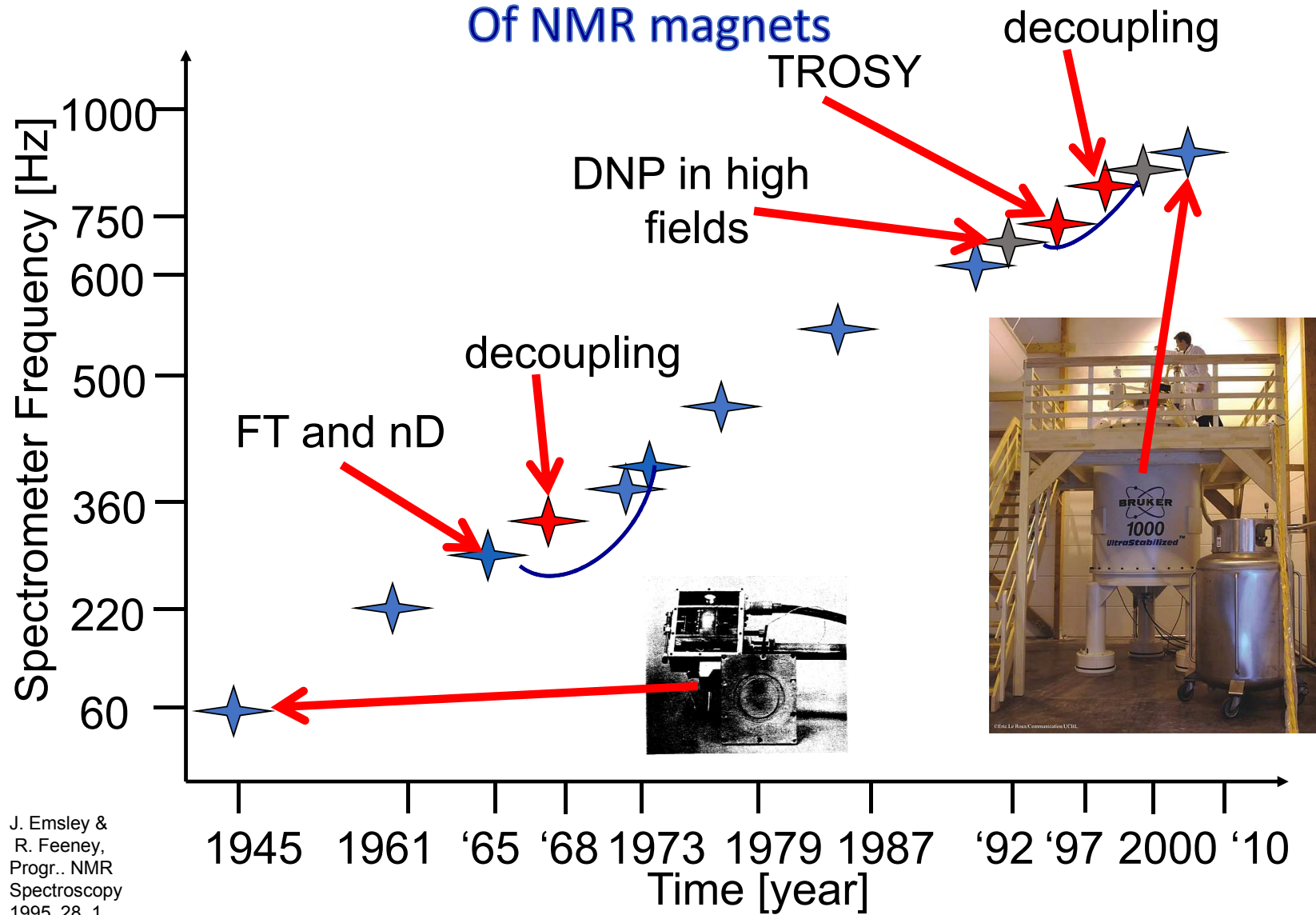


## 20T Superconducting Magnet





# Improvement of sensitivity, resolution and signal-to-noise ratio Of NMR magnets



J. Emsley &  
R. Feeney,  
Progr.. NMR  
Spectroscopy  
1995, 28, 1

# Quench

an **abnormal** termination of magnet operation

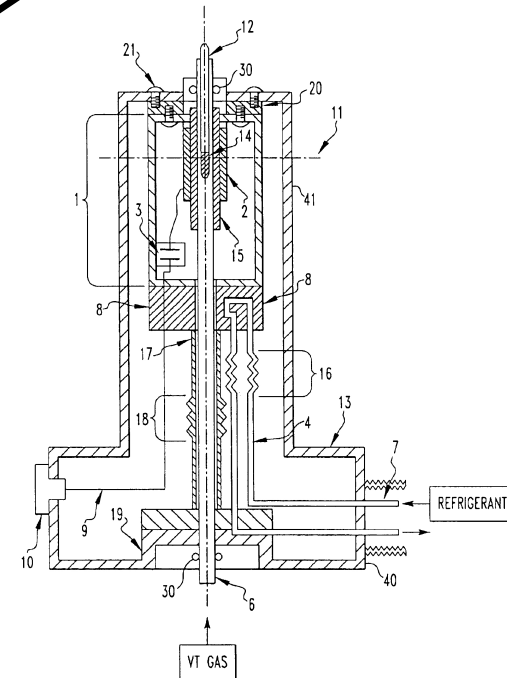
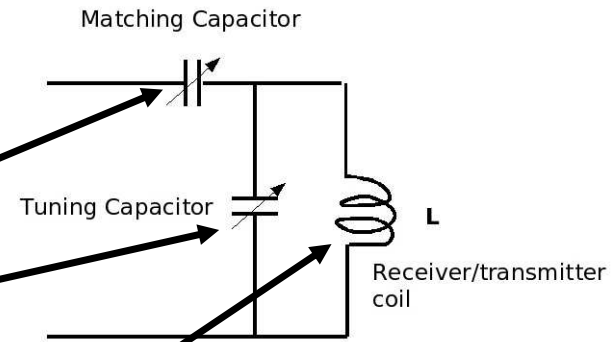
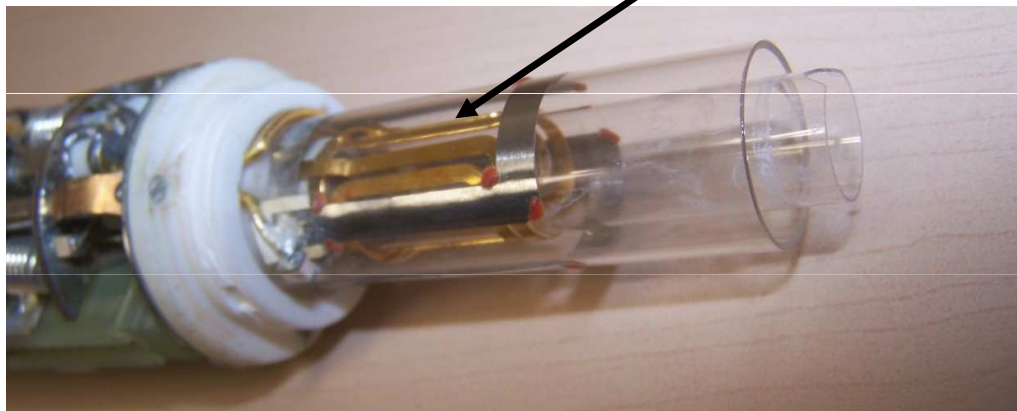
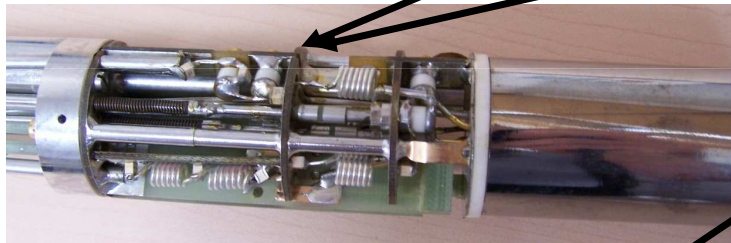
Occurs when part of the superconducting coil enters the normal (resistive) state.

This can **occur**

- i) because the field inside the magnet is too large
- ii) the rate of change of field is too large (causing eddy currents and resultant heating in the copper support matrix)
- iii) or a combination of the two.
- iv) a defect in the magnet can cause a quench.

**MOVIE: [https://www.youtube.com/watch?v=d-G3Kg-7n\\_M](https://www.youtube.com/watch?v=d-G3Kg-7n_M)**

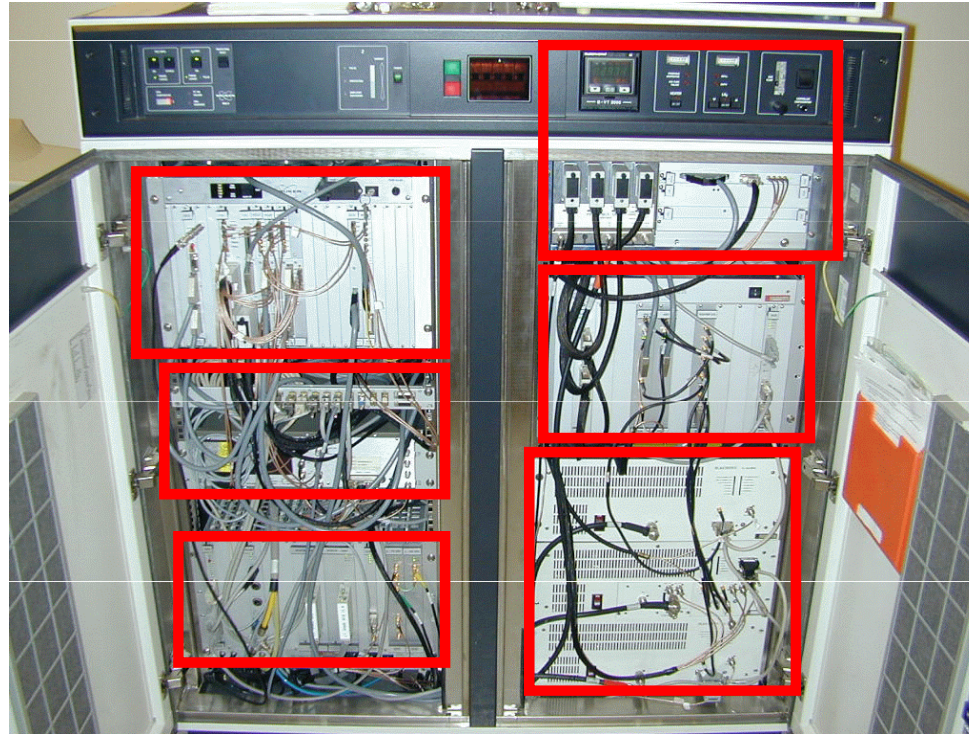
# NMR Probe(head)





## Spectrometer

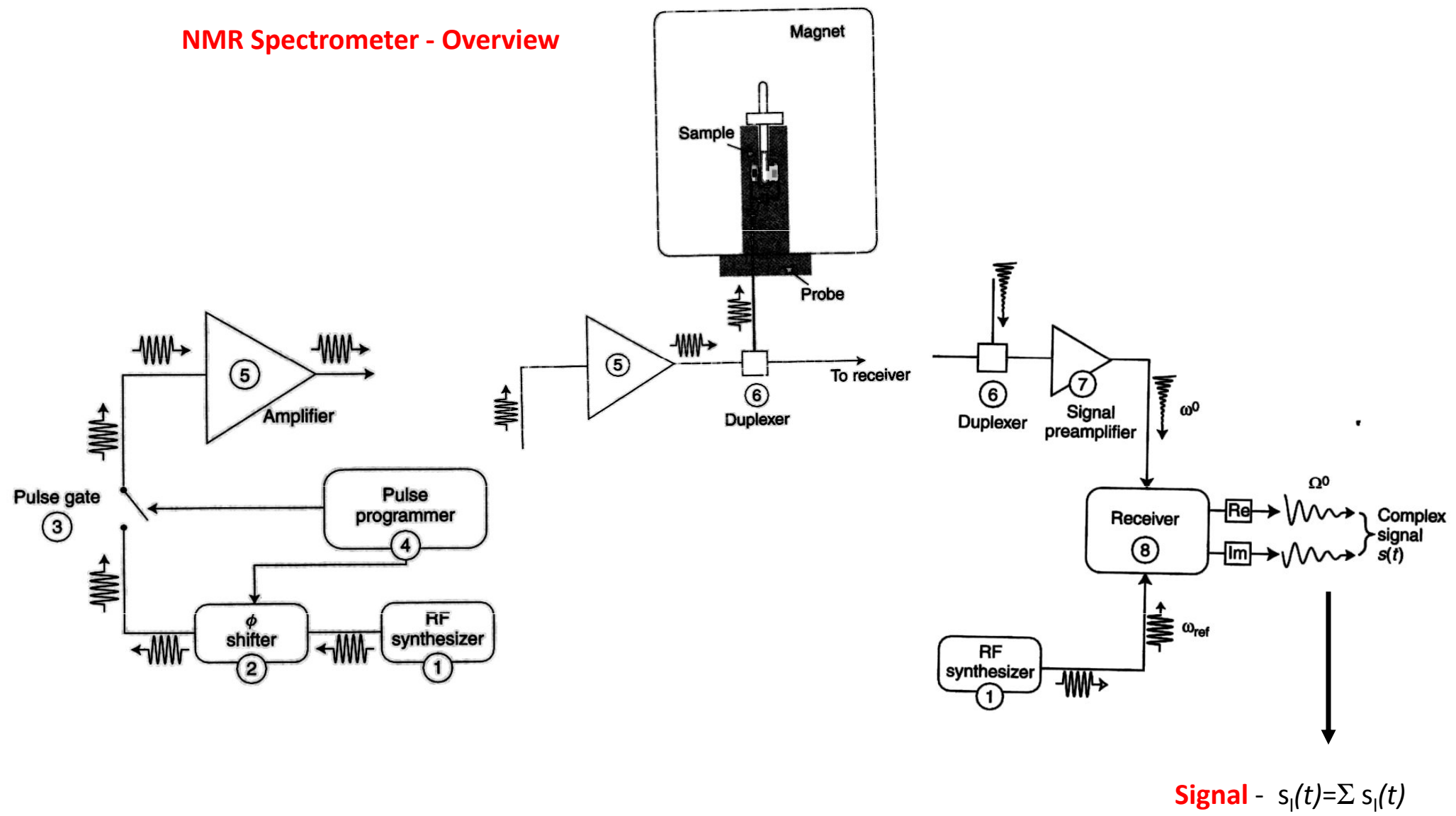
**CBU**  
**Control board**  
**unit**  
**FGU**  
**Frequency**  
**gen. u.**  
**Shimms**



**Temperature**  
**Unit**  
**AcquisitionCon**  
**troler**  
**Transmitter**

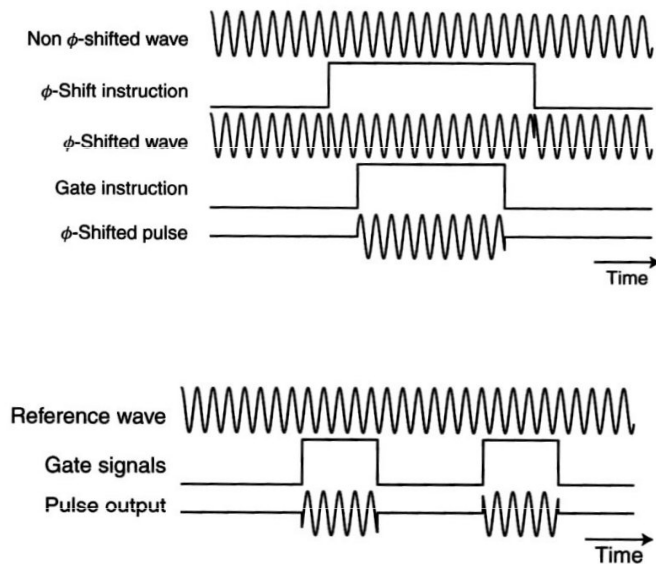


# NMR Spectrometer - Overview



**Signal** -  $s_i(t) = \sum s_i(t)$

## NMR radiofrequency pulse



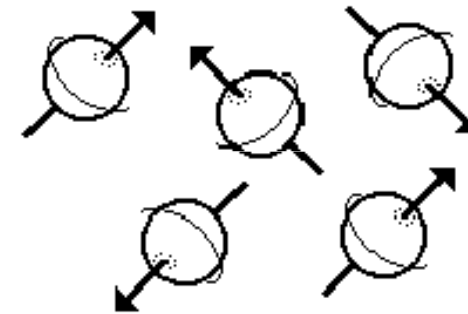
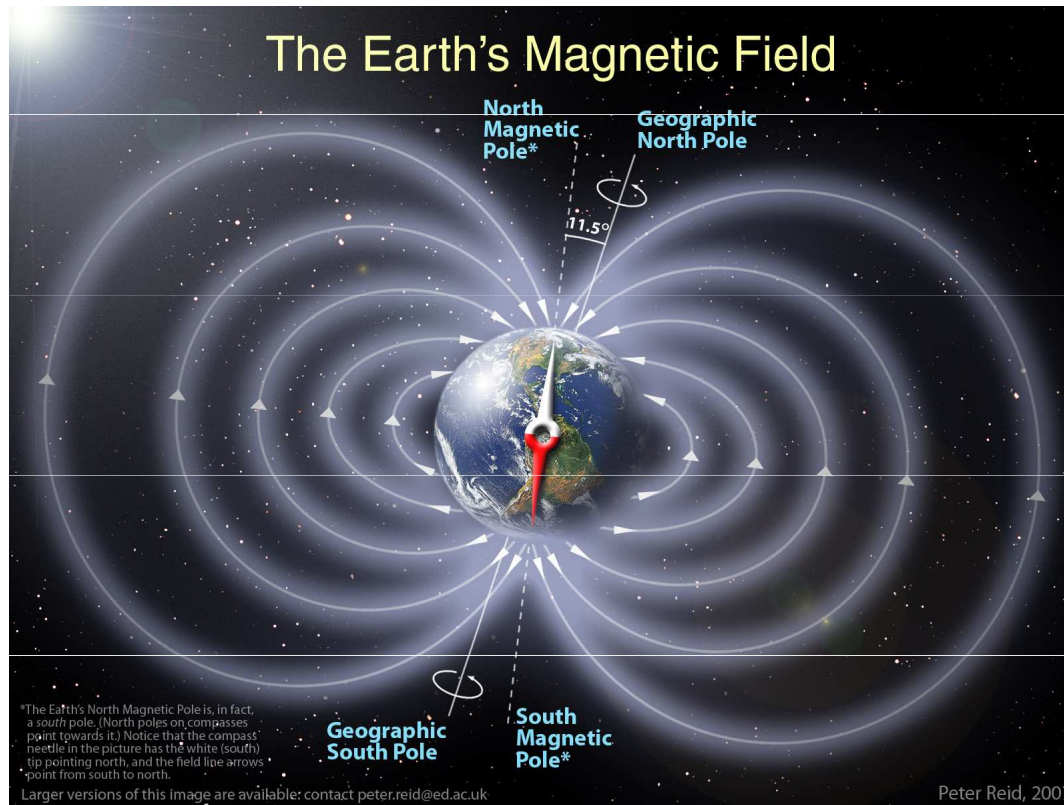
Pulzy:

- a) tvrdé – 7-30  $\mu\text{s}$ @-3~+3dB
- b) selektivní – ms~s@>30db
- c) adiabatické

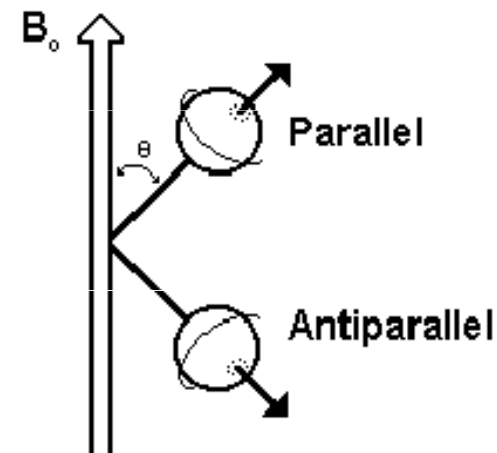
R.f. phase	Jargon
$\phi = 0$	'x-pulse'
$\phi = \pi/2$	'y-pulse'
$\phi = \pi$	'x-pulse' or '-x-pulse'
$\phi = 3\pi/2$	'y-pulse' or '-y-pulse'

For NMR, nuclear spin is needed!!!

Spin analogy to a compass needle

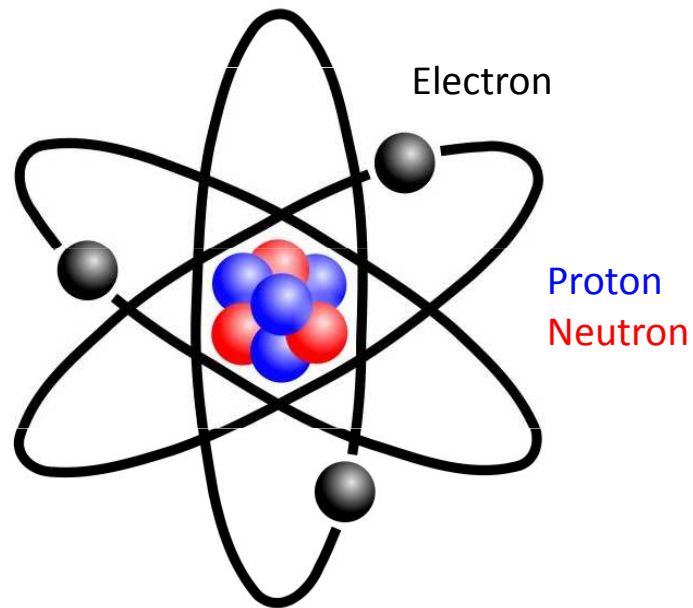


magnetic field = 0

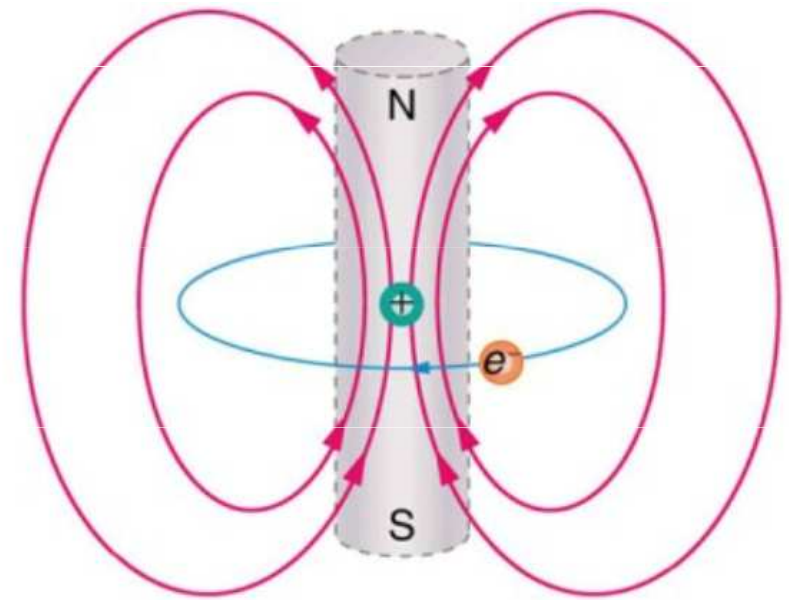


magnetic field > 0

# Atom



=

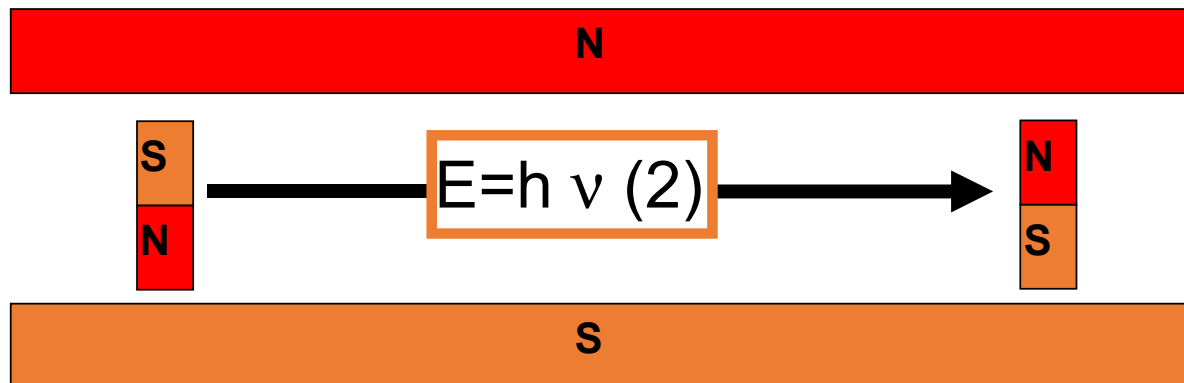


In the planetary model of the atom, an **electron orbits a nucleus**, forming a closed-current loop and **producing a magnetic field** with a north pole and a south pole.

Molecule is hence a group of small magnetic fields and each atom within the molecule experiences different local magnetic field.

# NMR - Refresh

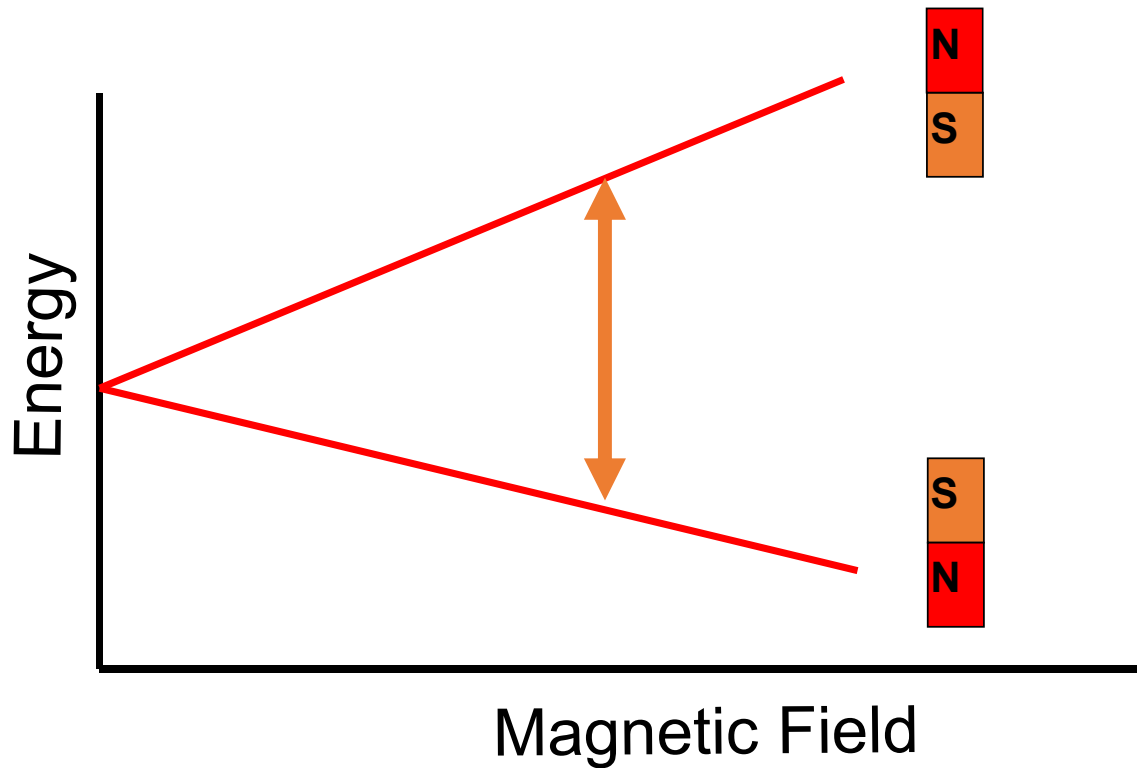
- 1) nuclear spin  $\neq 0$  ( $^1\text{H}$ ,  $^{13}\text{C}$ ,  $^{15}\text{N}$ ,  $^{31}\text{P}$ )
  - number of neutrons **and** the number of protons **both even**  $\Rightarrow$  **NO nuclear spin**
  - number of neutrons **plus** the number of protons **odd**  $\Rightarrow$  **half-integer spin** (i.e.  $\frac{1}{2}$ ,  $\frac{3}{2}$ ,  $\frac{5}{2}$ )
  - number of neutrons **and** the number of protons **both odd**  $\Rightarrow$  **integer spin** (i.e. 1, 2, 3)
- 2)  $\nu = \gamma B$  (1) - when placed in a magnetic field of strength **B**, a nuclei with a net spin can absorb a photon, of frequency  $\nu$ . The frequency  $\nu$  depends on the gyromagnetic ratio,  $\gamma$  of the nuclei
- 3) from quantum mechanics we know that nucleus with spin **I** can have **2I + 1** orientations  $\Rightarrow$  **nuclei with a spin  $\frac{1}{2}$**  can have **two orientations in** an external magnetic field – **low / high energy**



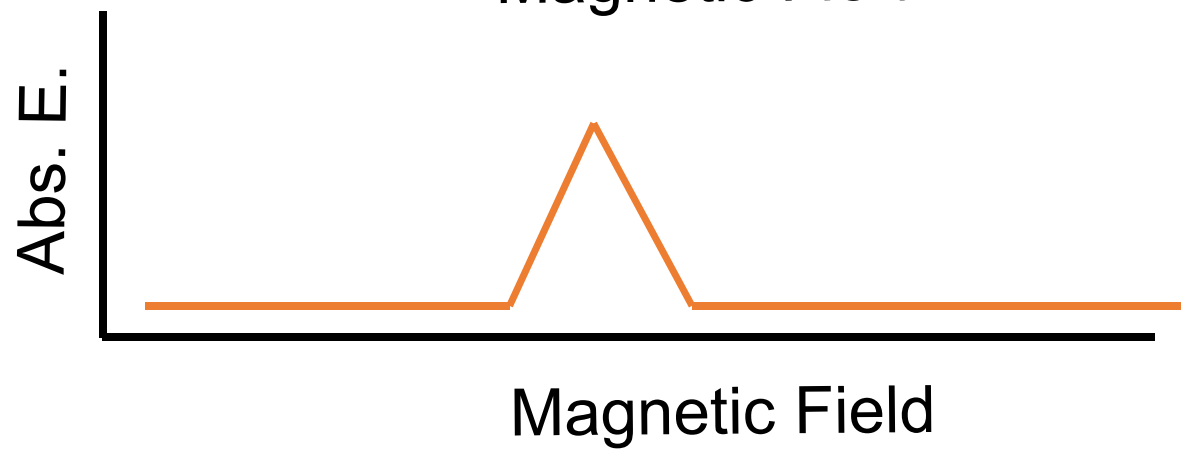
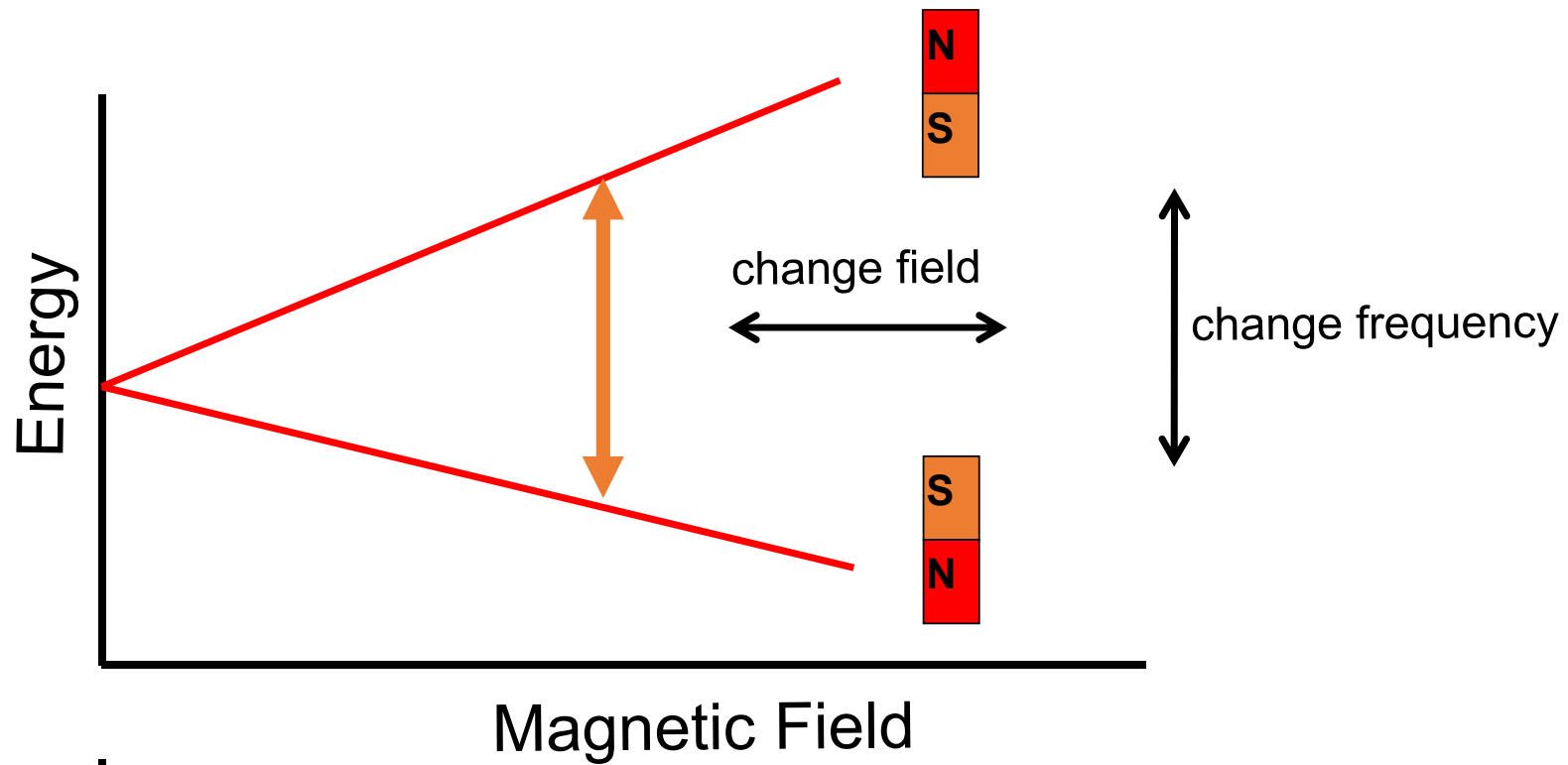
# *Nuclear Magnetic Resonance*

## Refresh

From (1) and (2):  $E = h \gamma B$







# CW vs. Fourier transform NMR

## Problem of NMR

the magnitude of the energy changes in NMR spectroscopy small  $\Rightarrow$  **sensitivity is a major limitation**

## Solution I.

increase sensitivity by recording many spectra, and then add them together; because **noise is random**, it adds as the square root of the number of spectra recorded.

**For example**, if **100** spectra of a compound were recorded and summed, then the **noise would increase** by a factor of **10**,

**but** the **signal would increase** in magnitude by a factor of **100**  
 $\Rightarrow$  large increase in sensitivity.

**However**, if this is done using a **CW-NMR**, the time needed to collect the spectra is very large (one scan takes **2 - 8** minutes).

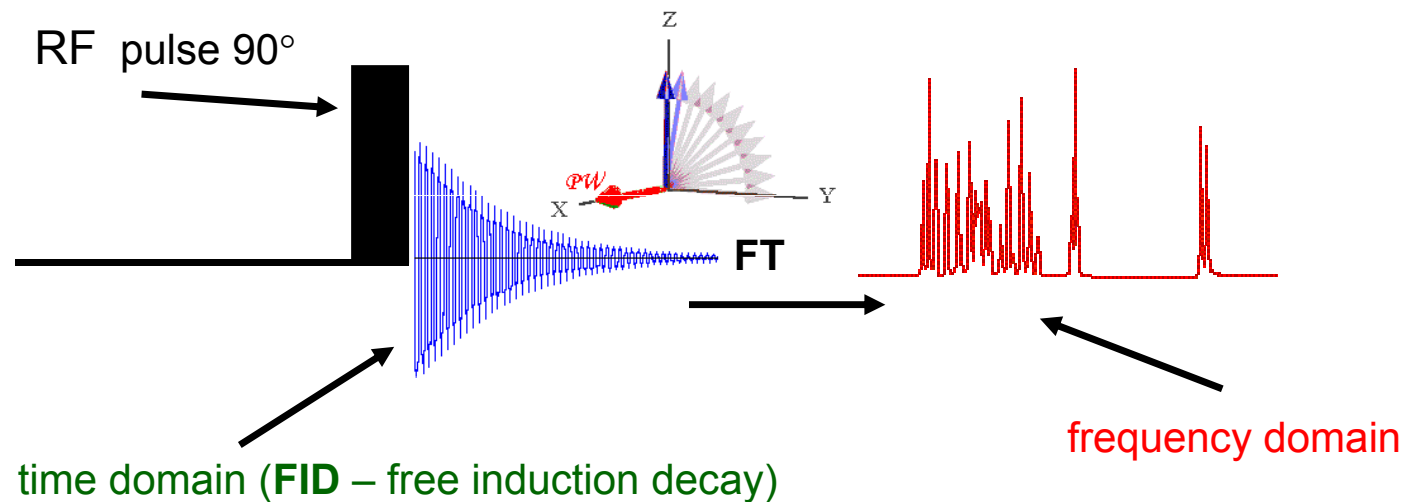
# CW vs. Fourier transform NMR

## Solution II.

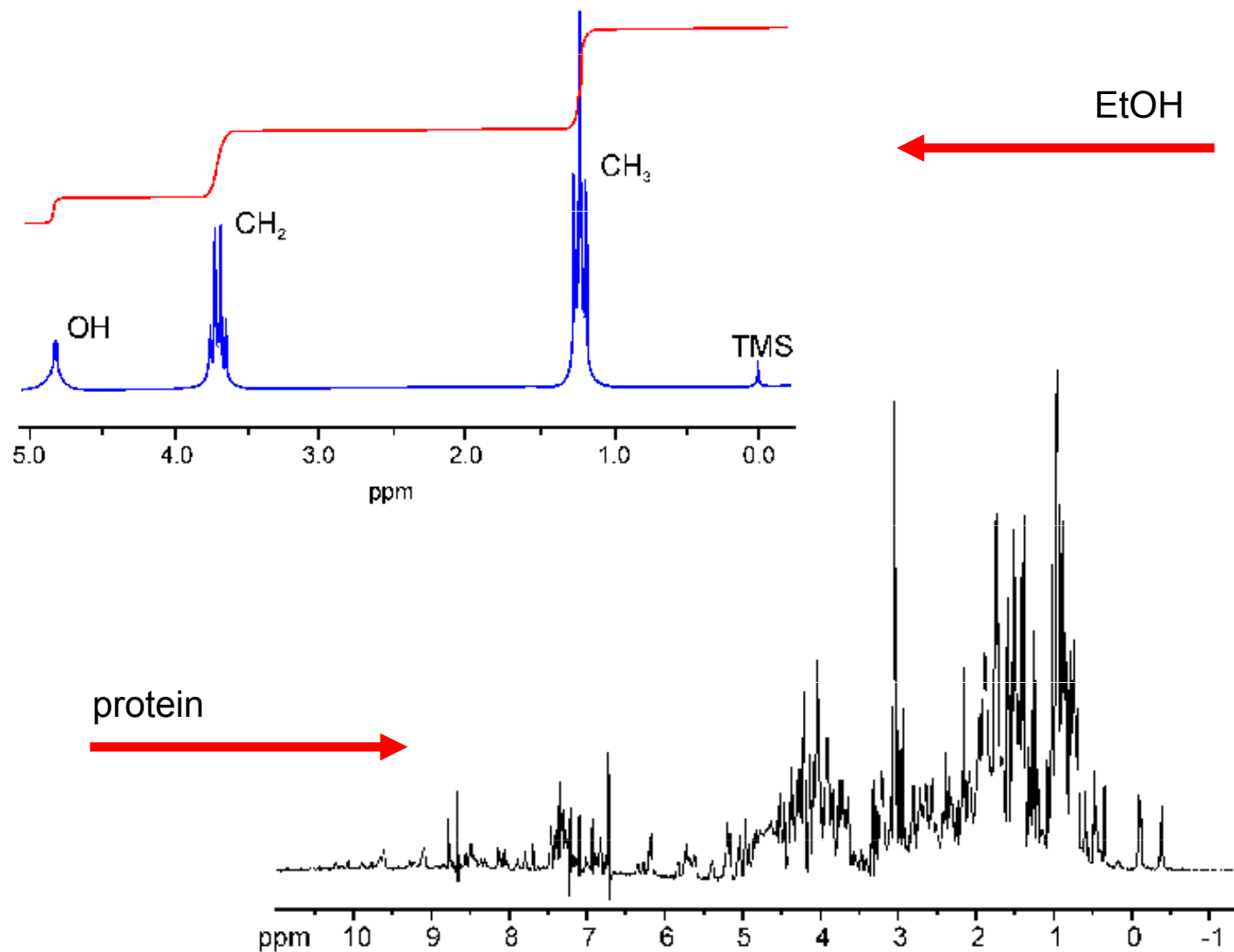
FT-NMR  $\Rightarrow$  **all frequencies** in a spectrum are **irradiated simultaneously** with a radio frequency pulse.

Following the pulse, the nuclei return to thermal equilibrium. A **time domain** emission signal is recorded by the instrument as the nuclei relax.

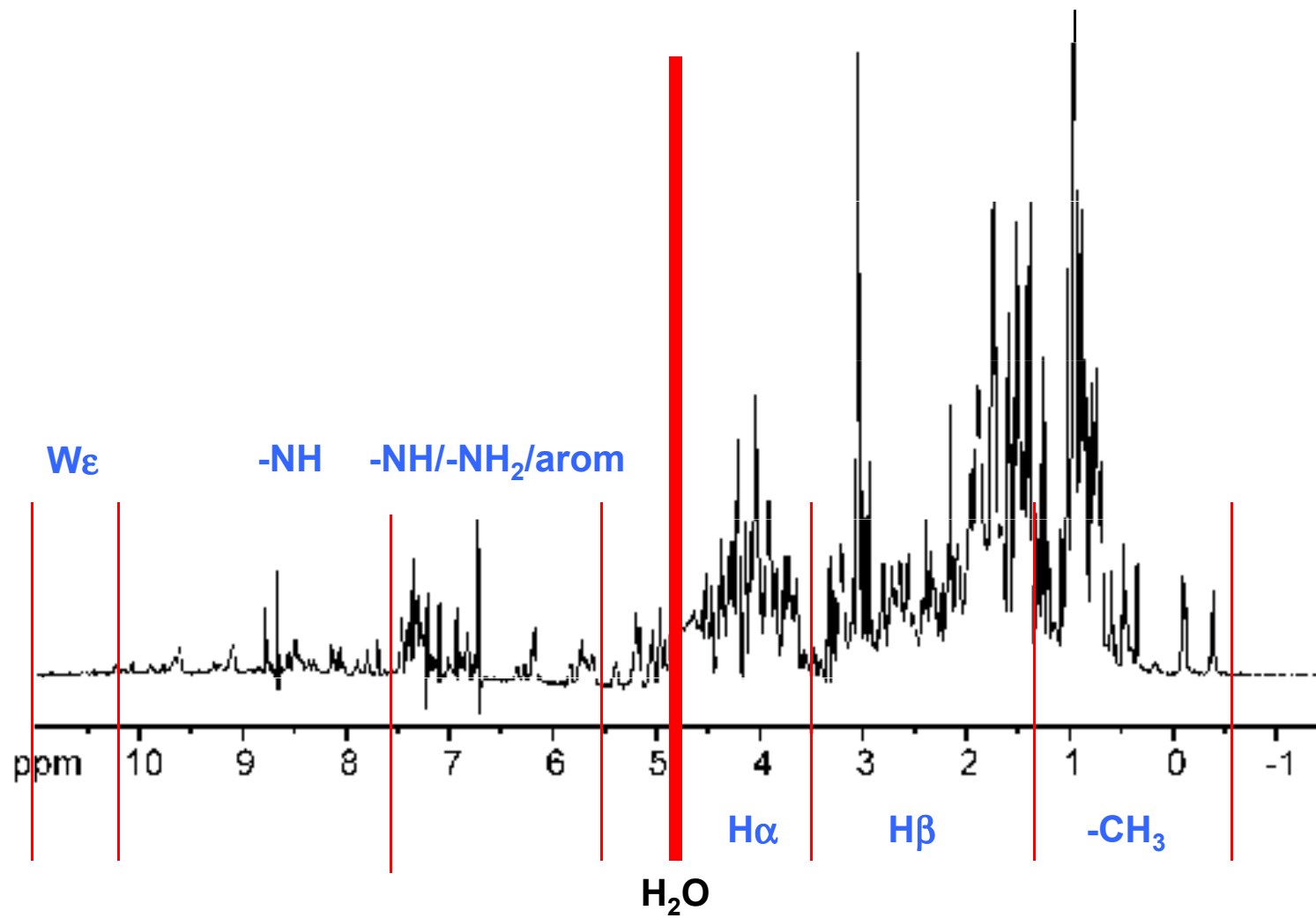
A **frequency domain** spectrum is **obtained by Fourier transformation**.



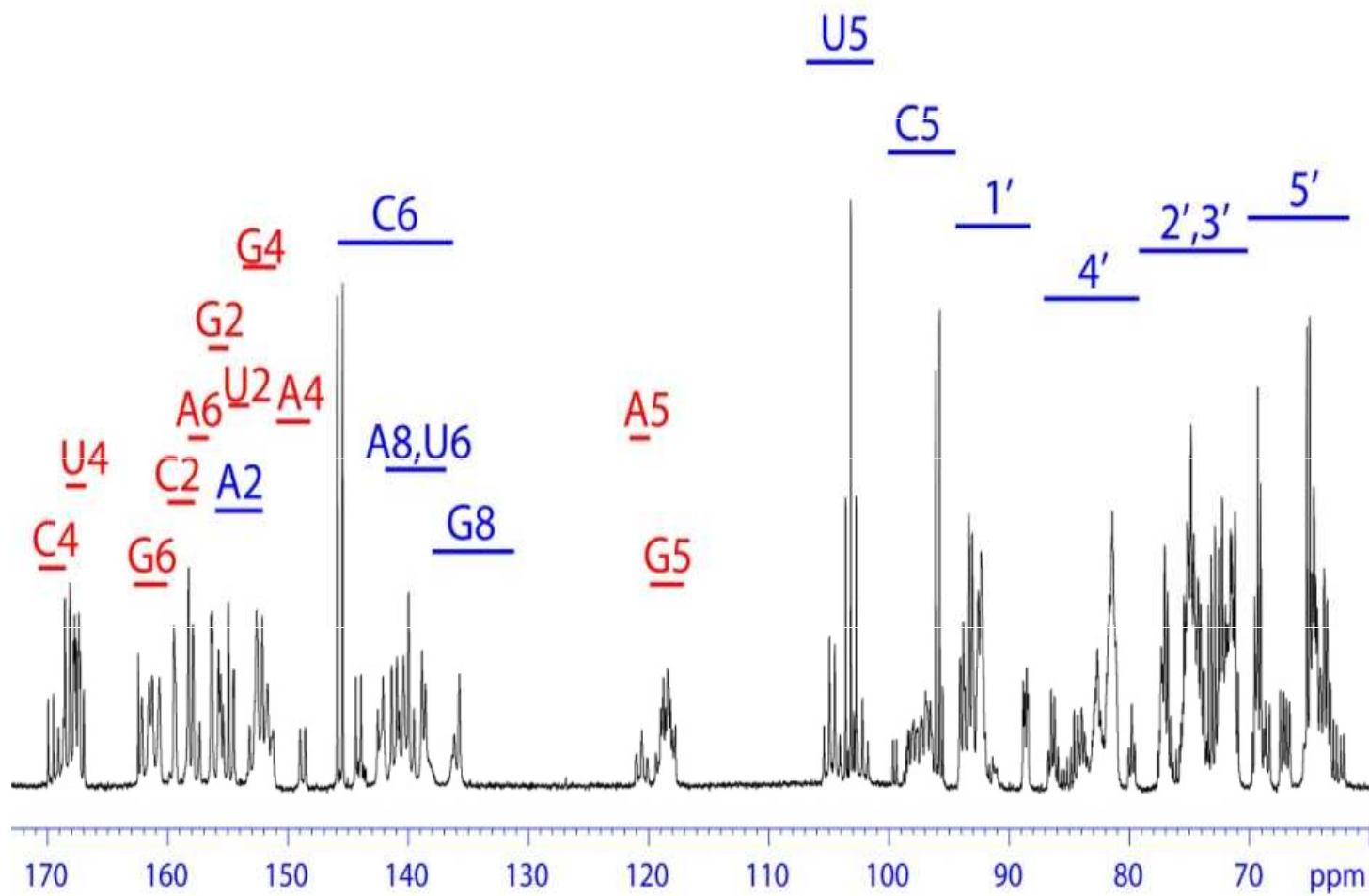
Each proton = 1 NMR signal



Each (non-exchangeable) proton = 1 NMR signal



Each (non-exchangeable) proton = 1 NMR signal





### Size



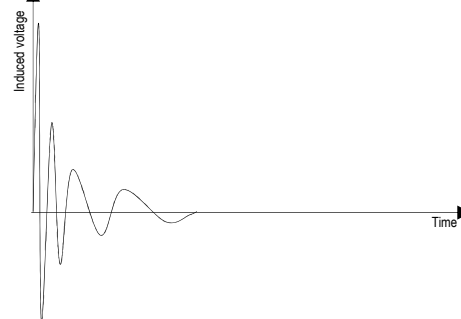
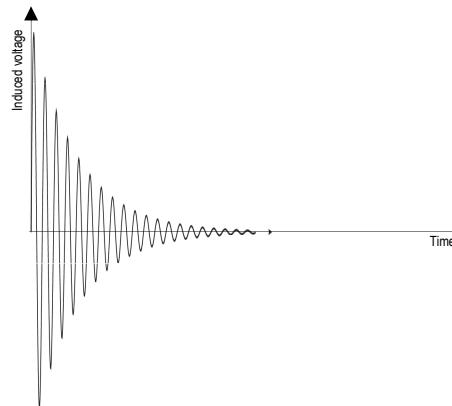
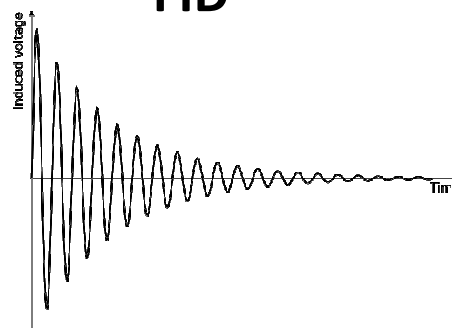
### Relaxation

slow (i.e. long  $t_2$  time)

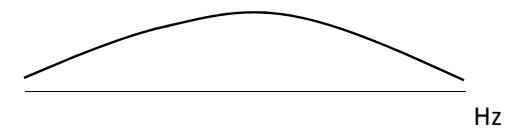
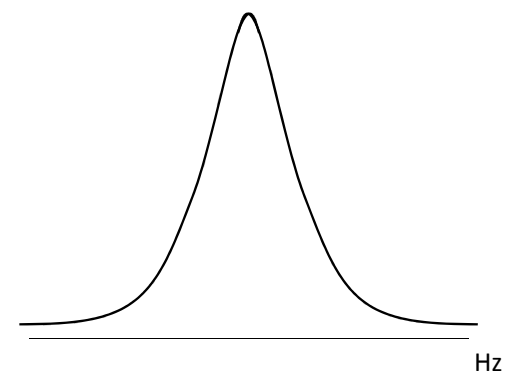
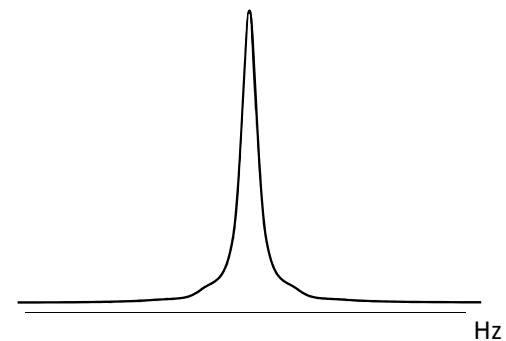
medium

fast

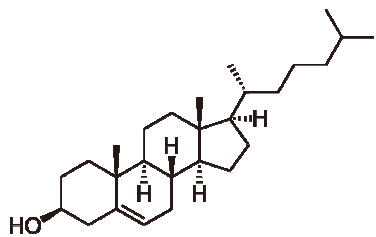
### FID



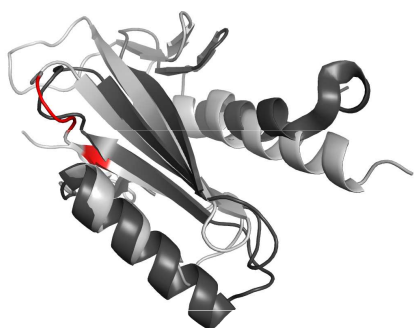
### NMR line(width) after FT



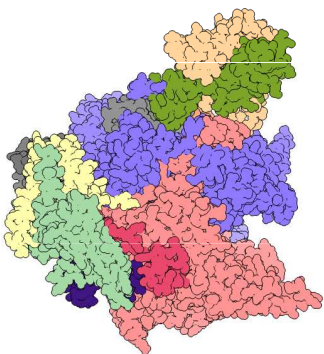
## Size



e.g. Cholesterol



Biomolecules 5-30 kDa



Large molecules 50+ kDa

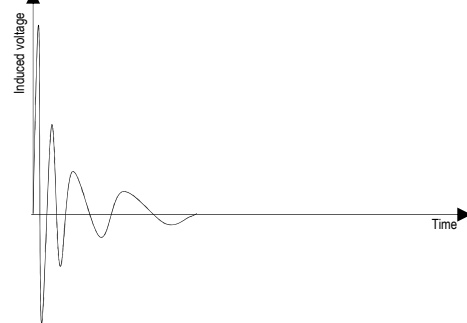
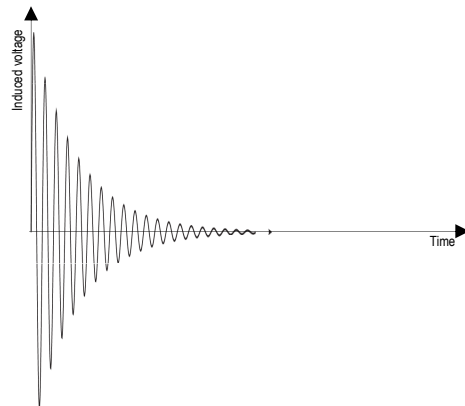
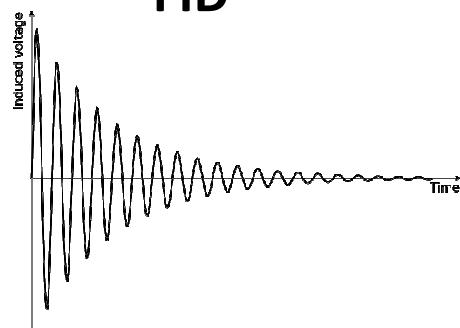
## Relaxation

slow (i.e. long  $t_2$  time)

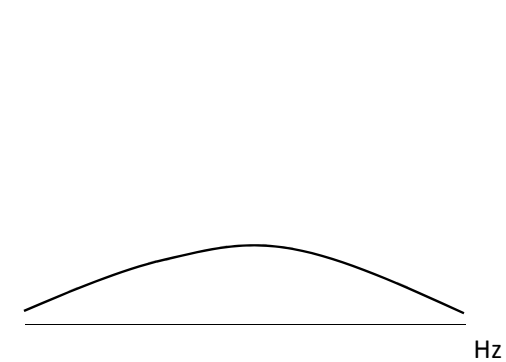
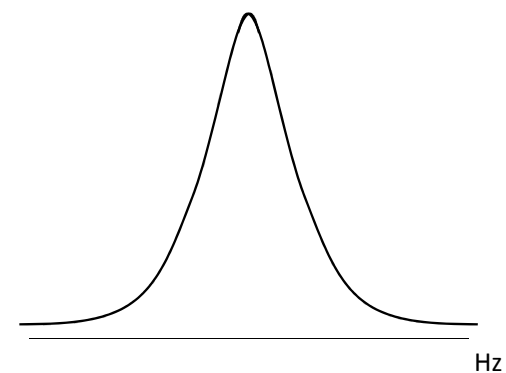
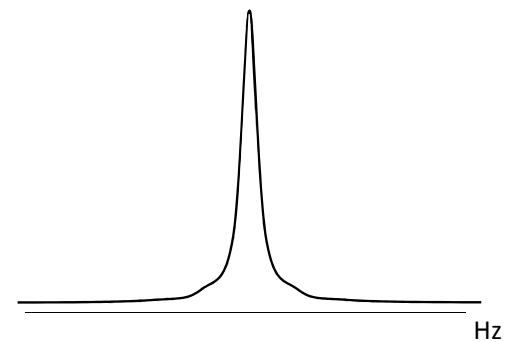
medium

fast

## FID

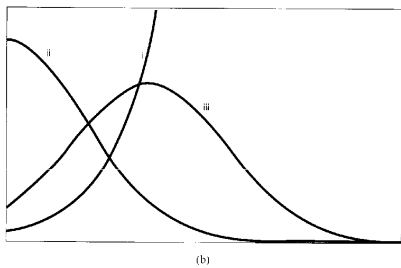
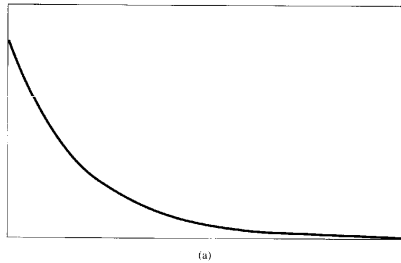


## NMR line(width) after FT



# **NMR data processing**

## NMR data processing



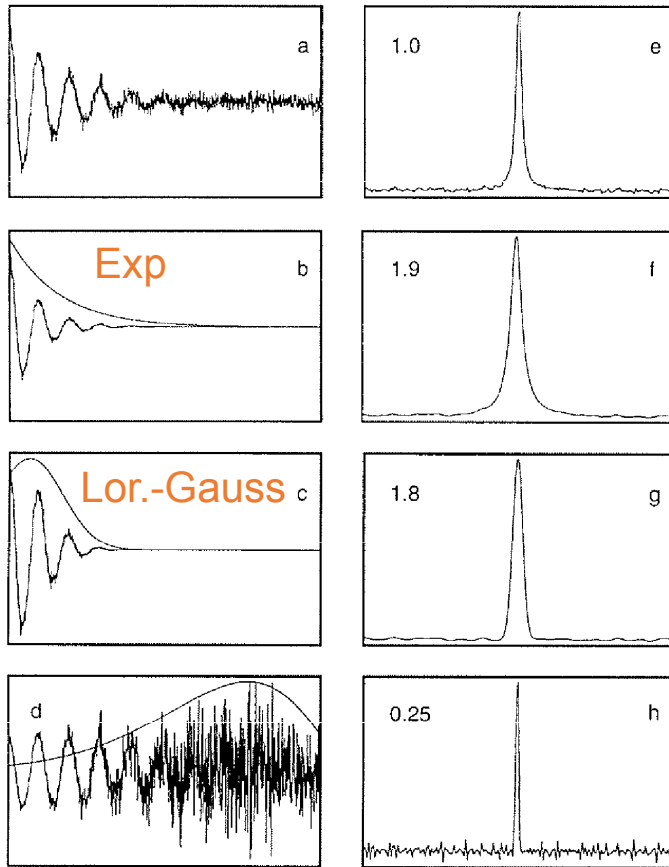
Window functions:

1) improvements of S/N ratio

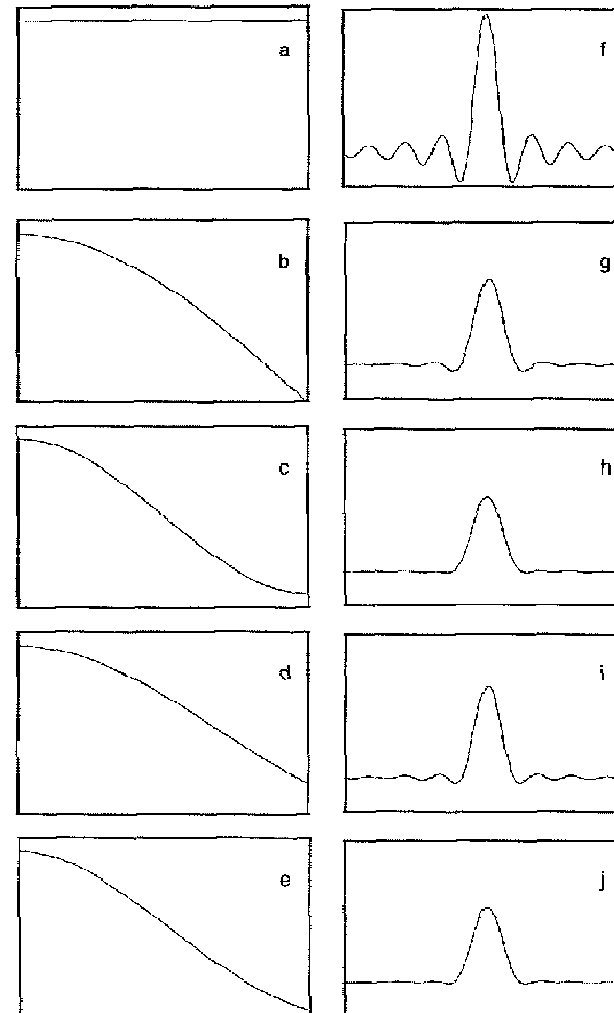
2) increasing resolution

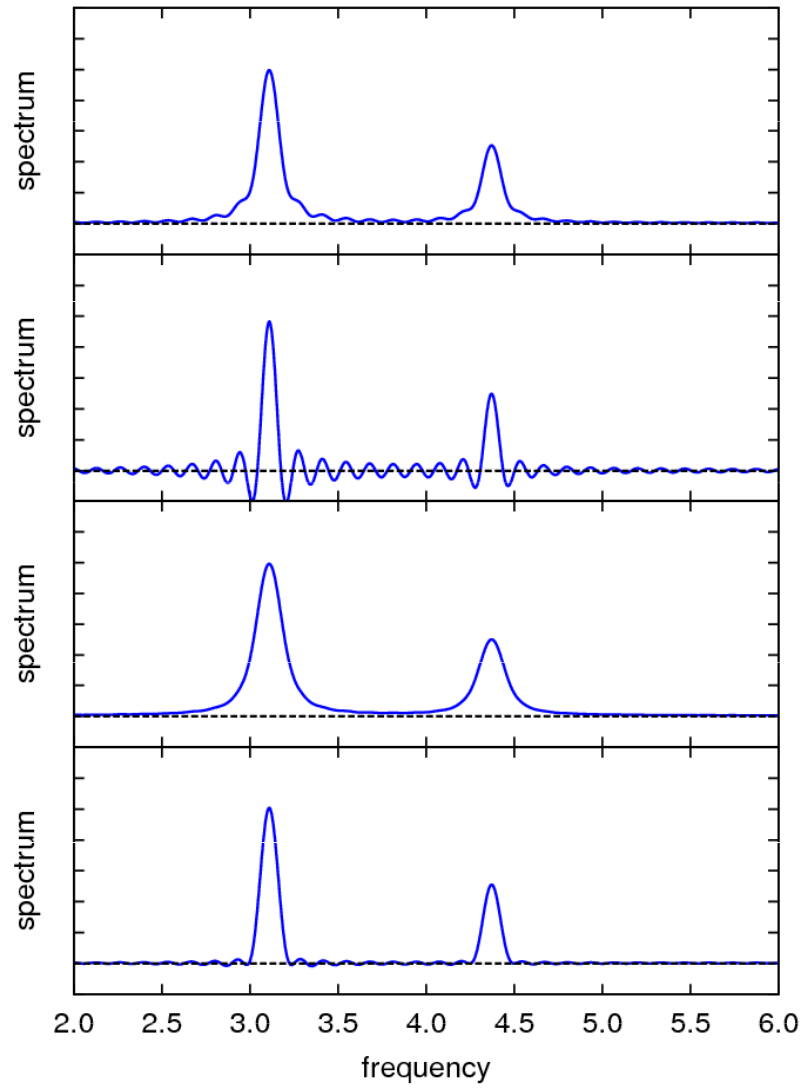
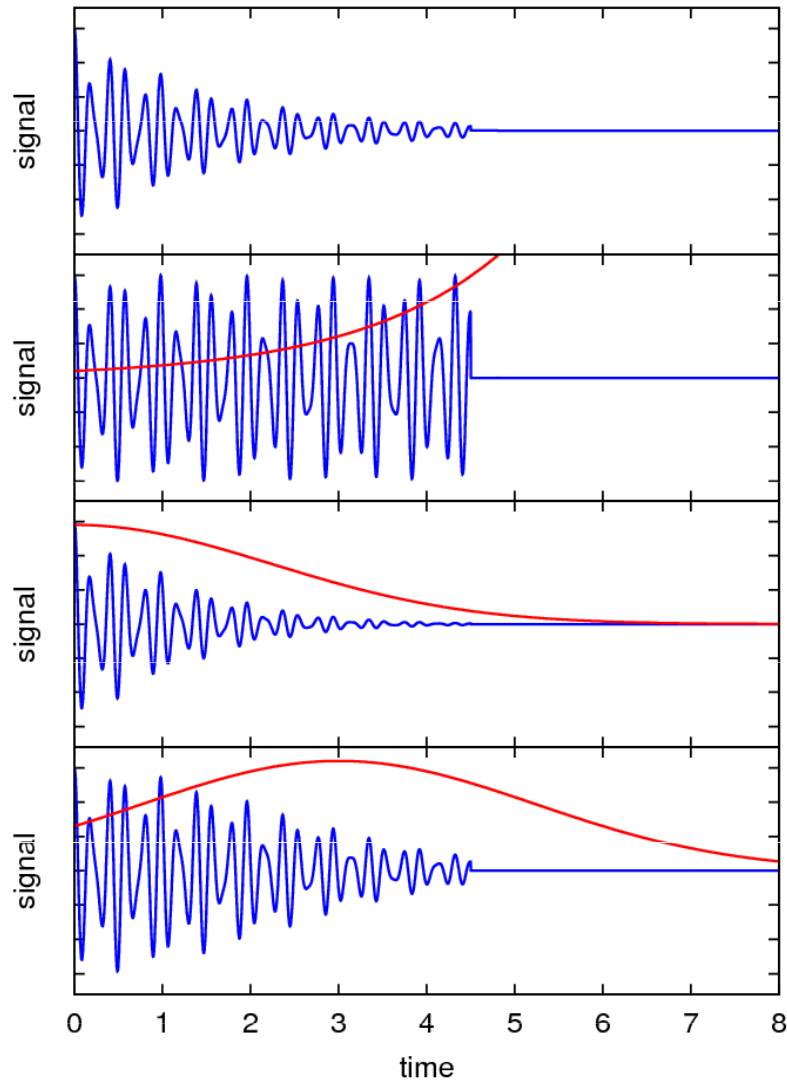
---

## NMR data processing – window functions – apodization



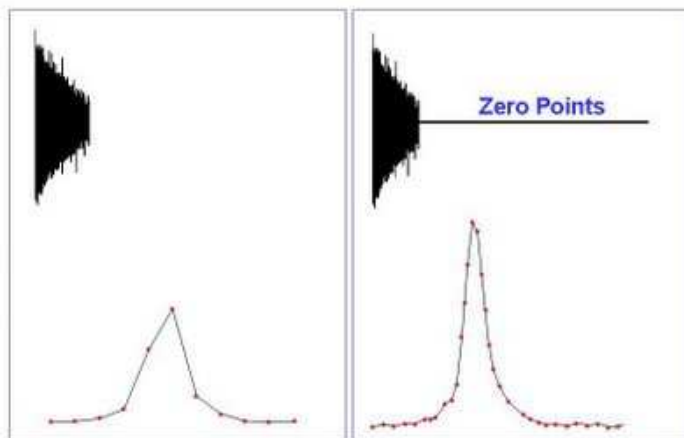
Kaiser w. function



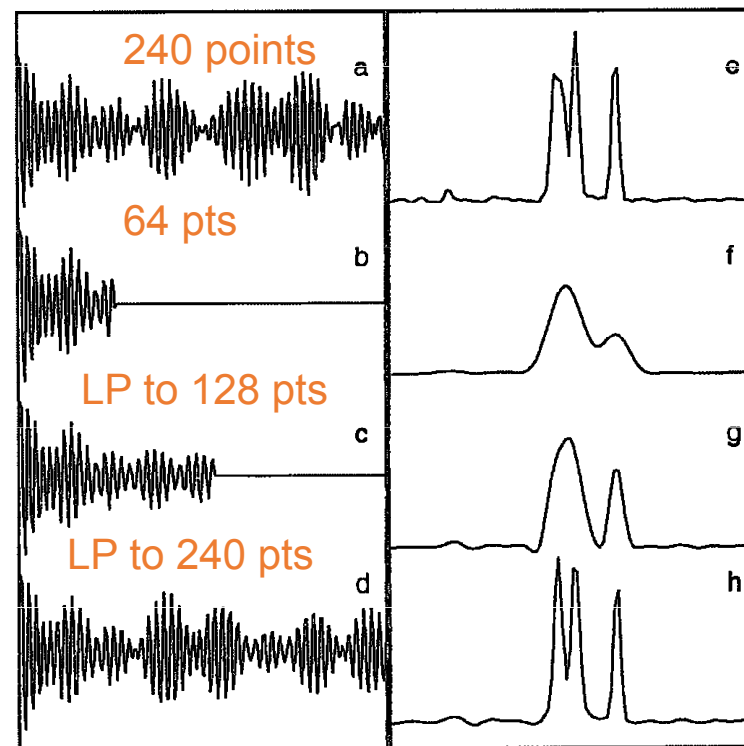


## NMR data processing – Zero Filling, Linear prediction

### Zero filling



### Linear prediction

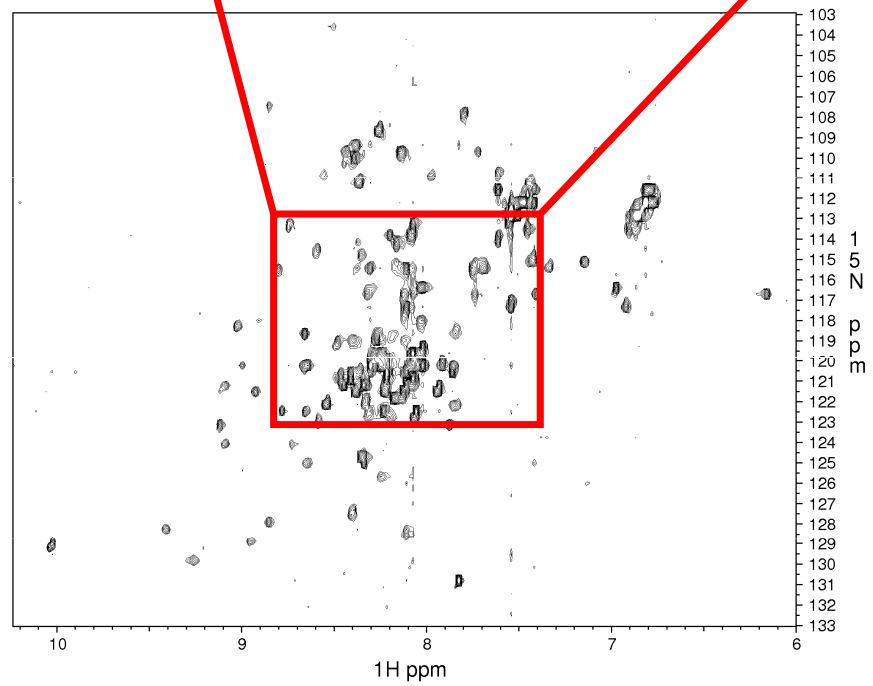
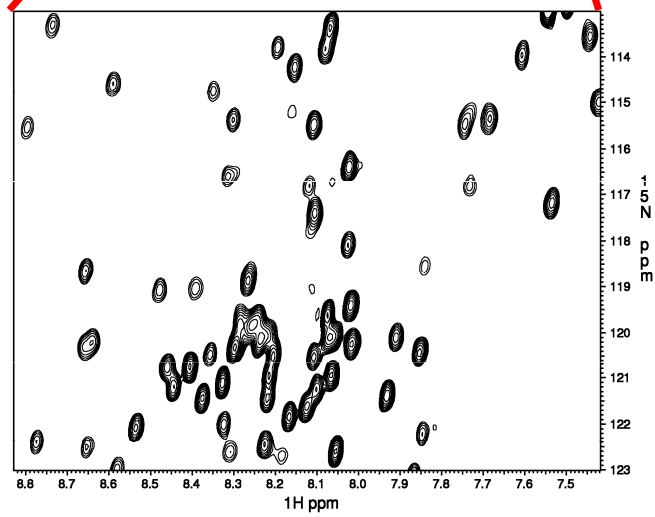
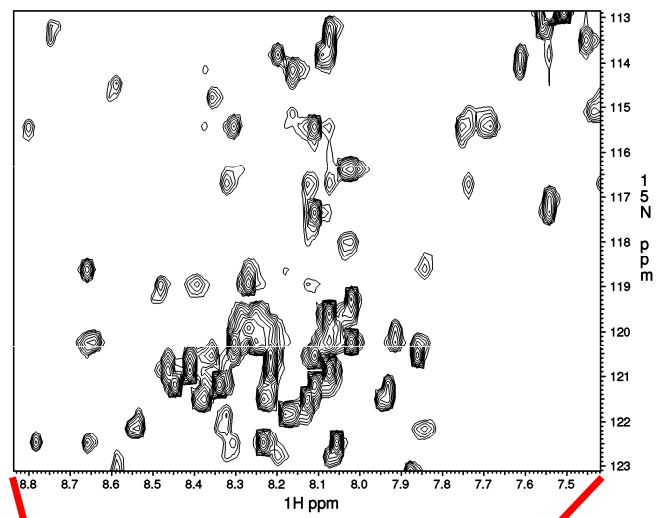
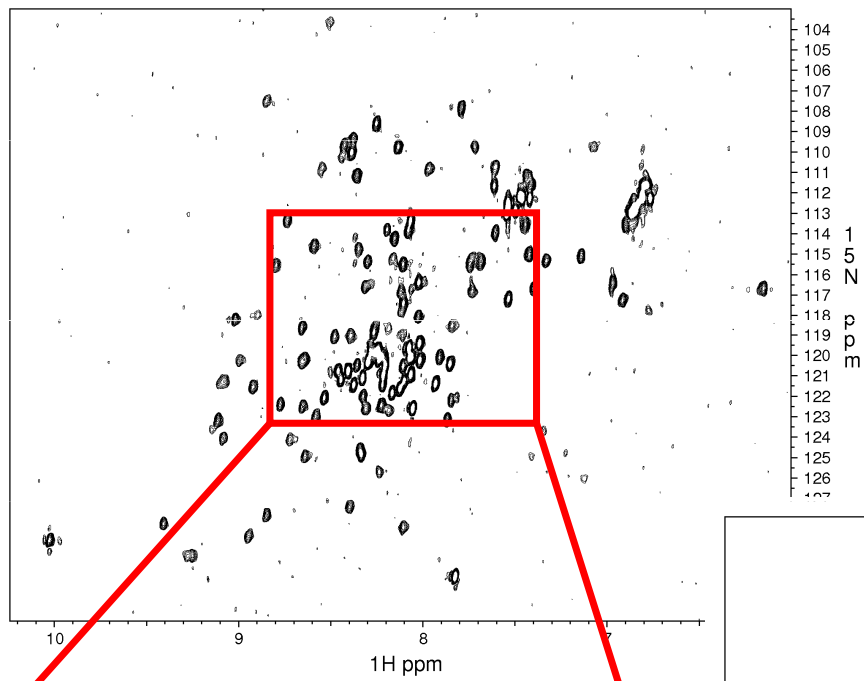


## NMR data processing - summary

- I) Solvent suppression
- II) Window function
- III) Zero-filling
- IV) FT
- V) Transpose (in case of multidimensional spectra)

```
|nmrPipe -fn POLY -time \  
|nmrPipe -fn SP -off 0.33 -end 0.98 -pow 2 -c 1.0 \  
|nmrPipe -fn ZF -size 2048 \  
|nmrPipe -fn FT -auto \  
|nmrPipe -fn PS -p0 -76.0 -p1 0.0 -ur \  
|nmrPipe -fn EXT -x1 11.0ppm -xn 6.0ppm -sw \  
|nmrPipe -fn POLY -ord 3 -auto \  
|nmrPipe -fn TP \  
F2
```





NMR as a tool for study **structure, dynamics** and **interactions** of biomolecules

- 1) Structure determination of NAs and proteins
- 2) **Protein – metal interaction**
- 3) **Protein – ligand interaction**

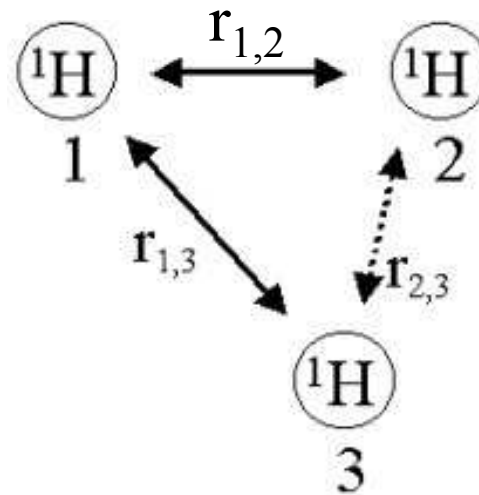
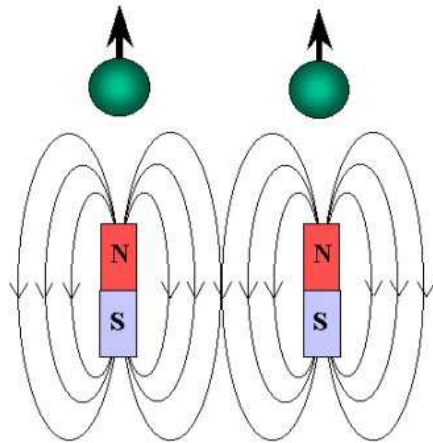
For most of the modern applications, enrichment by  $^{13}\text{C}$ ,  $^{15}\text{N}$  and often  $^2\text{H}$  needed!

Isotope	Ground state spin	Natural abundance [%]	Rel. Sensitivity
$^1\text{H}$	$\frac{1}{2}$	~100	$1.00 \times 10^{+0}$
$^{13}\text{C}$	$\frac{1}{2}$	1.10	$1.59 \times 10^{-2}$
$^{15}\text{N}$	$\frac{1}{2}$	0.37	$1.04 \times 10^{-3}$
$^{19}\text{F}$	$\frac{1}{2}$	100	$8.30 \times 10^{-1}$
$^{31}\text{P}$	$\frac{1}{2}$	~100	$6.63 \times 10^{-2}$
$^{12}\text{C}$	0	98.90	-
$^{16}\text{O}$	0	~100	-

# NMR as a tool for study **structure, dynamics and interactions** of biomolecules

- 0) AA/NA sequence, resonance assignment, standard chemical shifts
- 1) Structure determination of proteins/NAs
- 2) NMR can provide detailed information about the structure at the atomic level resolution relying on the spatial proximity of two interacting protons – nuclear Overhauser enhancement (**NOE**)
- 3) Additional structural information can be obtained (residual dipolar couplings – **RDCs**, *J*-couplings, backbone chemical shifts - **CSI**)

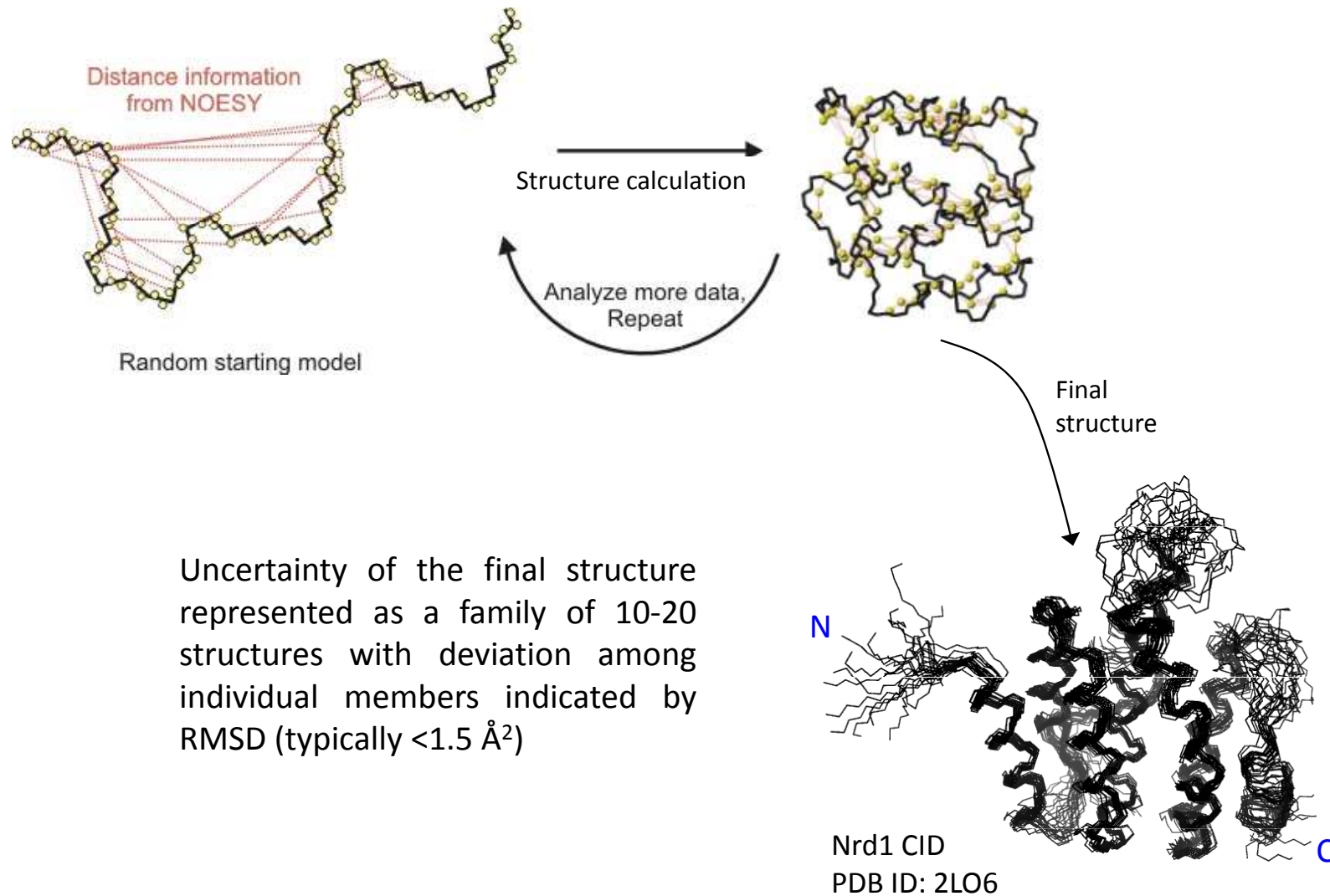
**NOE:**



$$r_{1,2}; r_{1,3}; r_{2,3} \leq 6 \text{ \AA}$$

$$1 \text{ \AA} = 1.10^{-10} \text{ m}$$

## Iterative procedure of structure determination by NMR

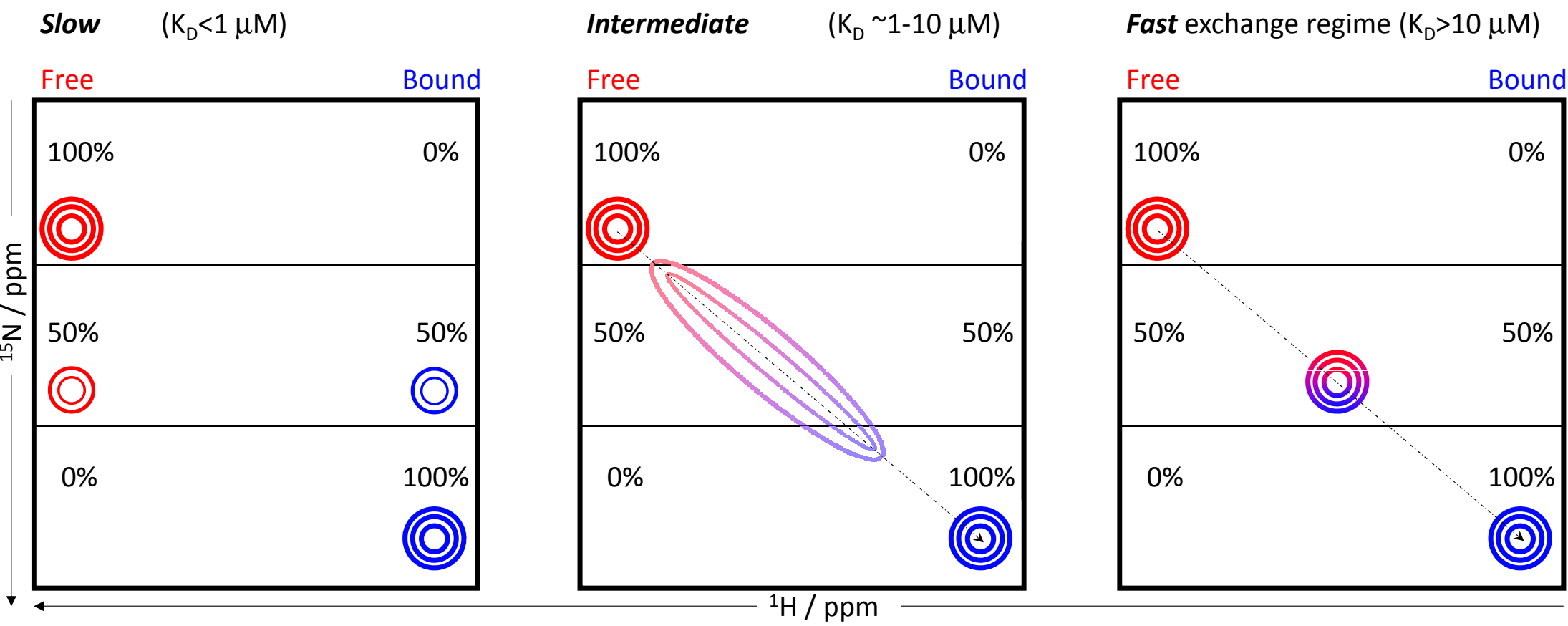


Uncertainty of the final structure represented as a family of 10-20 structures with deviation among individual members indicated by RMSD (typically  $<1.5 \text{ \AA}^2$ )

[http://www.fbreagents.com/basics\\_nmr/9proteins.htm](http://www.fbreagents.com/basics_nmr/9proteins.htm)

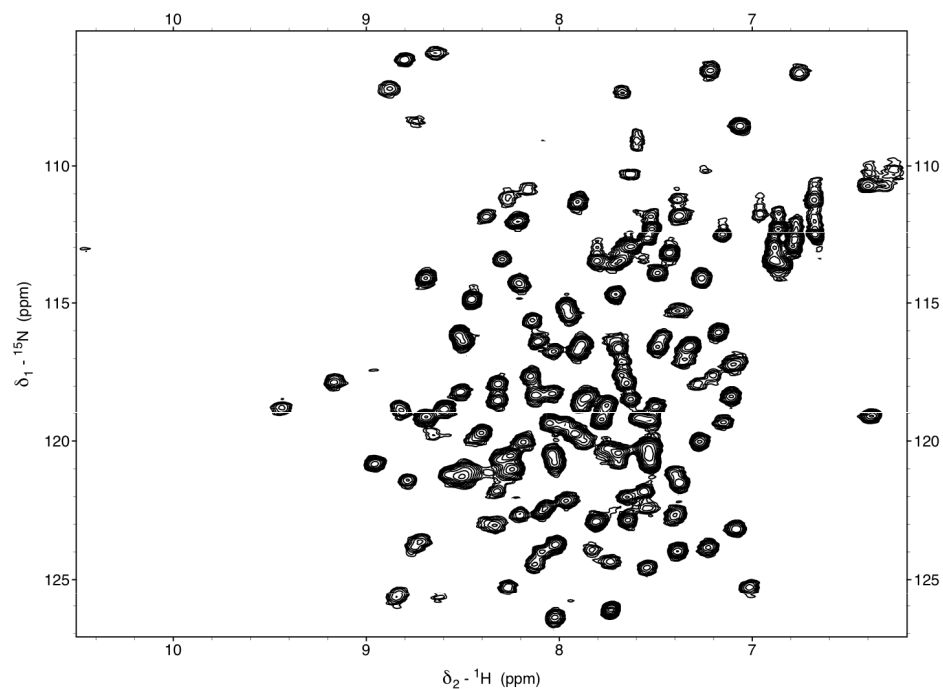
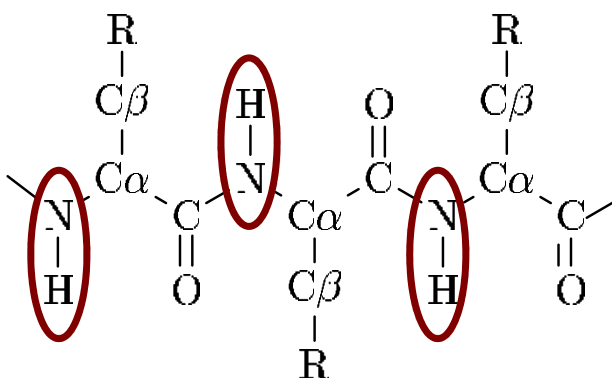
# Studying interactions by NMR titration

- 1) **Slow** exch. regime (on the NMR timescale) – individual peaks for each of the studied states (e.g. free / complexed forms of a protein), peak intensity representing population of a given state
- 2) **Intermediate** exchange regime
- 3) **Fast** exchange regime – single peak whose chemical shift position is given by the molar ratio of the states present in solution



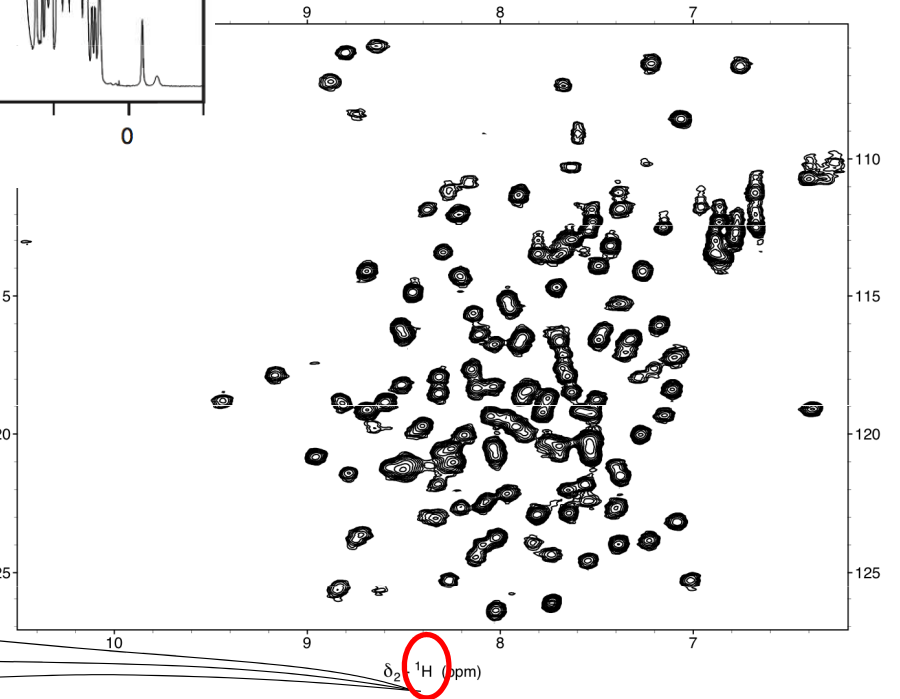
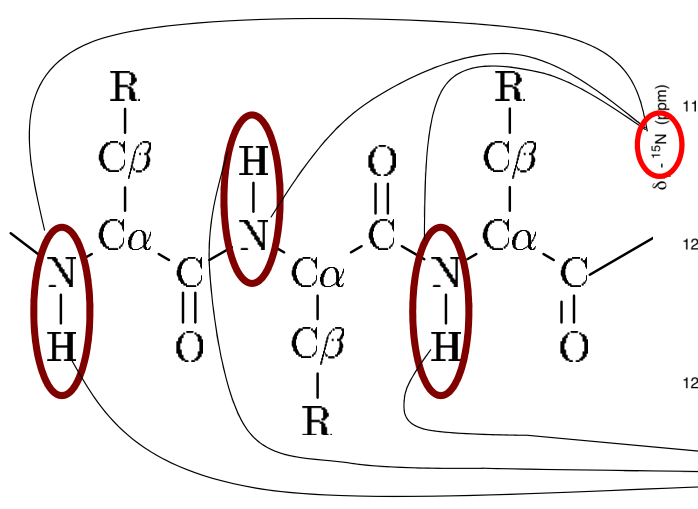
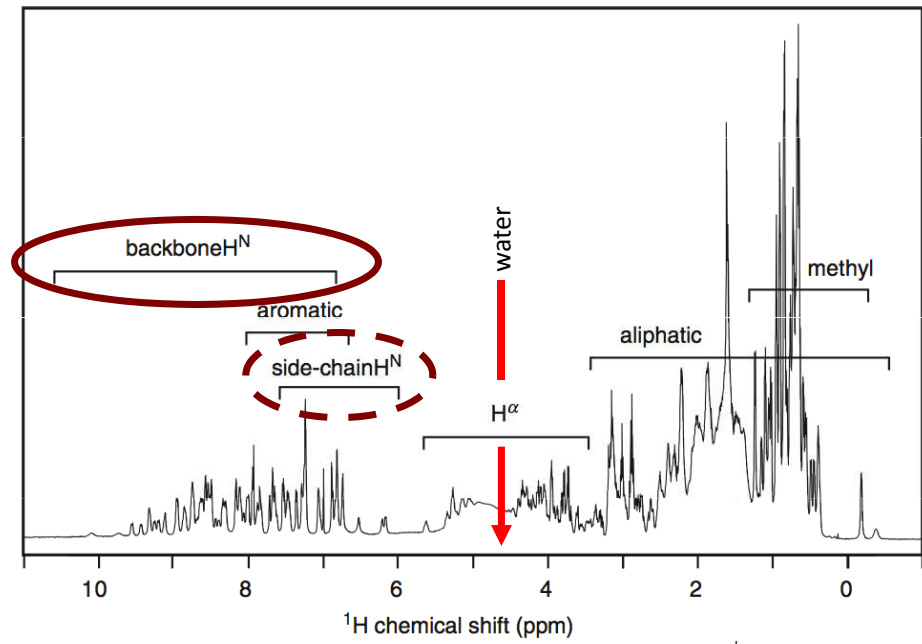
## $^{15}\text{N}$ - $^1\text{H}$ HSQC – Heteronuclear Single Quantum Coherence

- 1) 1 peak  $\cong$  1 amino acid
- 2) good estimate of the protein folding status
- 3) no information about sequential assignment (which peak is which amino acid)
- 4) for sequential assignment third dimension needed ( $^{13}\text{C}$ )
- 5) once assignment of the peaks known – HSQC is optimal tool for monitoring interactions by NMR through titrations (i.e. stepwise addition of small amounts of ligand to the nearly constant volume solution with the isotopically enriched molecule)



$^1\text{H}$ - $^{15}\text{N}$  HSQC, cca 155 aa, well folded, 600MHz, 293K

$^1\text{H}$  1D, Cavanagh et al., 2007



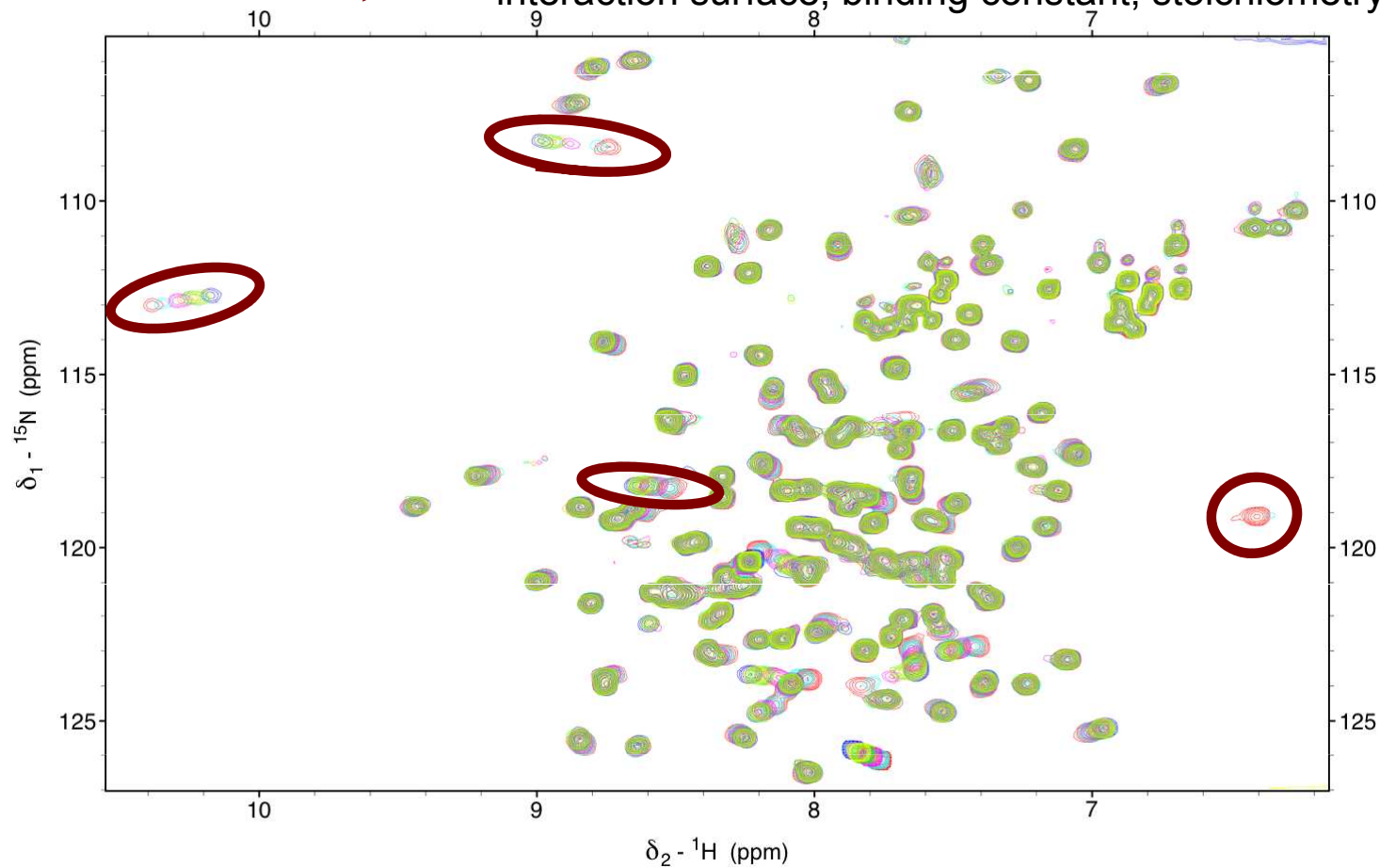
$^1\text{H}$ - $^{15}\text{N}$  HSQC, cca 155 aa, well folded, 600MHz, 293K



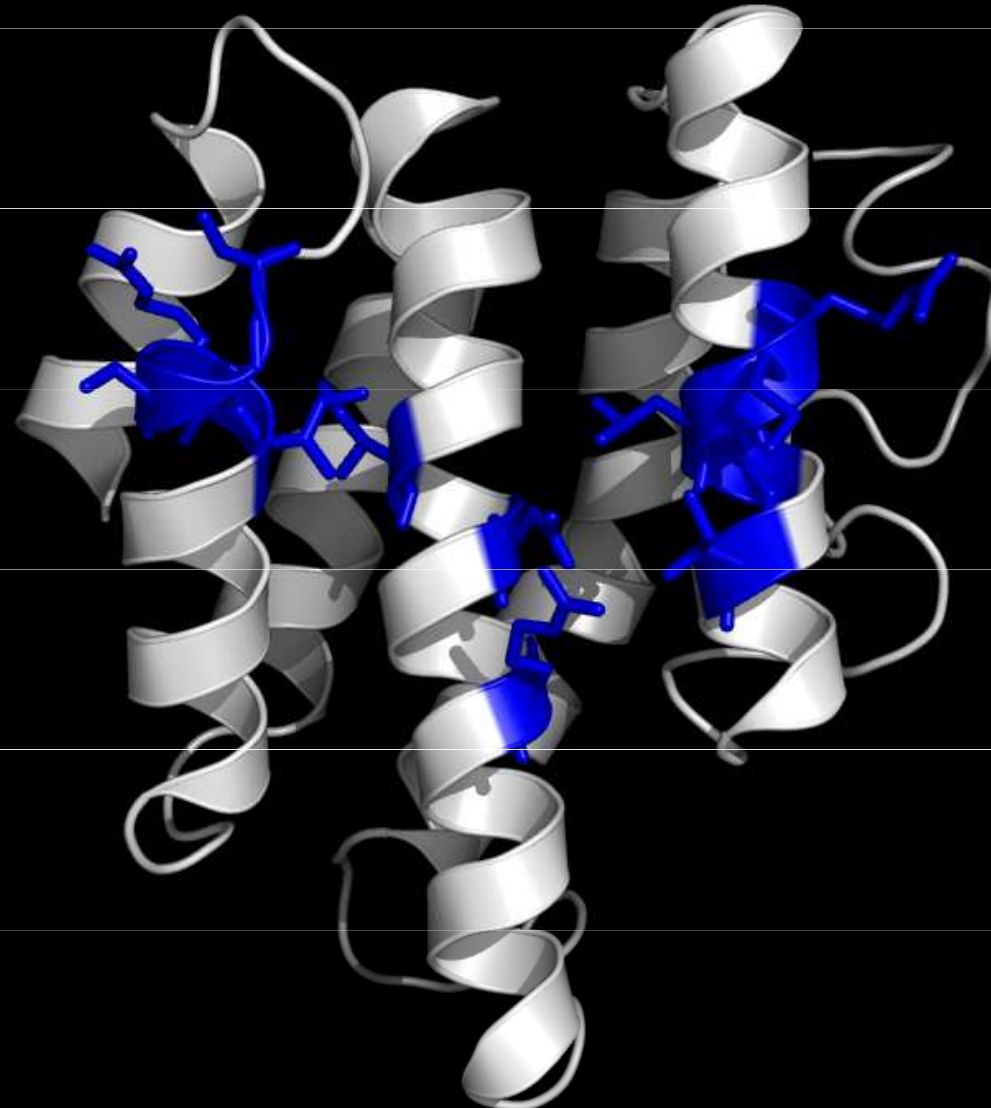
# Interaction of Nrd1-CID with C-terminal domain (CTD)

**NMR Titration** -  $^{15}\text{N}$  enriched CID + unlabeled CTD-Ser5P in  $n$ -steps,  $n=6$  in our case

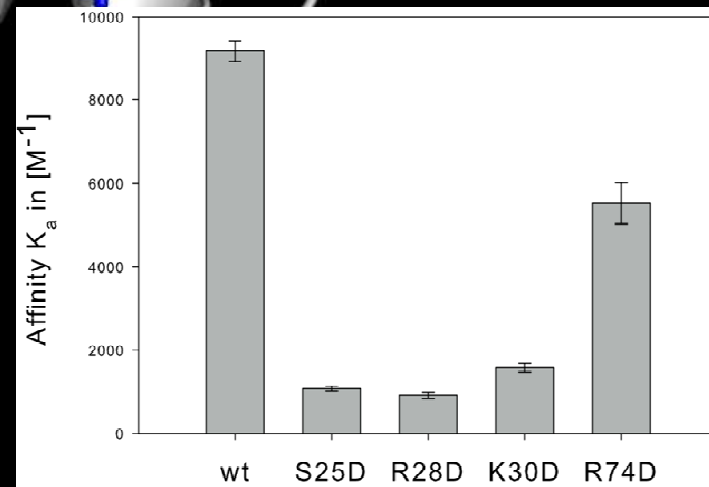
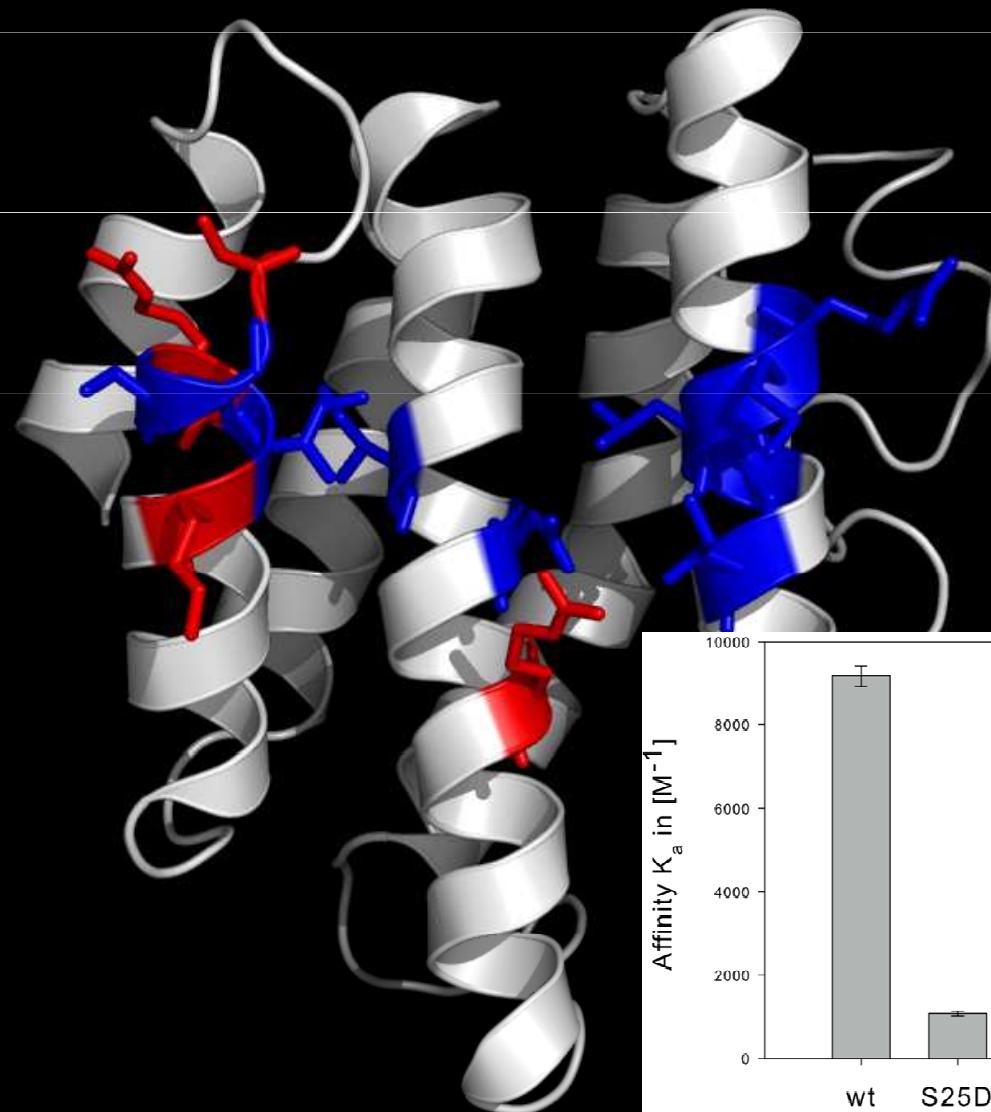
- peaks corresponding to the interacting residues of CID change their chemical shift (position in the spectrum)
- => interaction surface, binding constant, stoichiometry



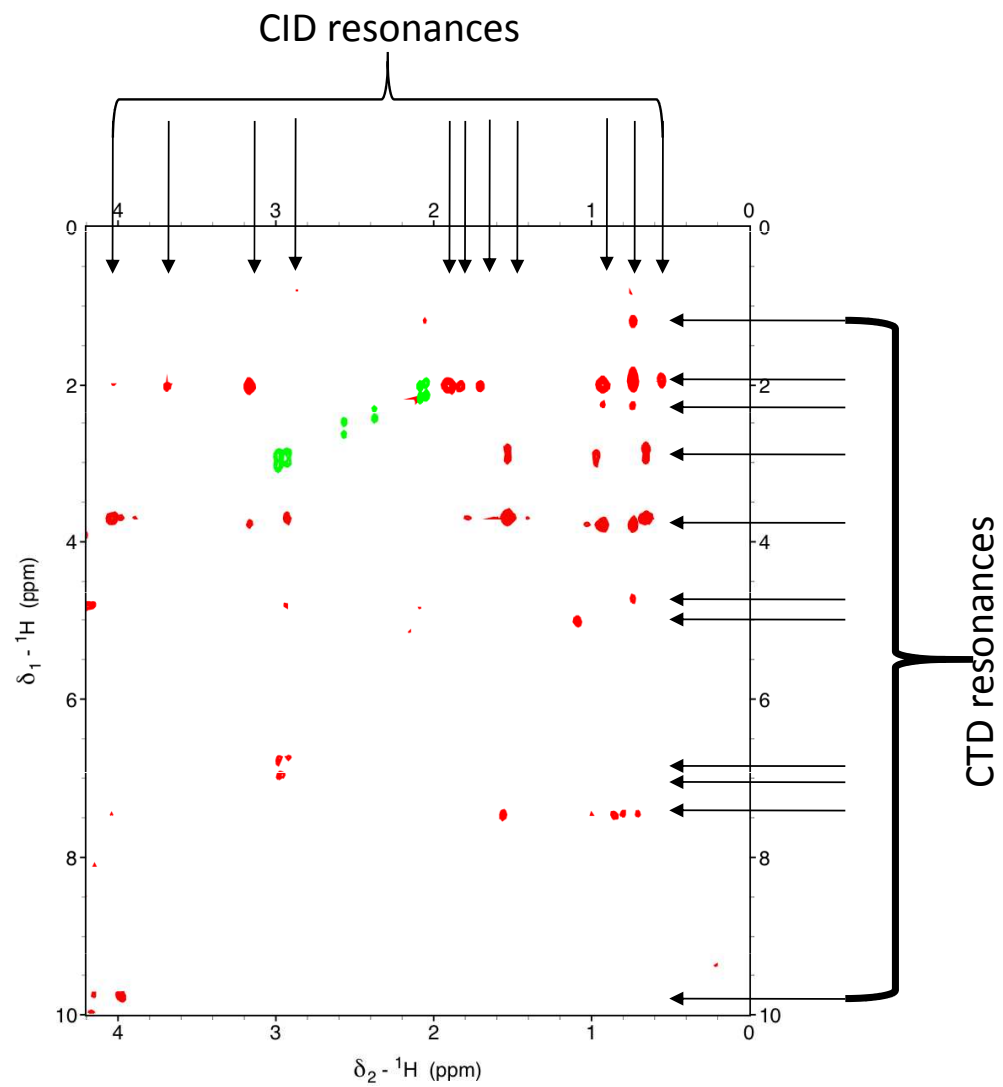
**Nrd1 CID interaction surface** — CID residues experiencing the largest chemical shift variations upon the interaction with 5-phospho-Ser CTD shown in blue with side-chains in stick representation



## CTD-CID interaction with **mutants** studied by fluorescence anisotropy



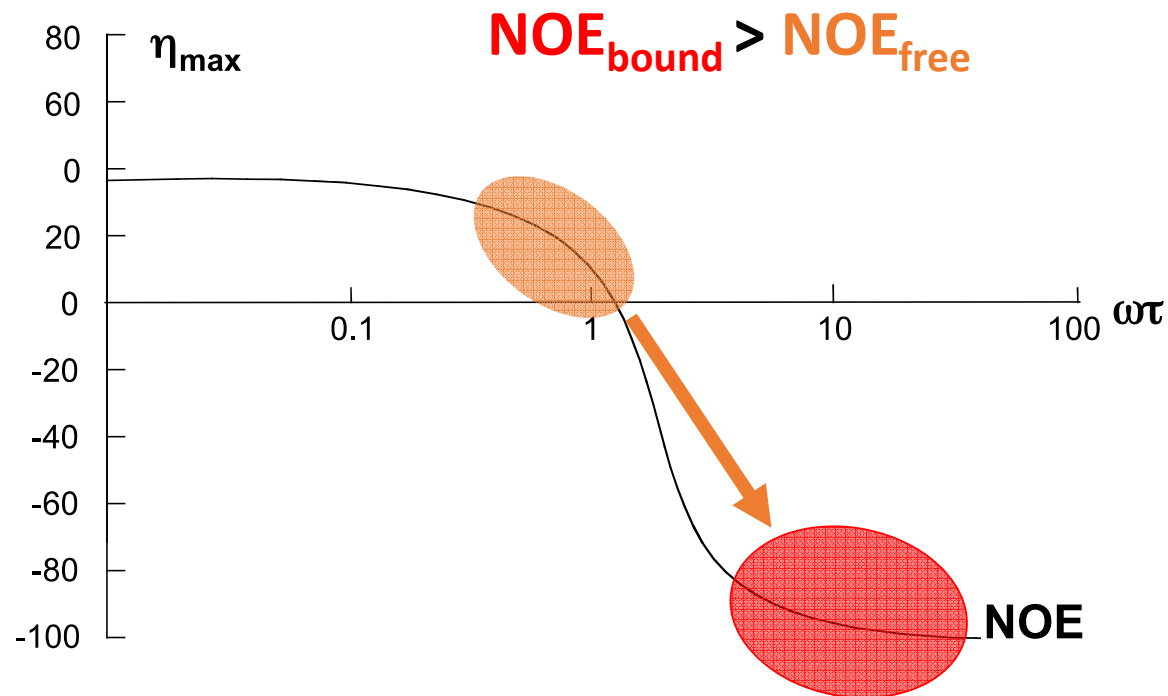
# Interligand NOEs between CID and CTD – 900MHz, 150ms, 293K



# Transferred-NOE

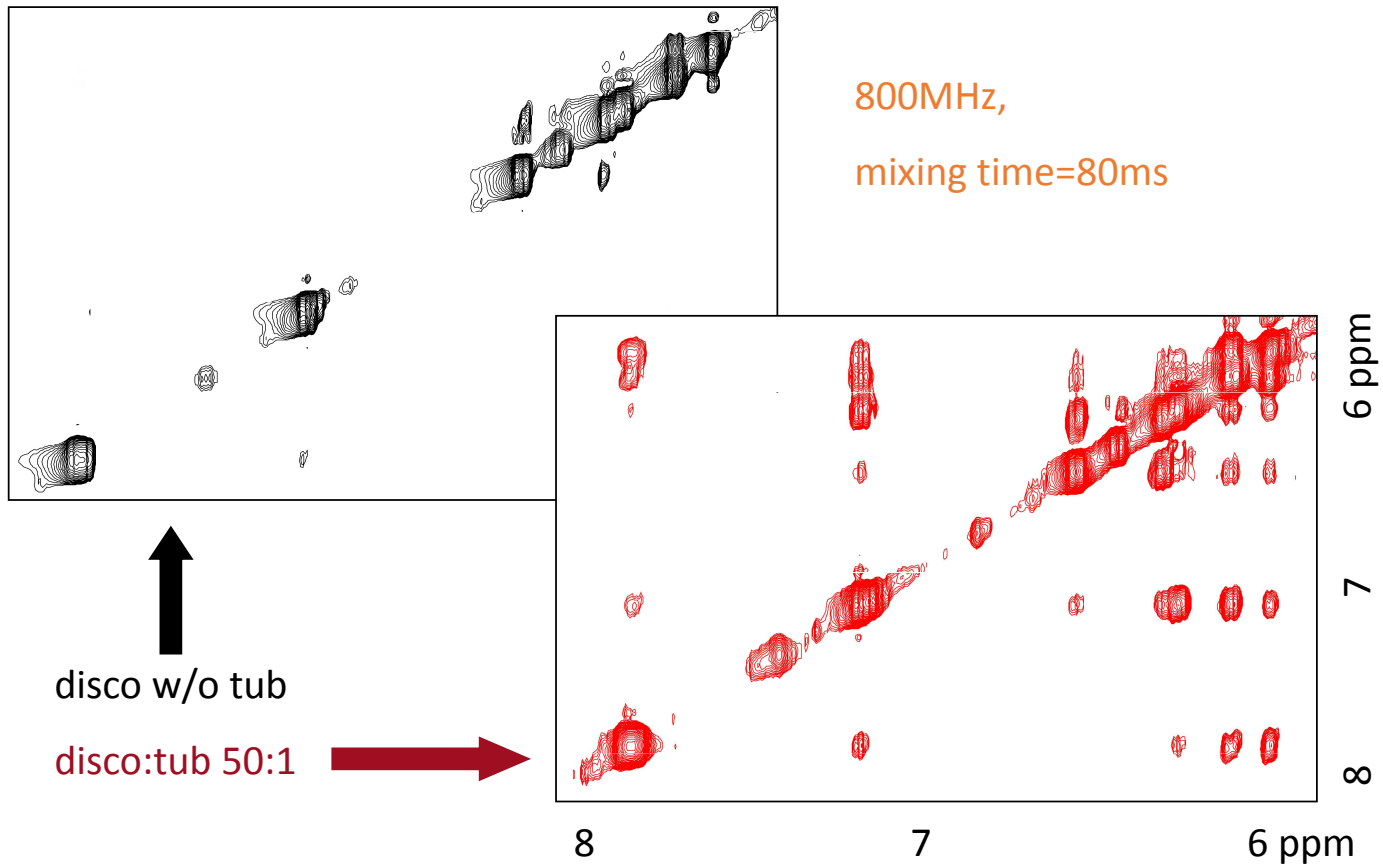
$$\text{NOE} = p_{\text{bound}} \cdot \text{NOE}_{\text{bound}} + p_{\text{free}} \cdot \text{NOE}_{\text{free}}$$

$$\tau_{c,\text{bound}} \gg \tau_{c,\text{free}} \quad (\text{and } p_{L,\text{free}} \gg p_{L,\text{bound}})$$

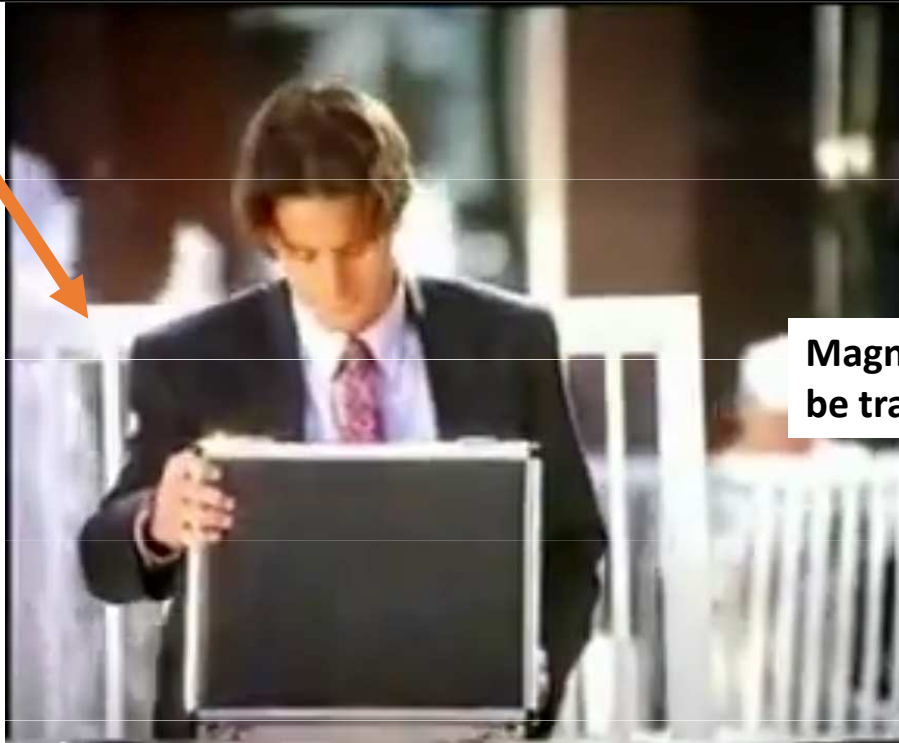


Transferred NOE Experiments

tr-NOESY ~600 $\mu$ M Discodermolide **without** and **with** ~12 $\mu$ M tubulin



protein



Magnetization to be transferred



ligand1



ligand2

Transferred magnetization  
Note the weak "signal"

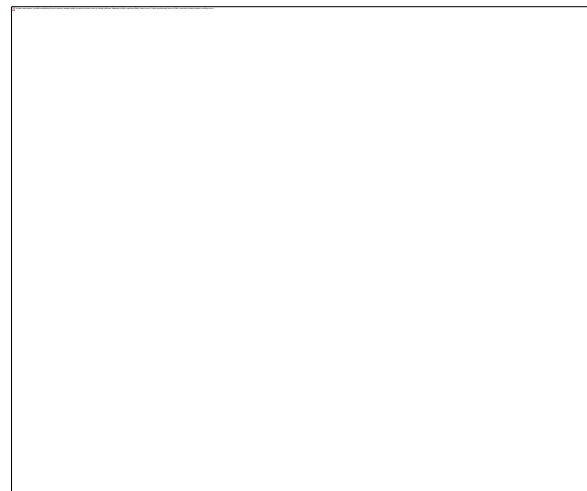


They "compete" for same place but never "meet"

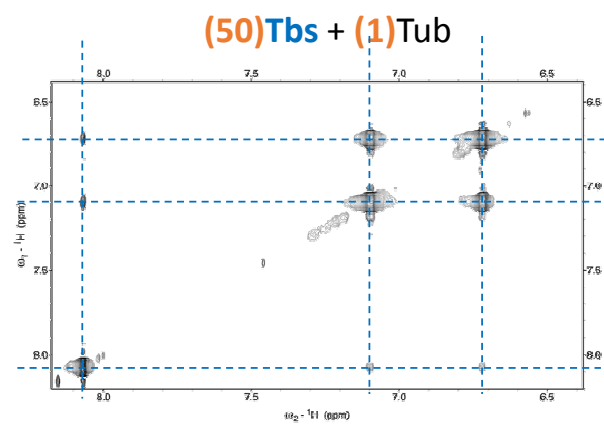
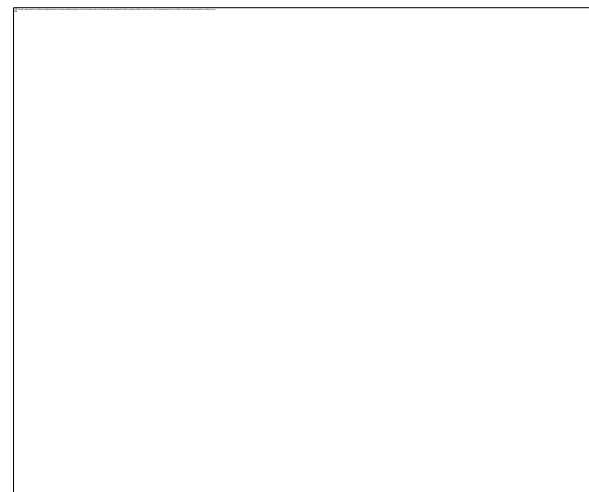
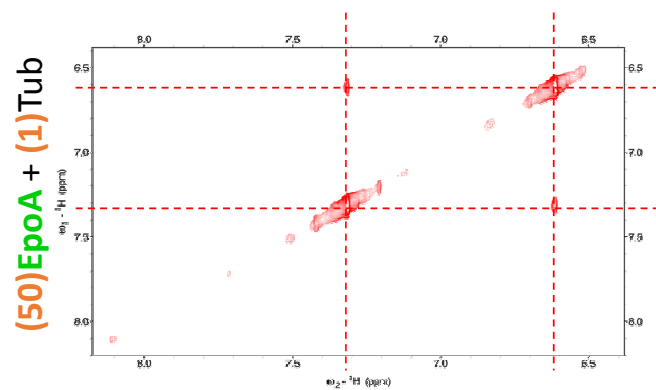


***interligand NOE Experiments***

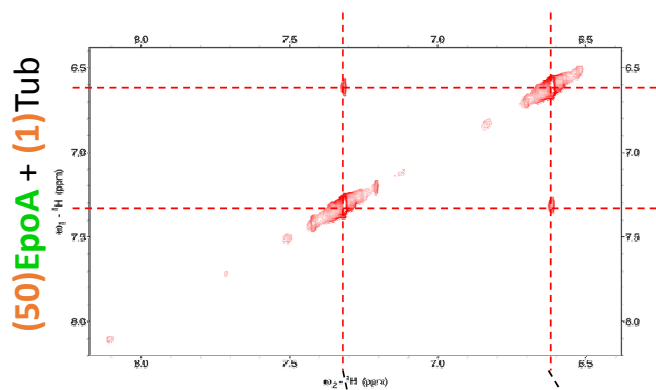
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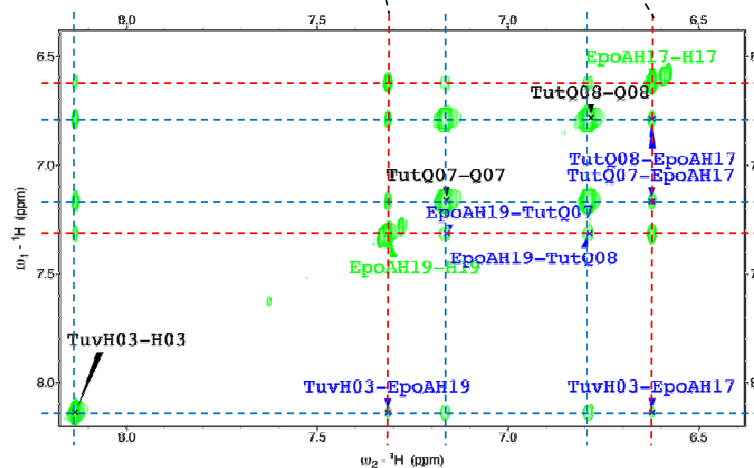
## interligand NOE Experiments



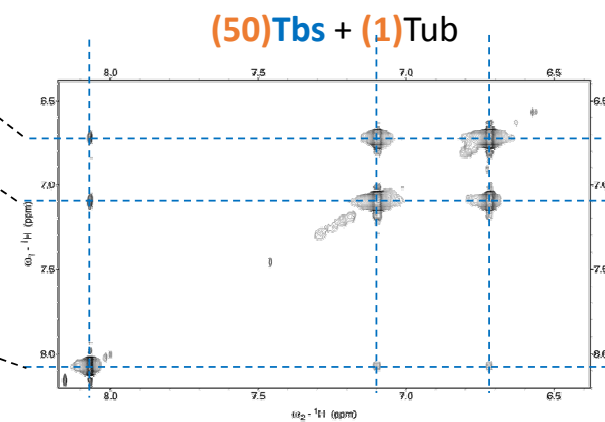
## interligand NOE Experiments



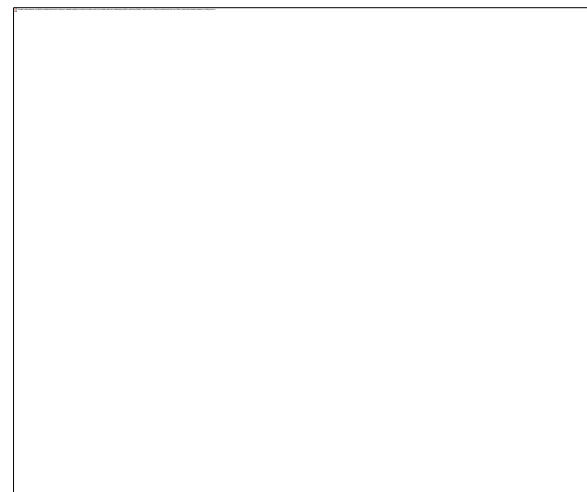
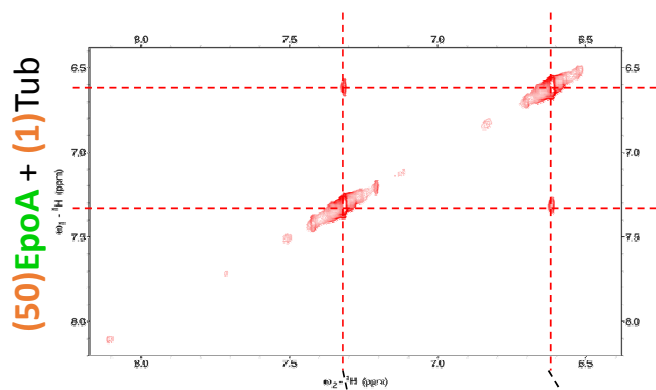
(50)Tbs+(50)EpoA+(1)Tub



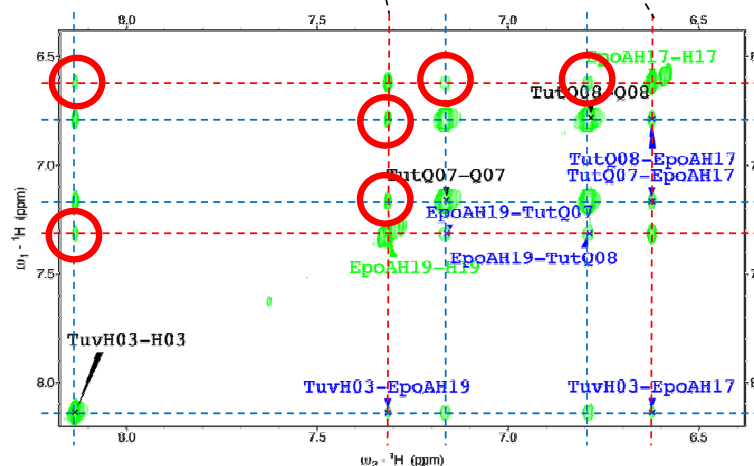
interligand x-peaks, 100-450ms, 900MHz



## interligand NOE Experiments



(50)Tbs+(50)EpoA+(1)Tub



interligand x-peaks, 100-450ms, 900MHz

