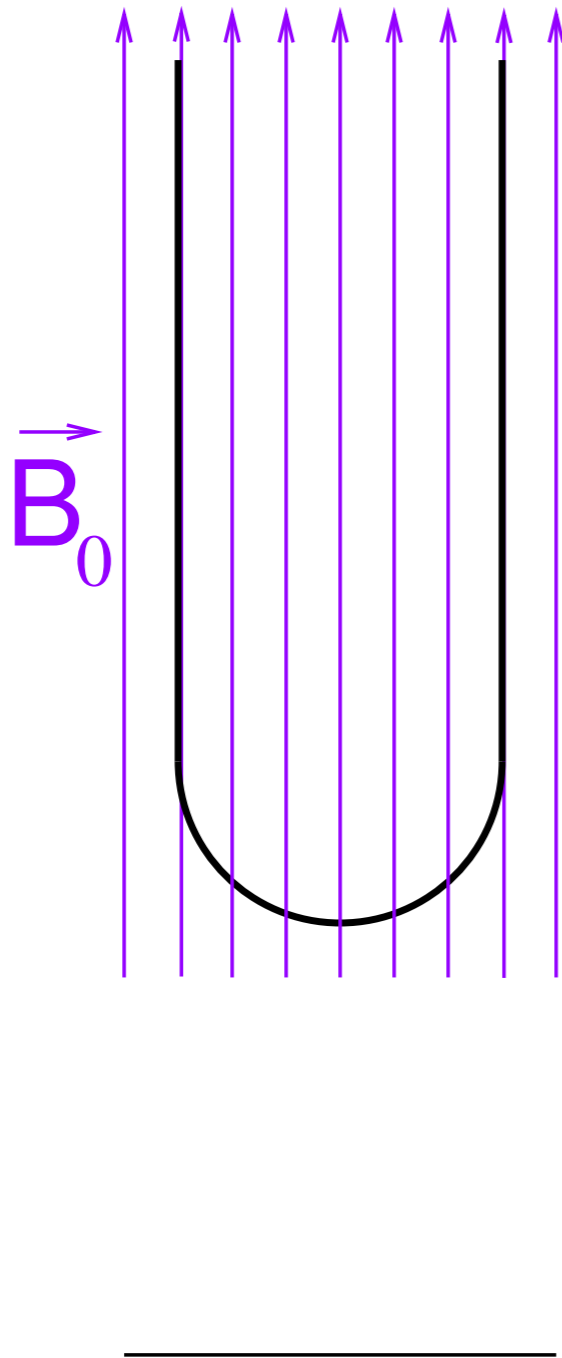
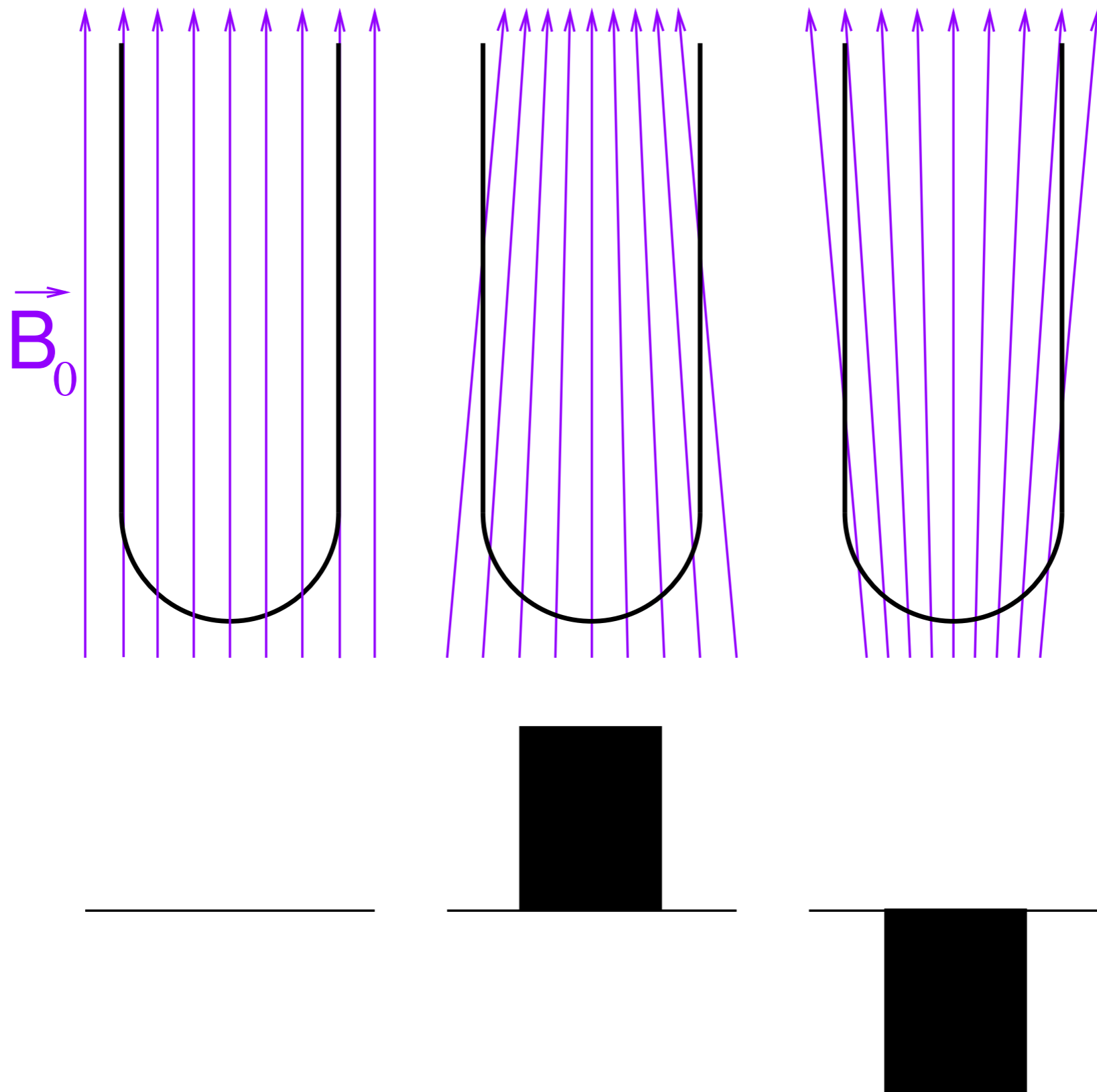


# Lecture 13: Field gradients

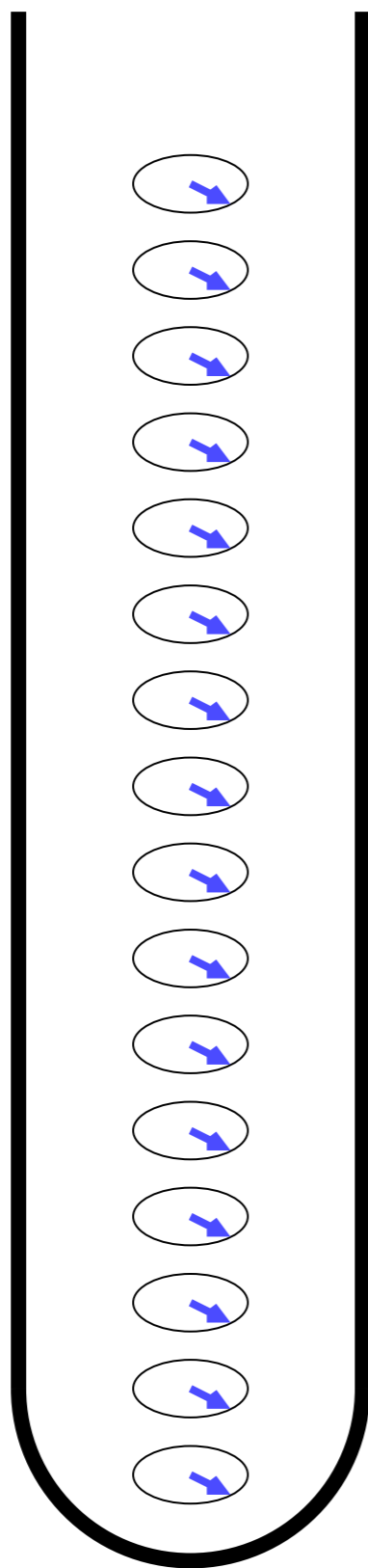
# Homogeneous field



# Pulsed field gradients ( $G_z$ )

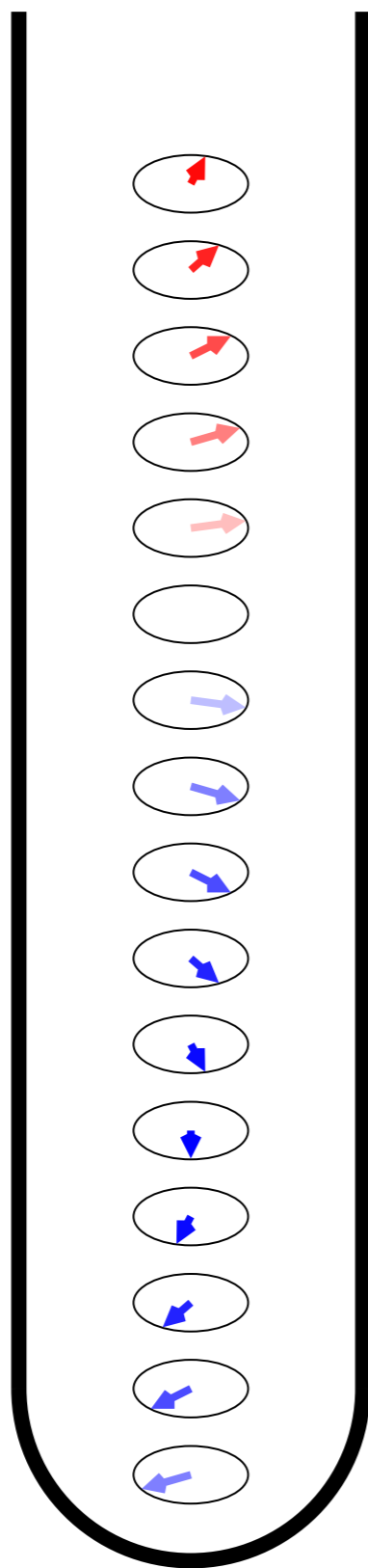


# Gradients dephase transverse magnetization



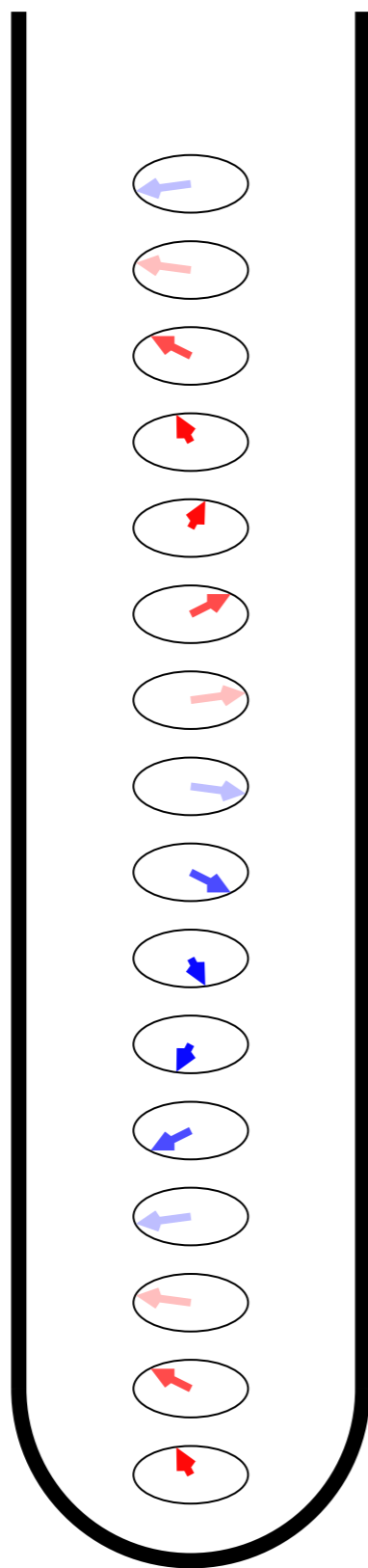
$$G_z = 0 \text{ units}$$

# Gradients dephase transverse magnetization



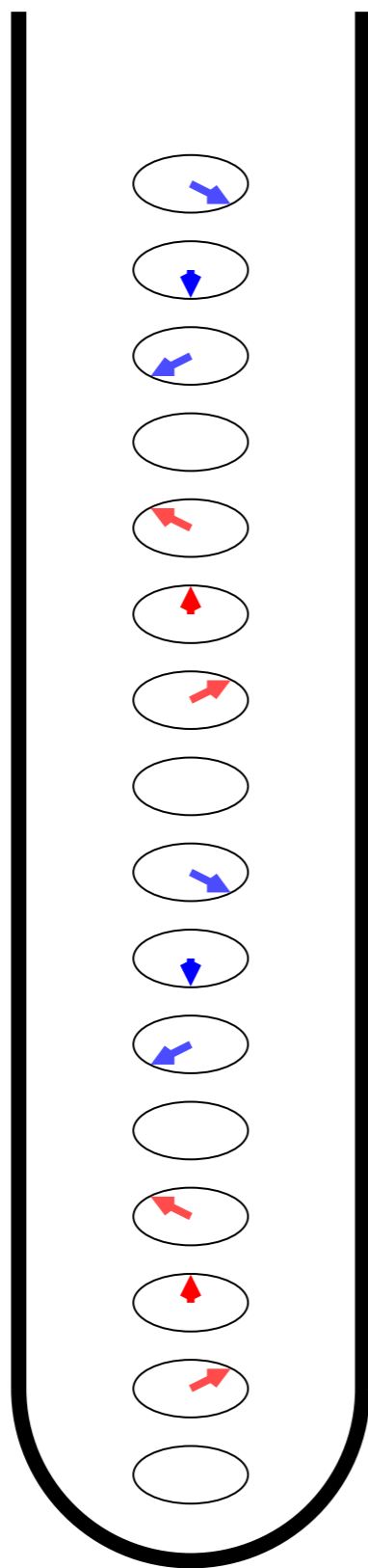
$$G_z = 1 \text{ units}$$

# Gradients dephase transverse magnetization



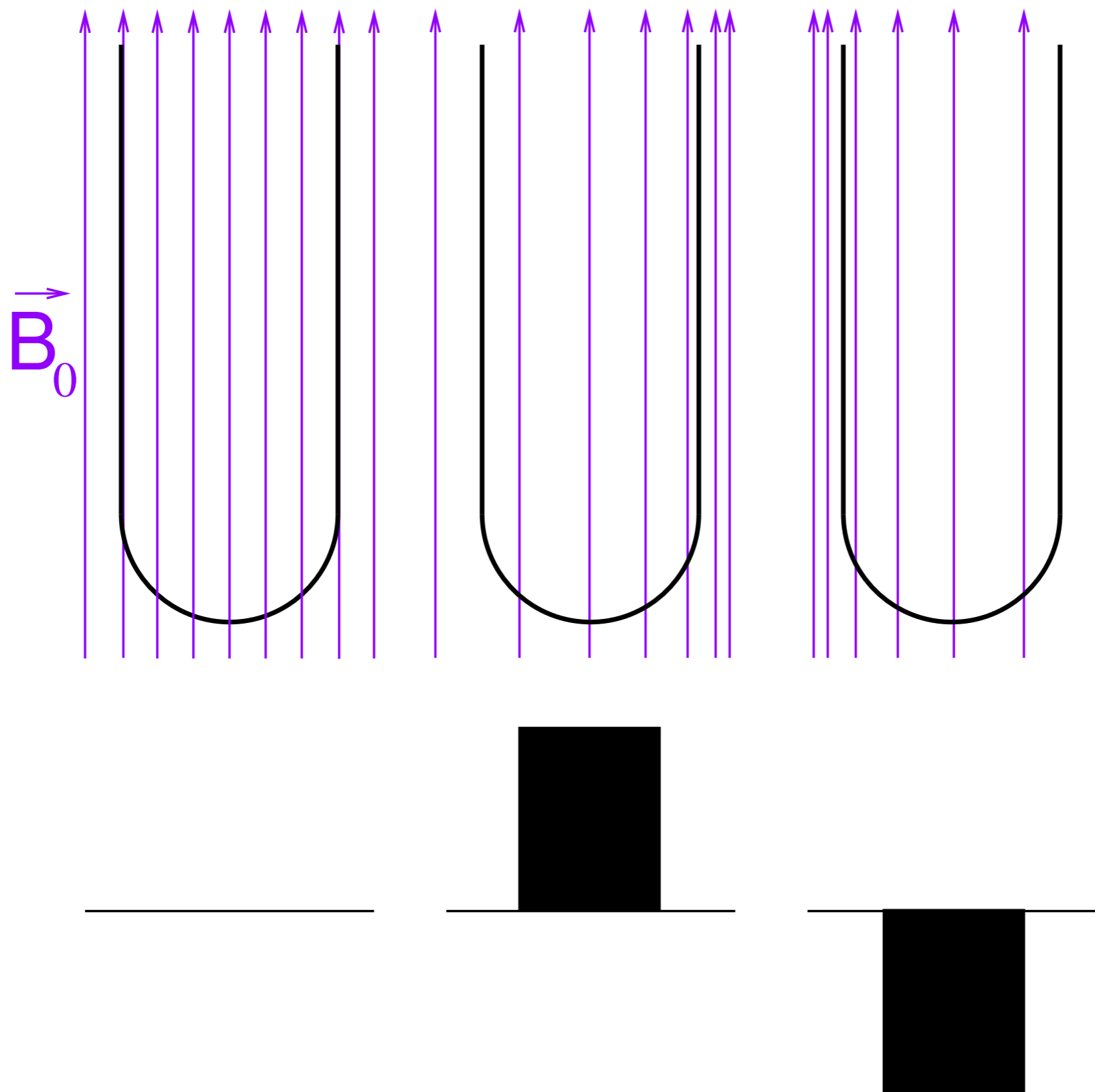
$$G_z = 2 \text{ units}$$

# Gradients dephase transverse magnetization



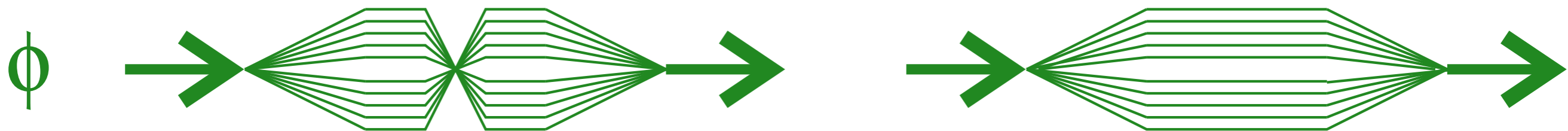
$$G_z = 4 \text{ units}$$

# Pulsed field gradients ( $G_y$ )

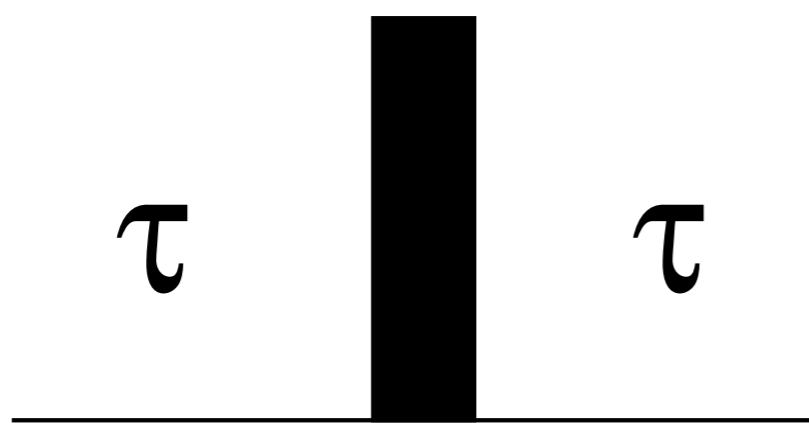




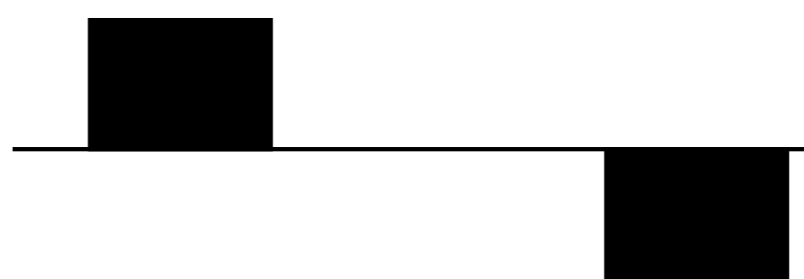
# Gradient echoes



$^1\text{H}$



$G_z$



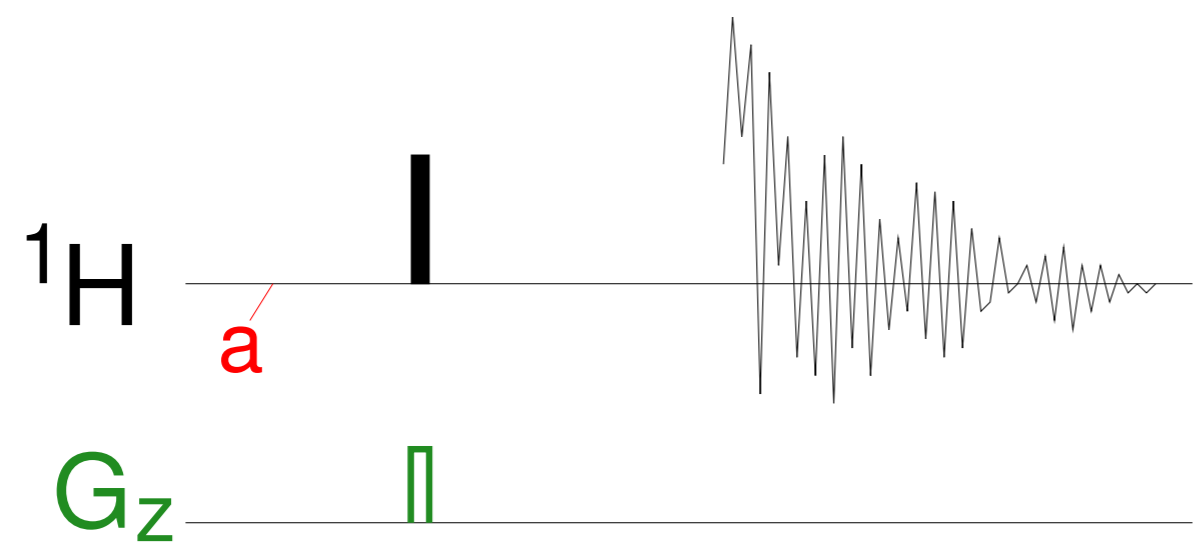
# **GRADIENTS AND MAGNETIC RESONANCE IMAGING**

**Lars G. Hanson**

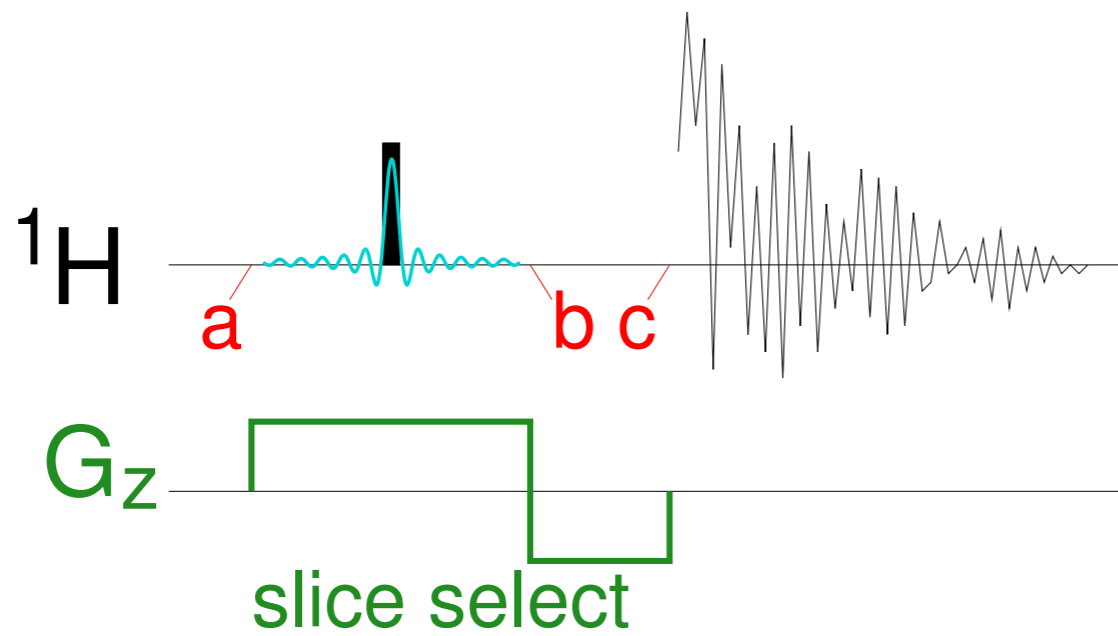
**Copenhagen University Hospital Hvidovre**

[https://eprints.drcmr.dk/37/1/MRI\\_English\\_a4.pdf](https://eprints.drcmr.dk/37/1/MRI_English_a4.pdf)

# Slice selection by $G_z$

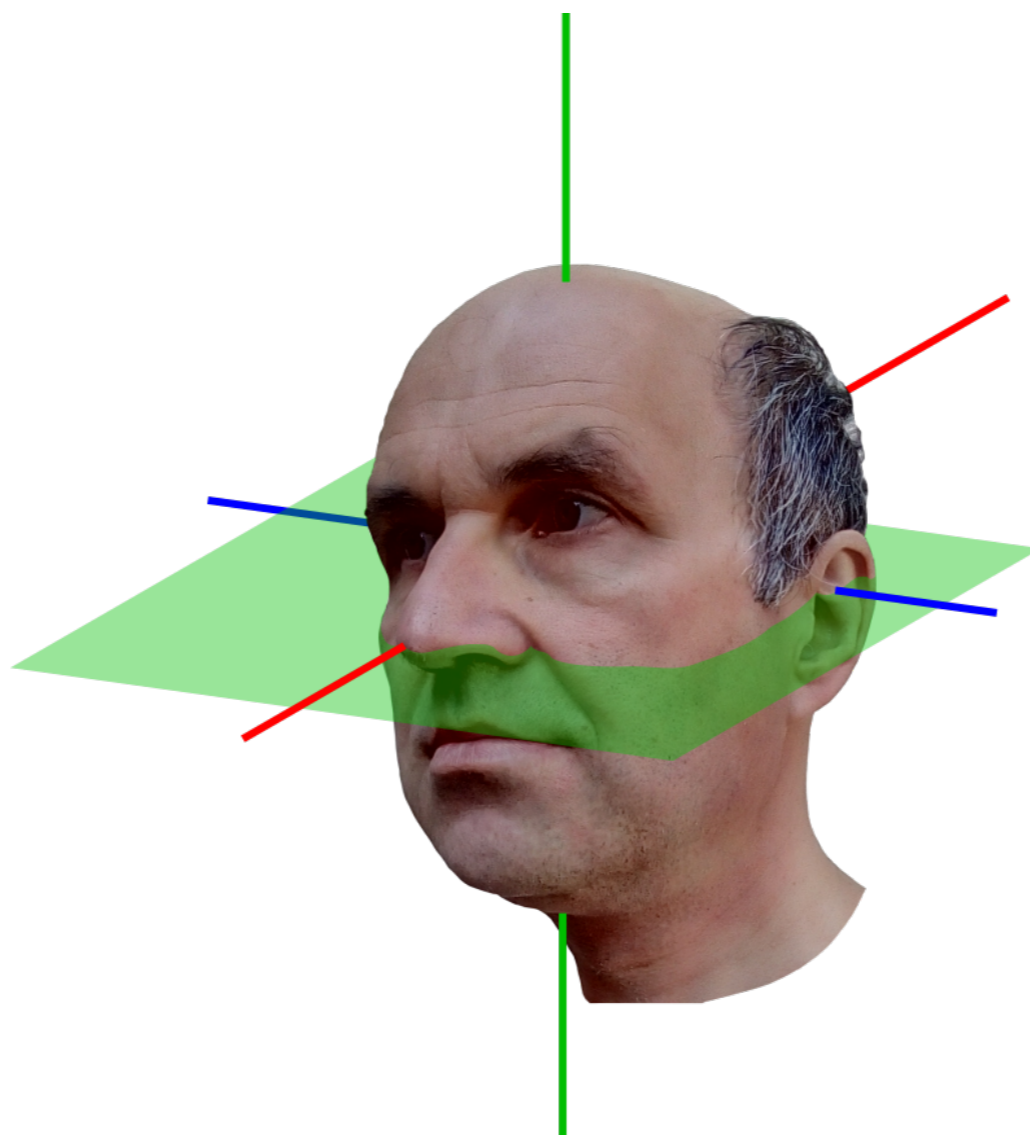


# Slice selection by $G_z$

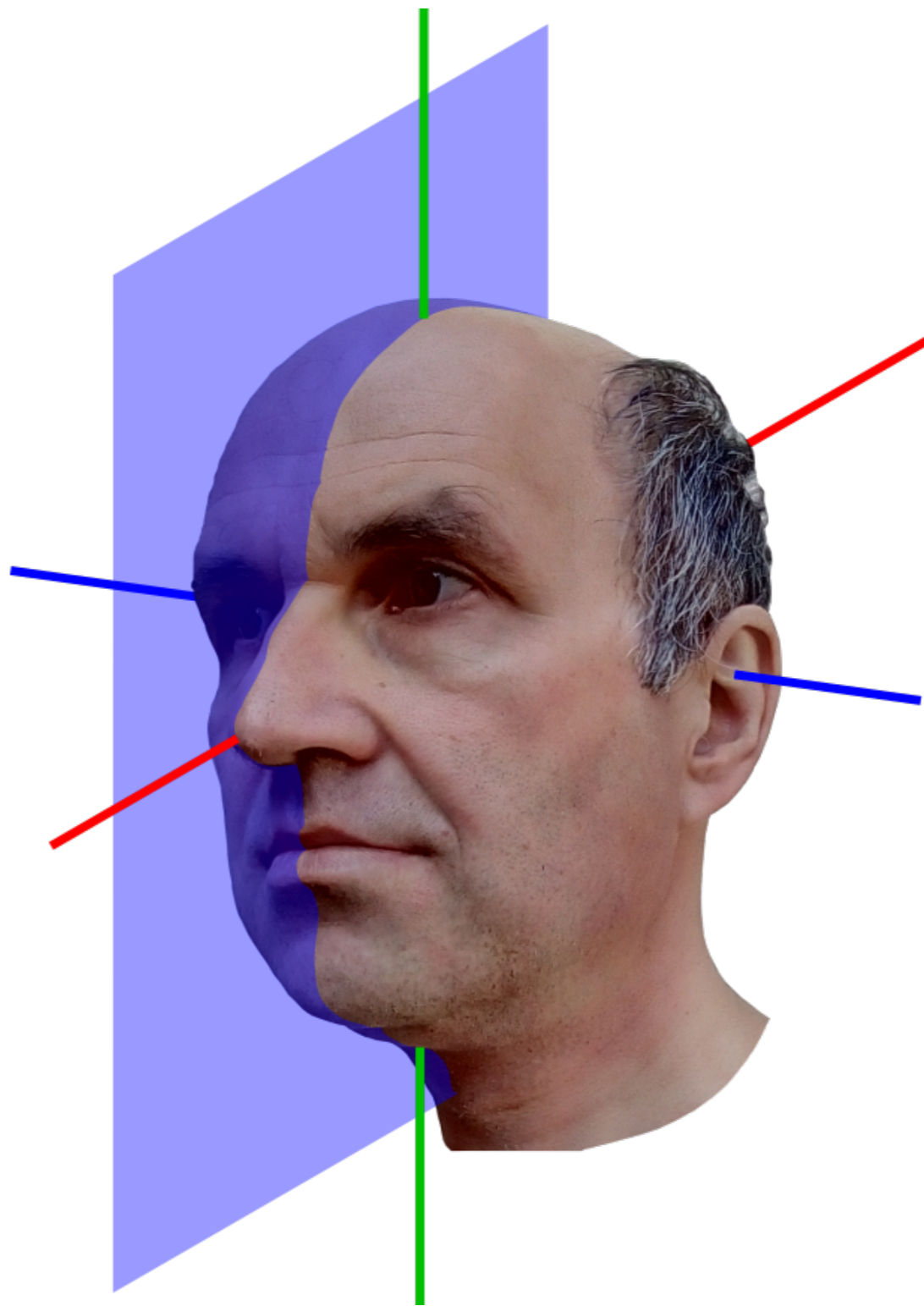


Selective pulse: **amplitude modulation**

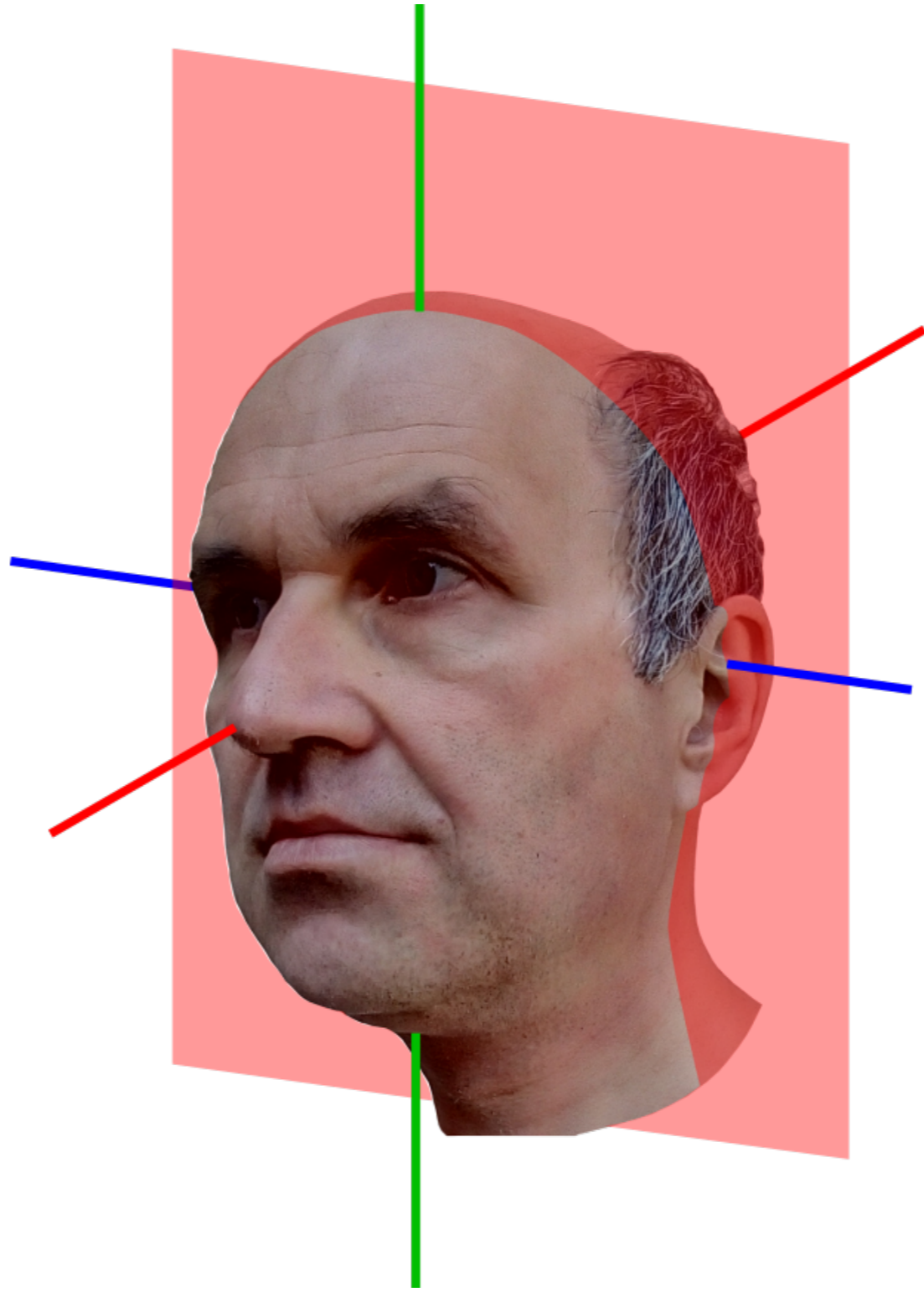
# Axial slice selection by $G_z$



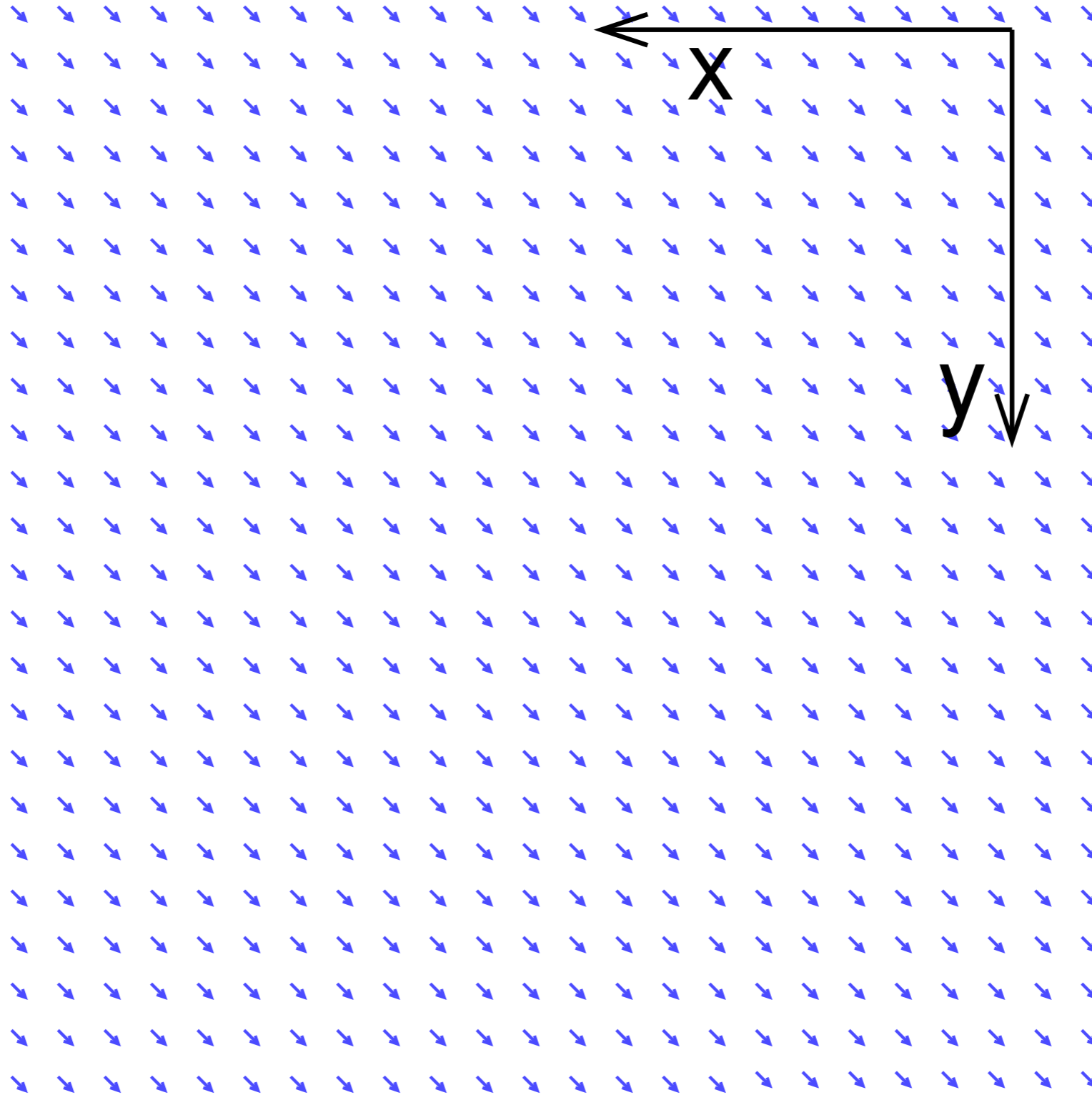
# Sagittal slice selection by $G_x$



# Coronal slice selection by $G_y$

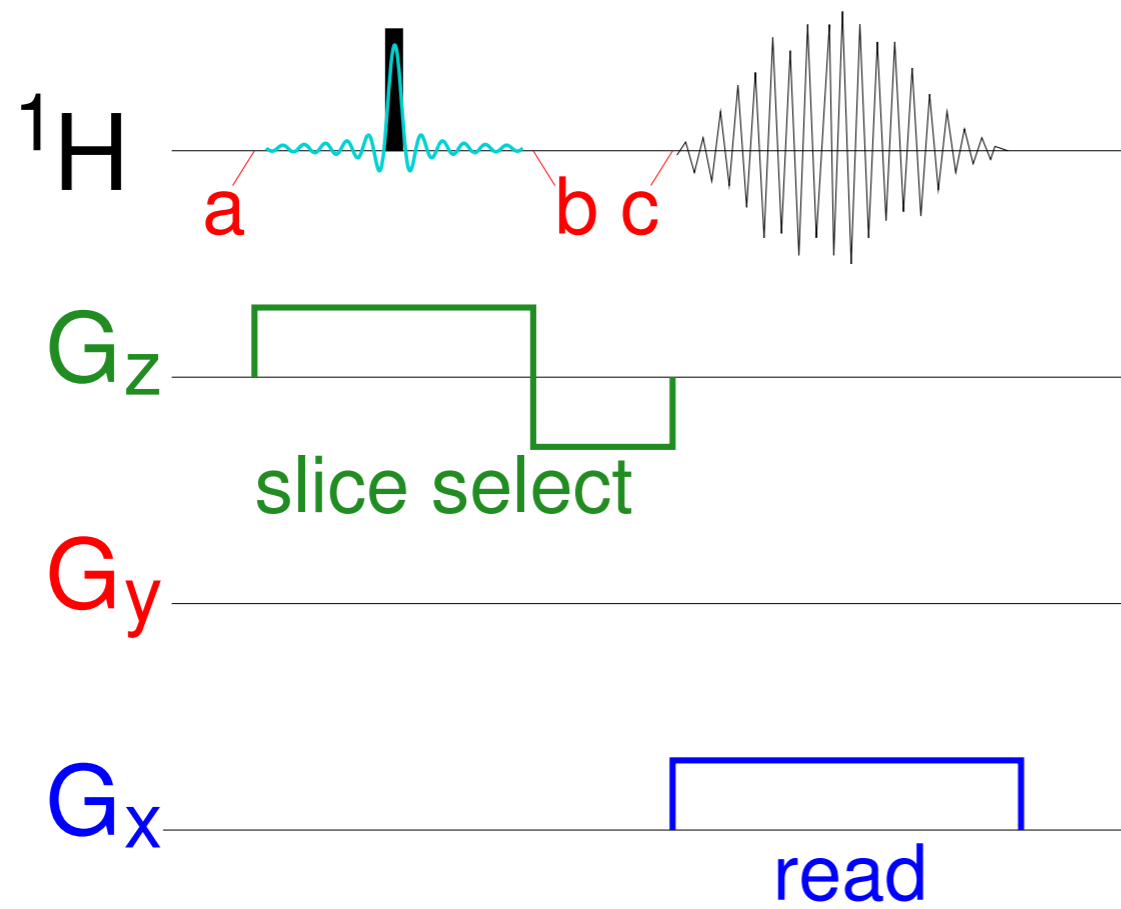


# Magnetization in the slice

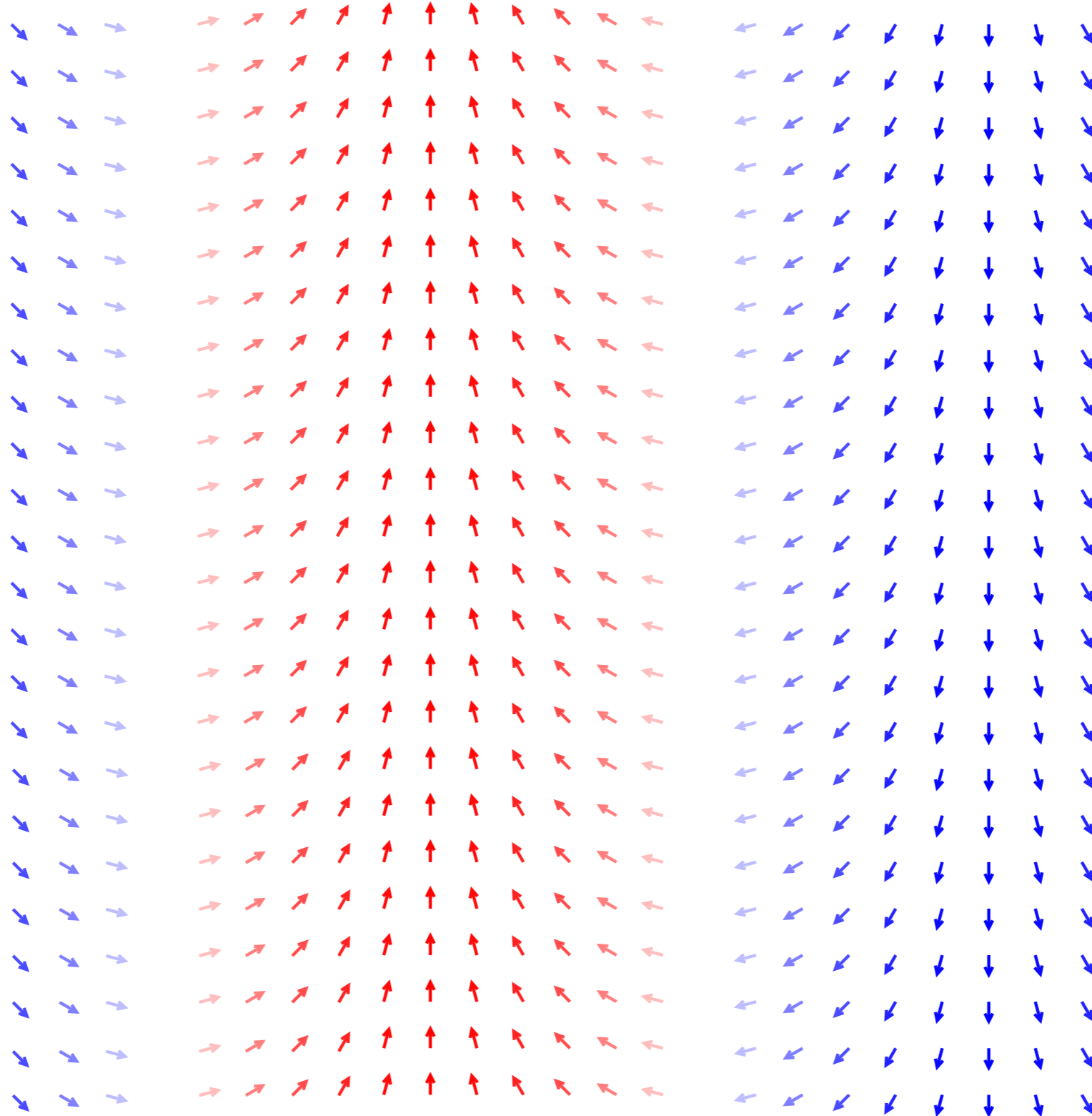




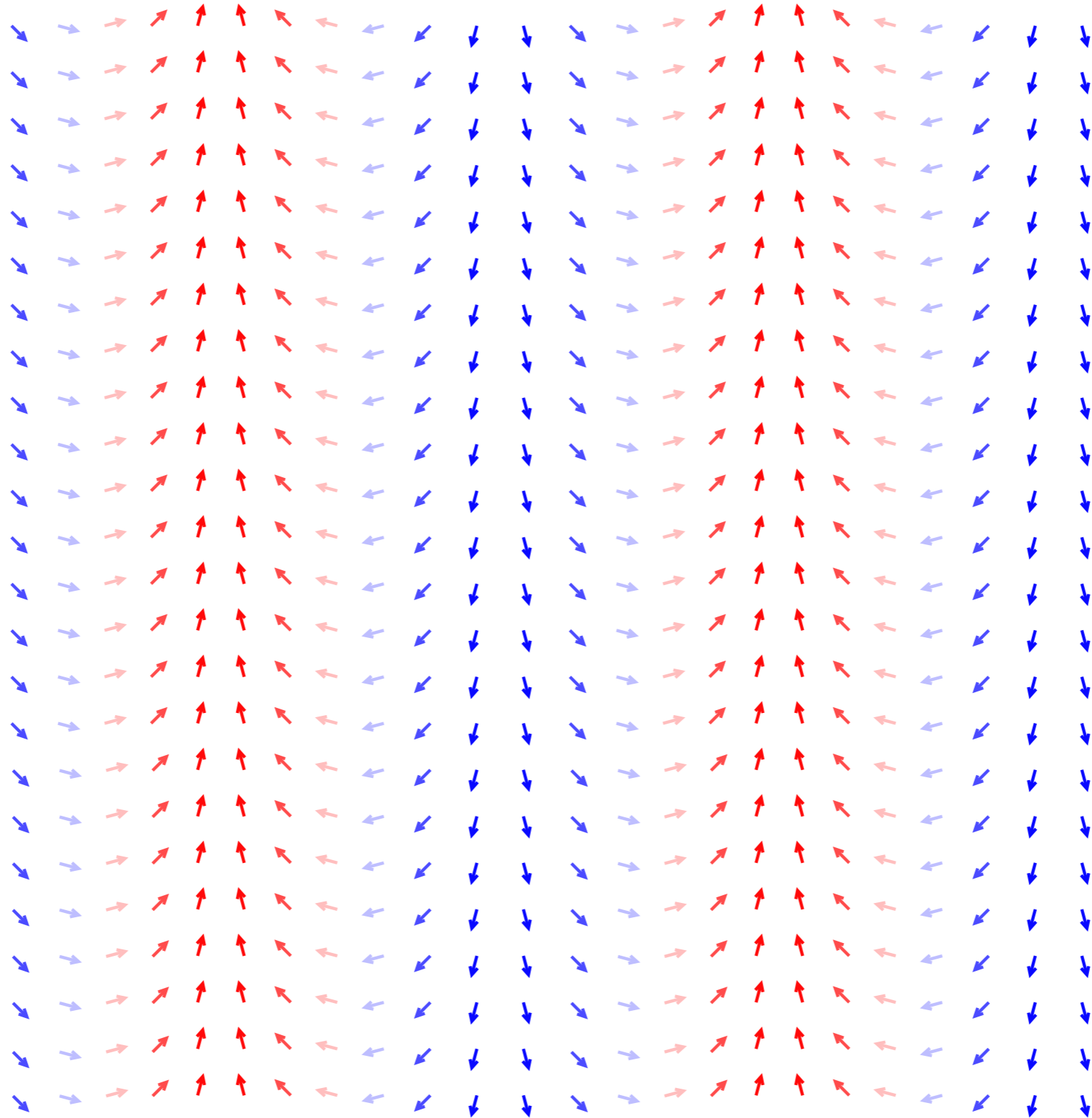
# 1D imaging in the slice



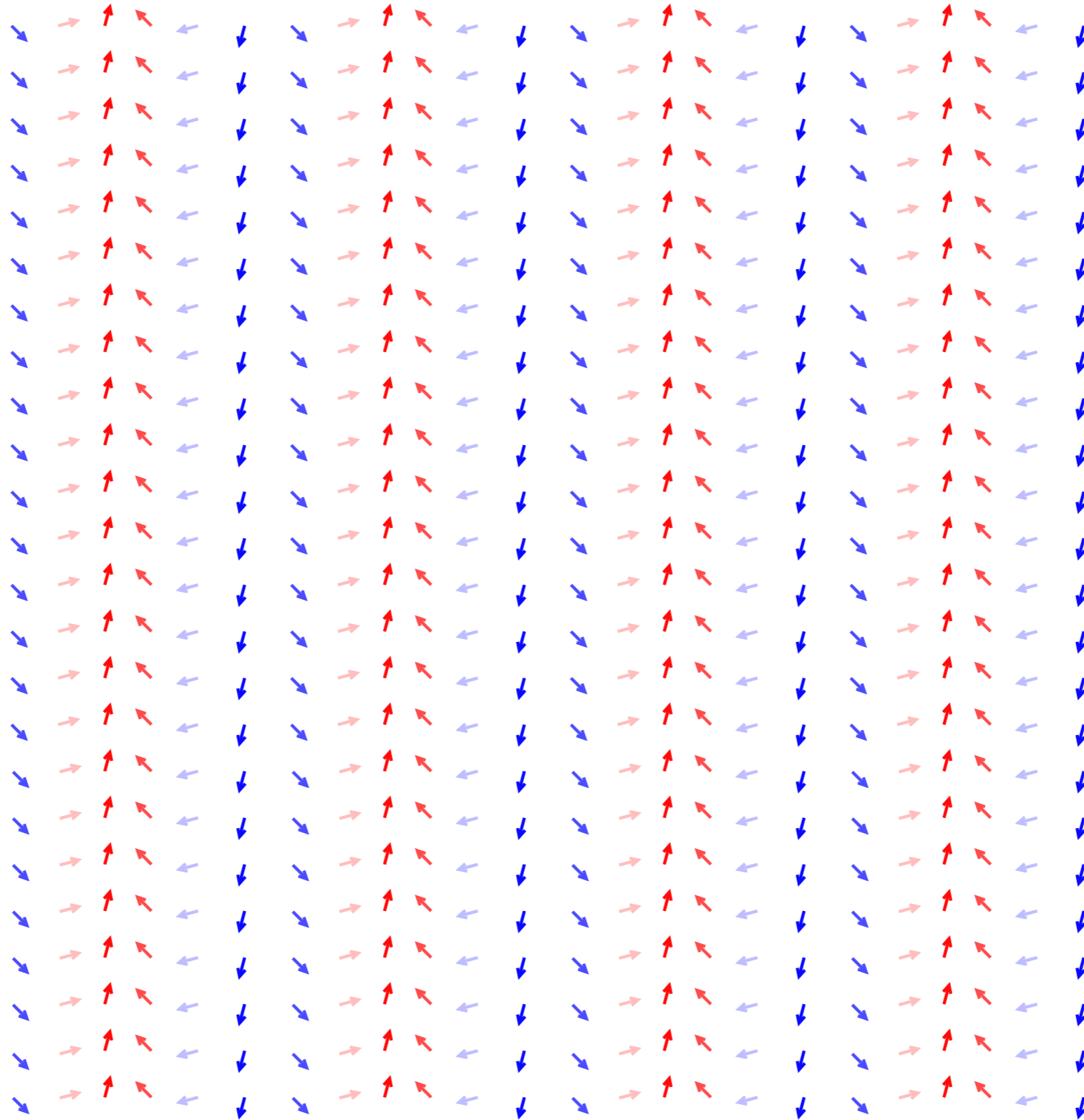
# Magnetization in the slice with gradient $G_x$



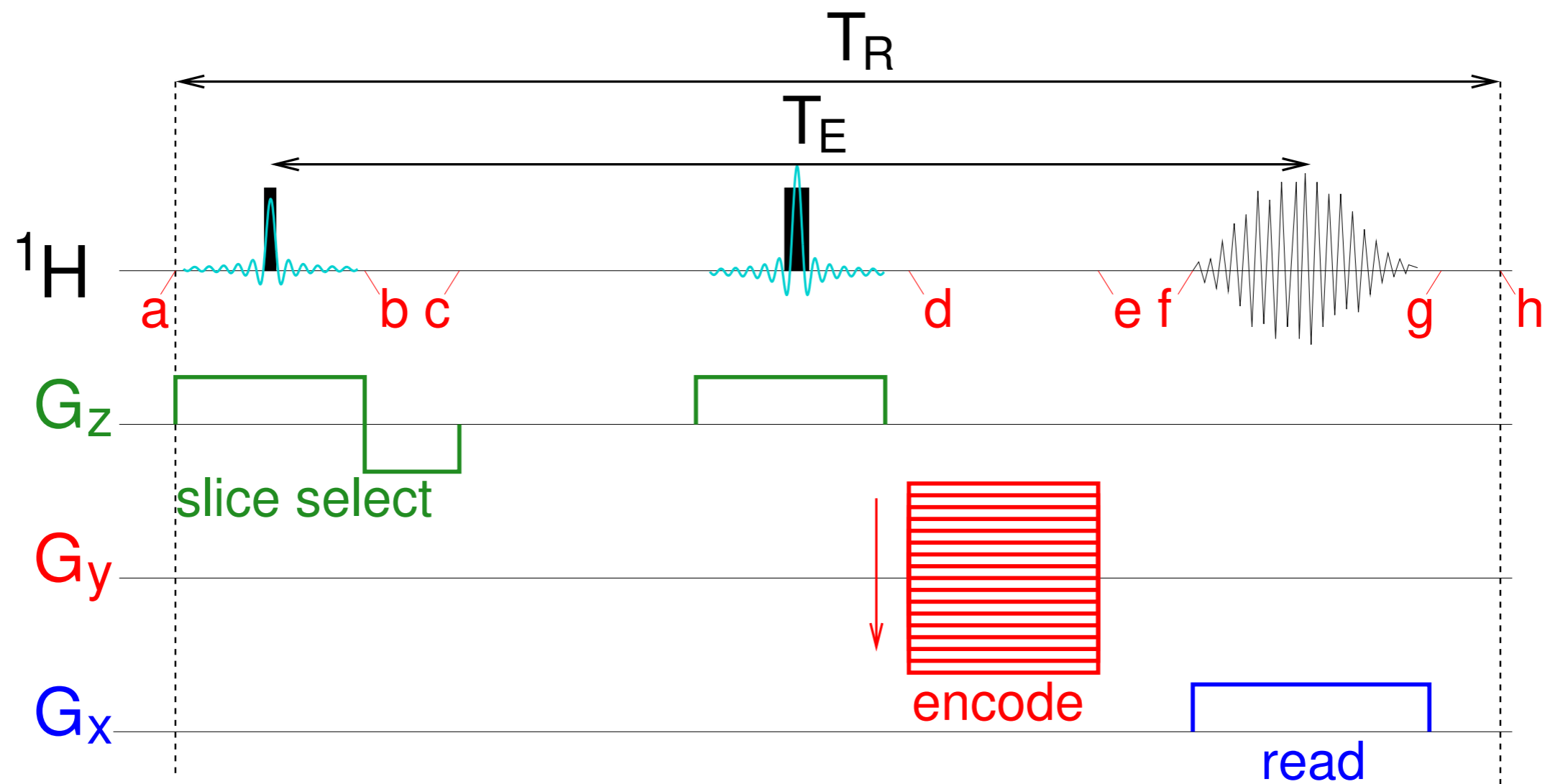
# Magnetization in the slice with gradient $G_x$



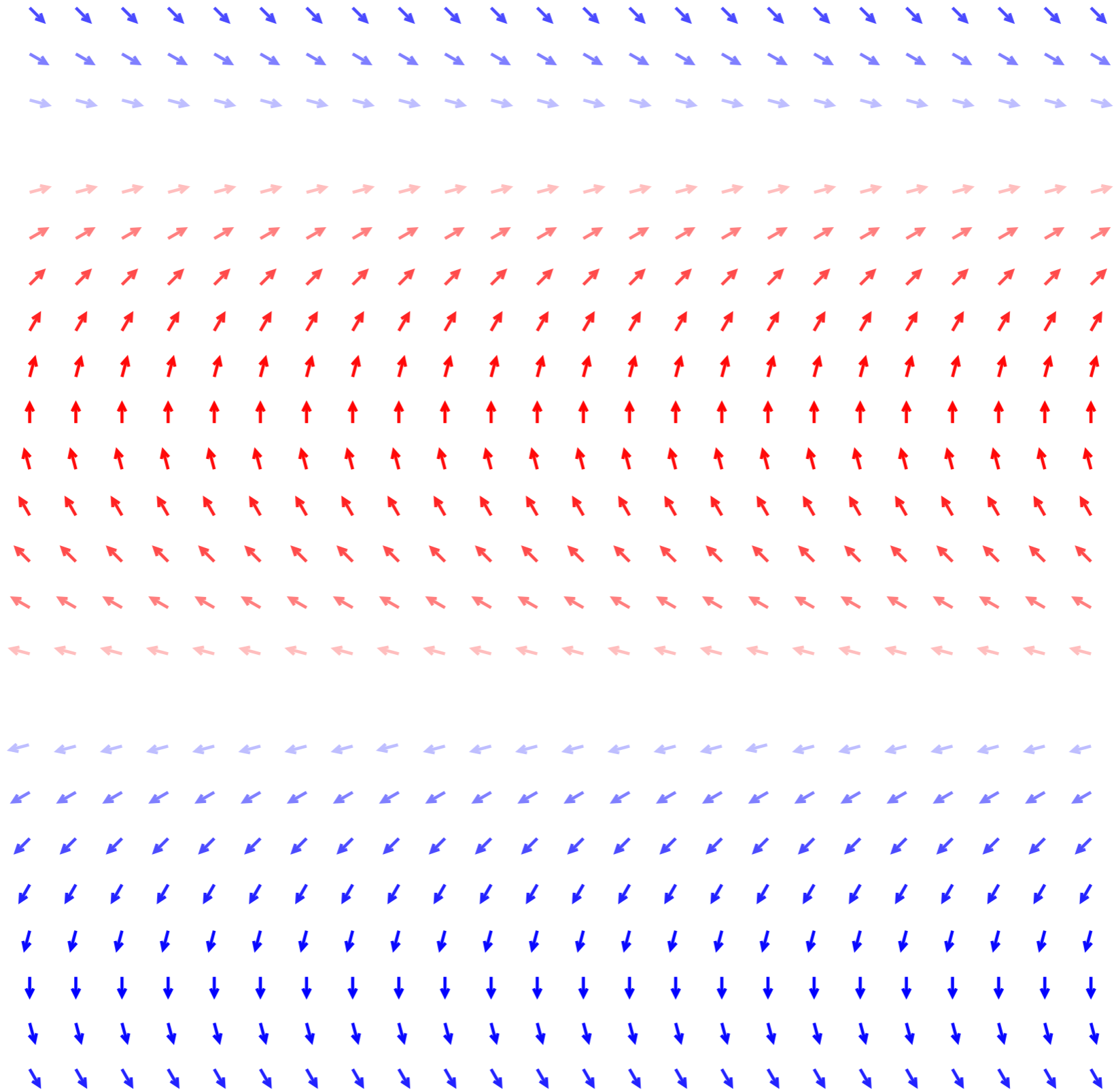
# Magnetization in the slice with gradient $G_x$



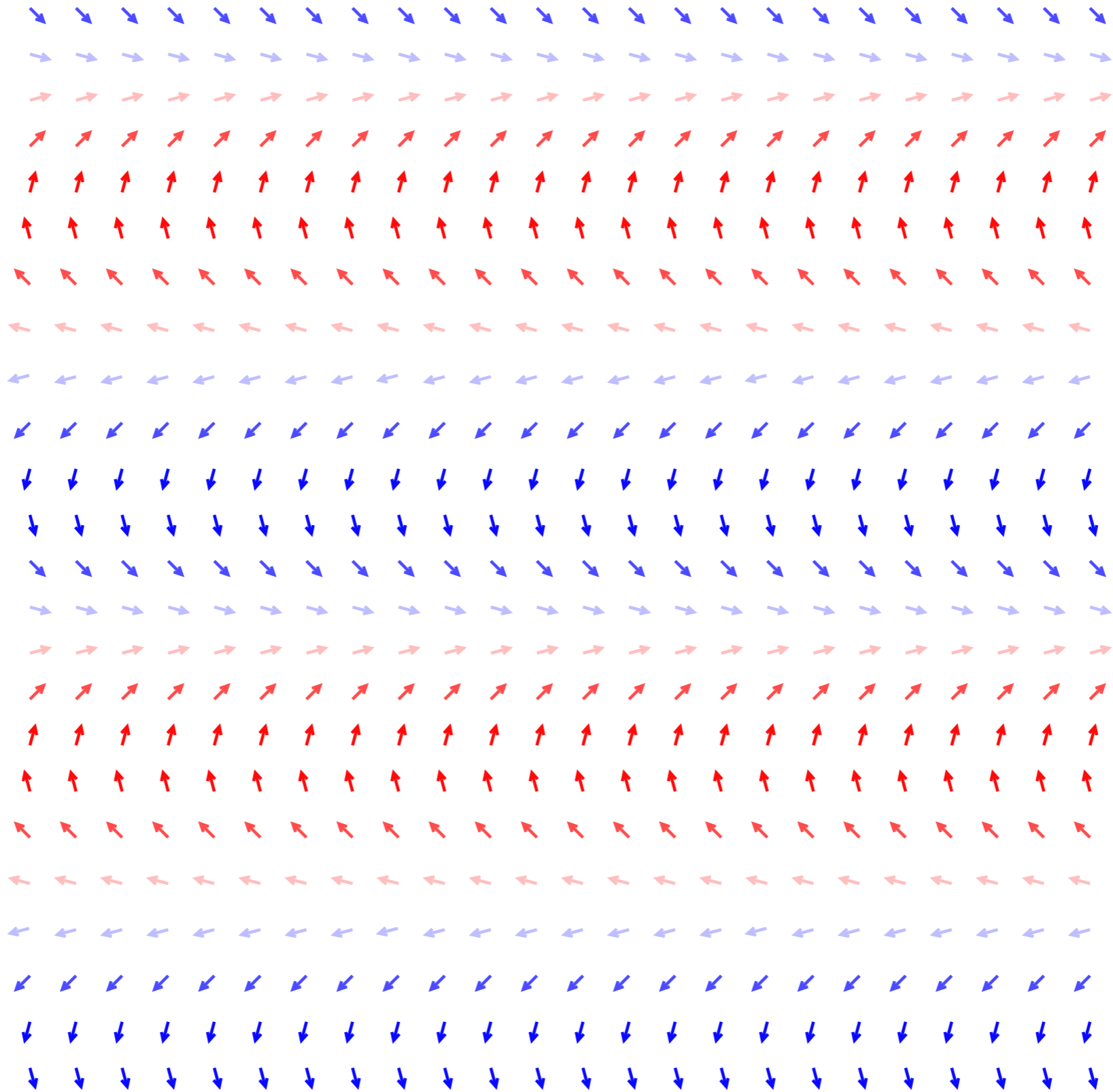
# 2D imaging in the slice



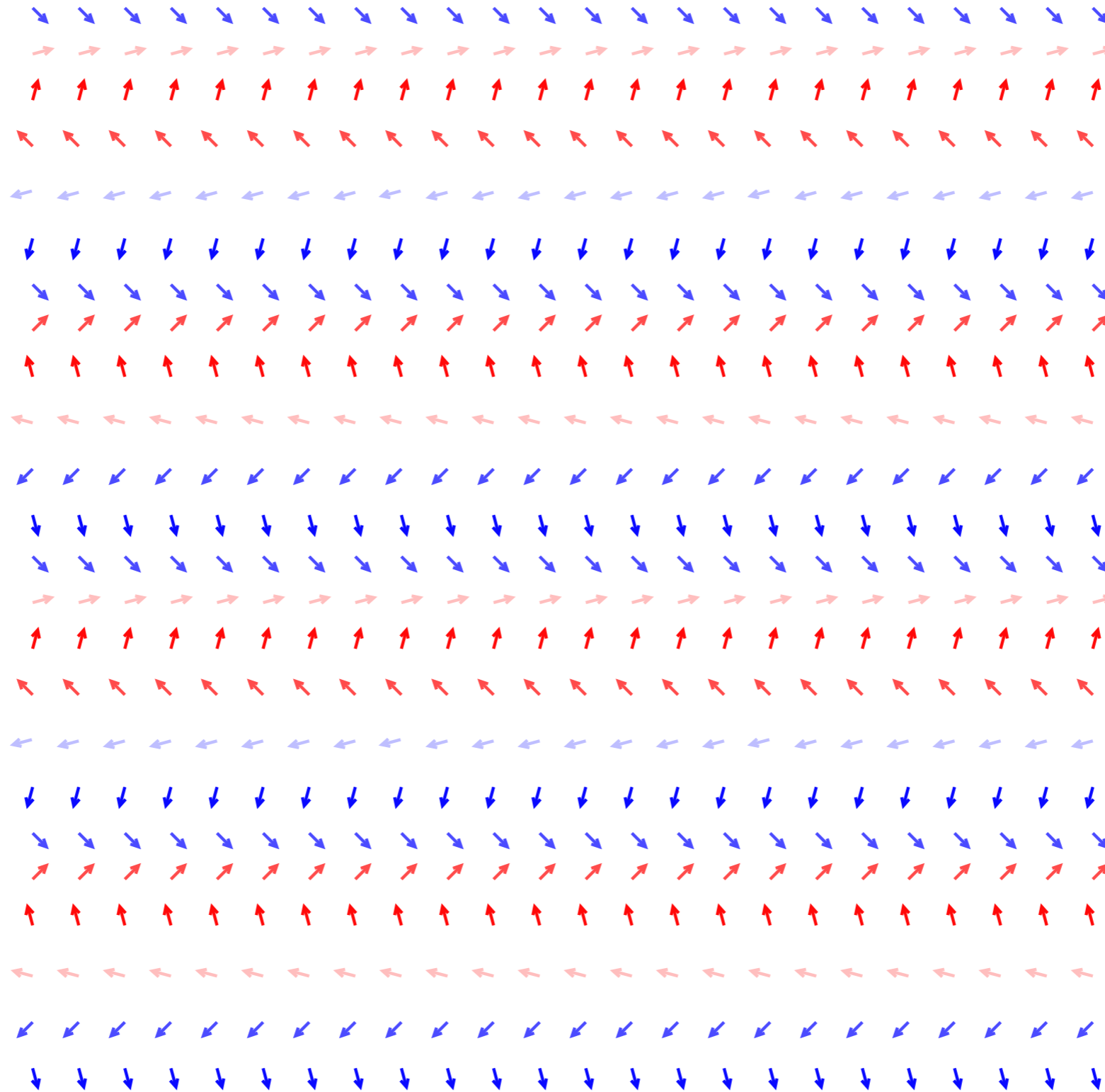
# Magnetization in the slice with gradient $G_y$



# Magnetization in the slice with gradient $G_y$

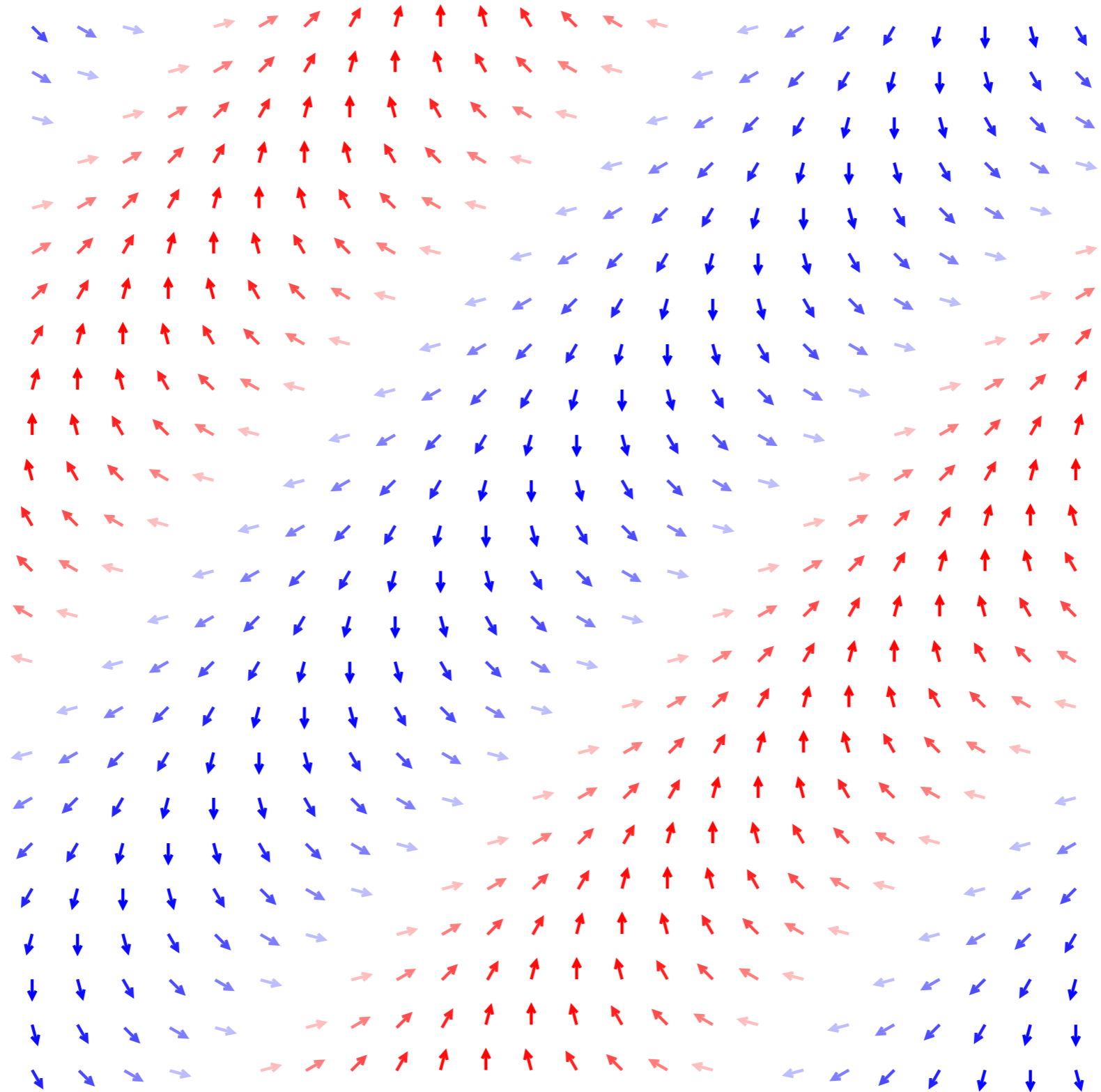


# Magnetization in the slice with gradient $G_y$

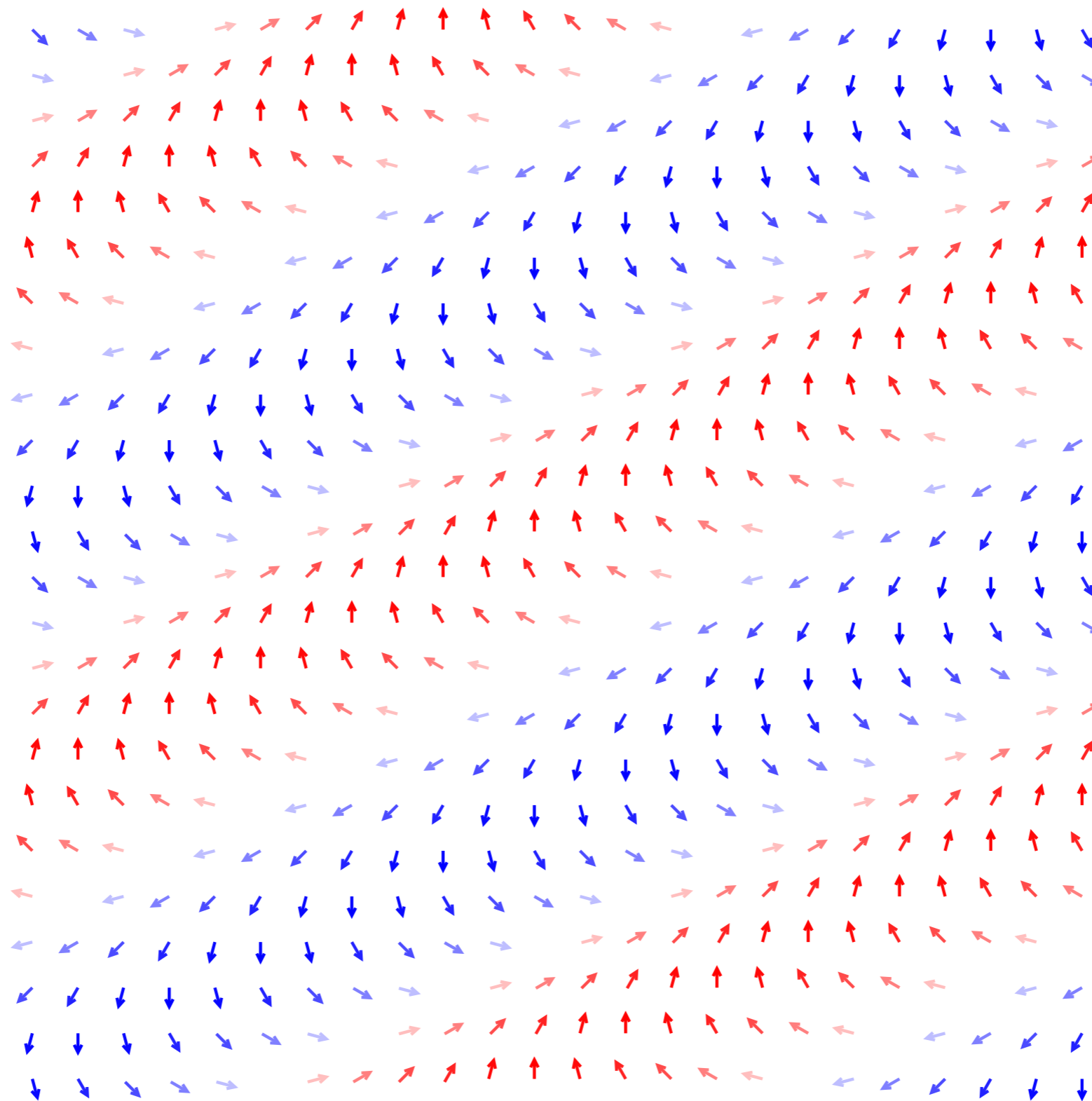




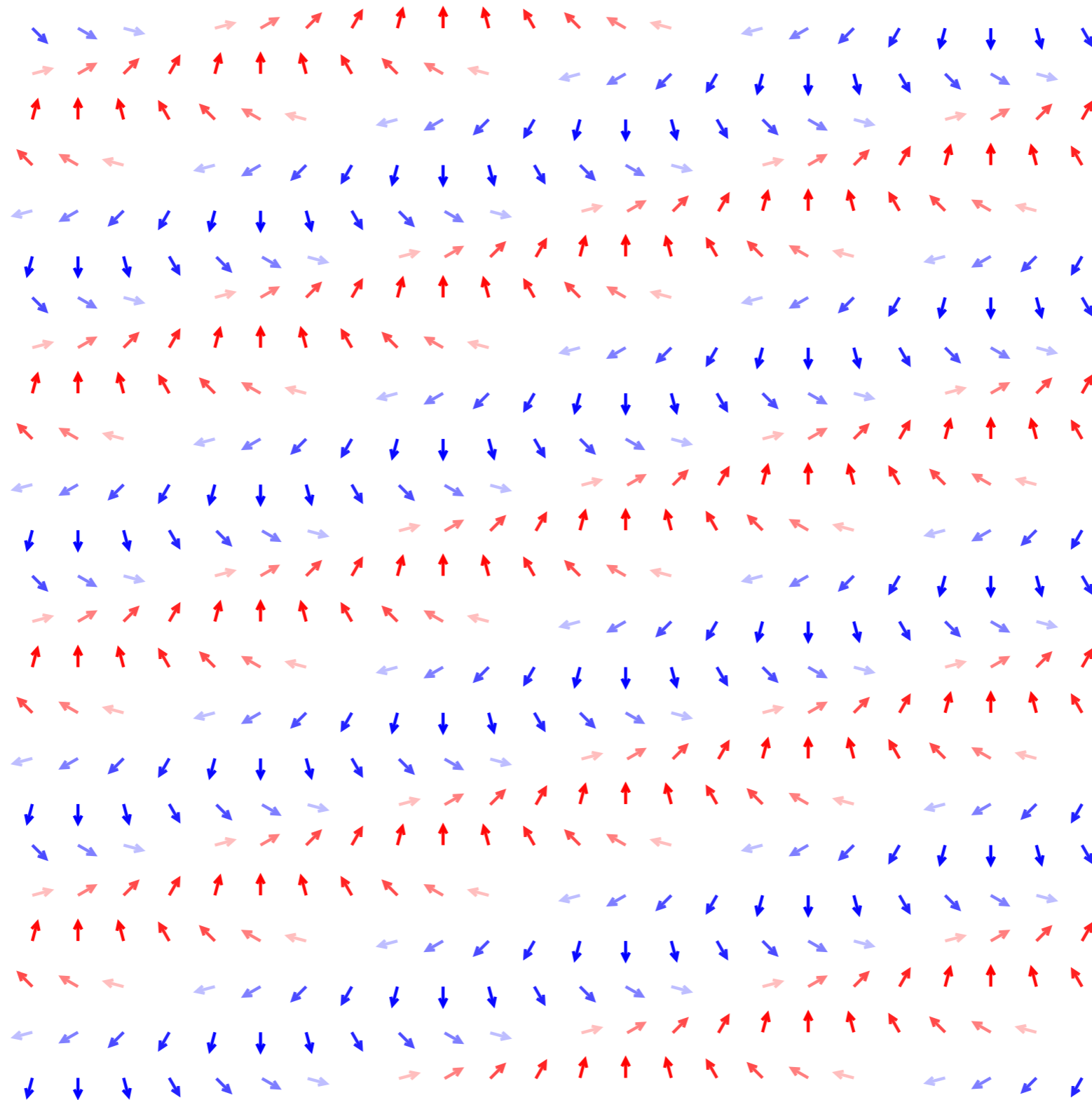
# Combination of gradients $G_x$ and $G_y$



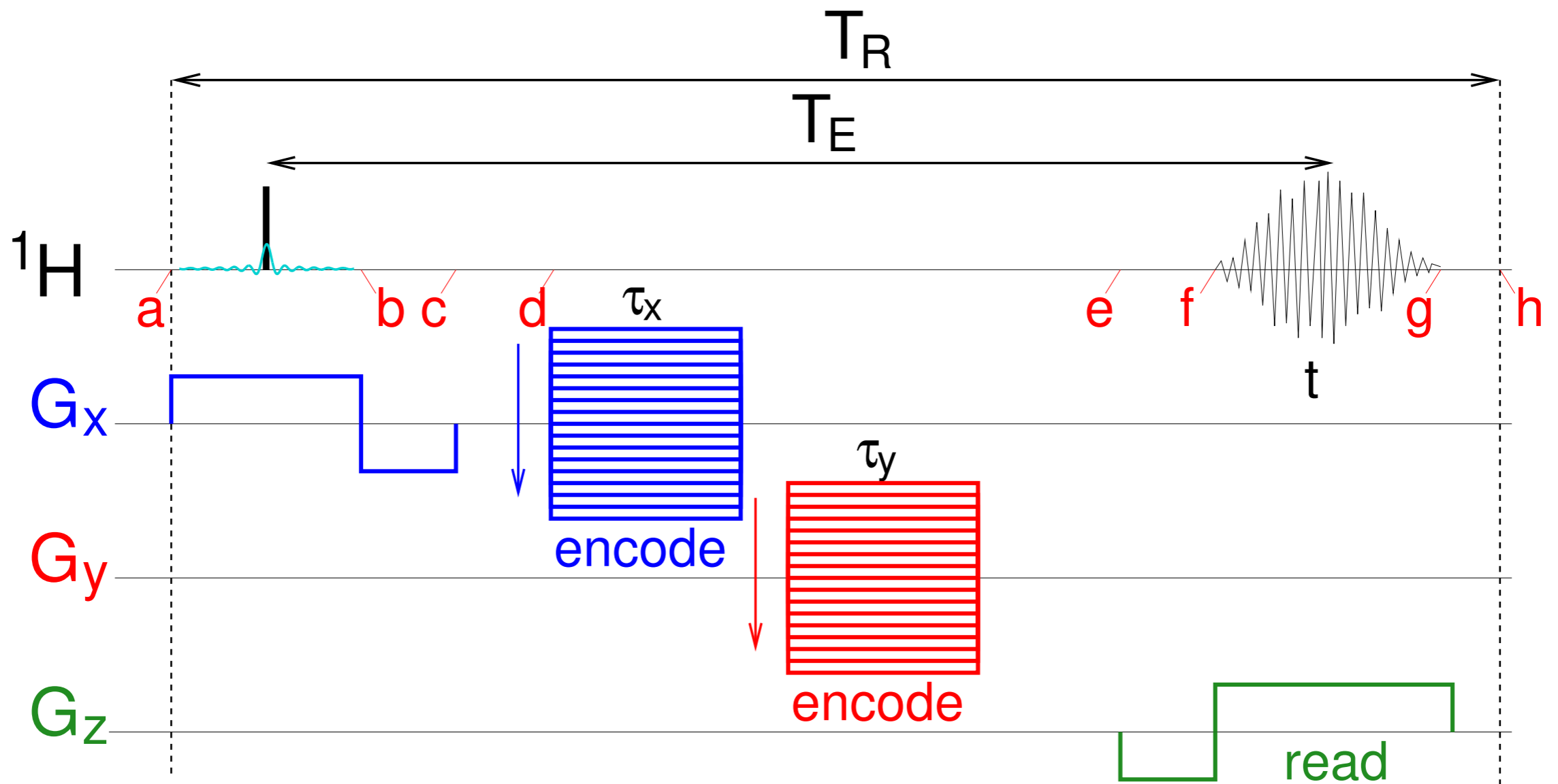
# Combination of gradients $G_x$ and $G_y$



# Combination of gradients $G_x$ and $G_y$



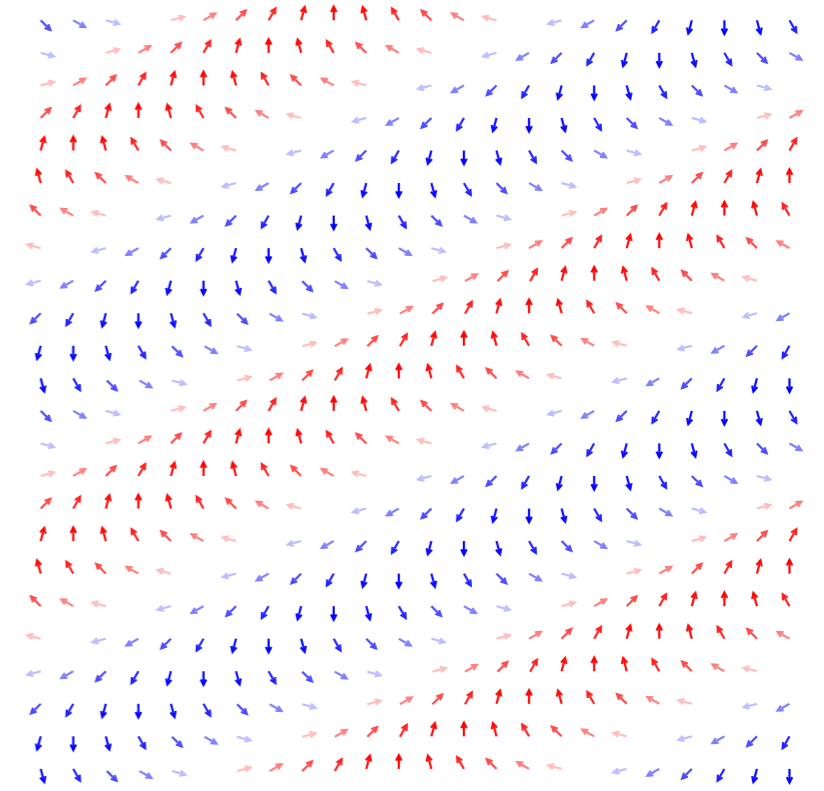
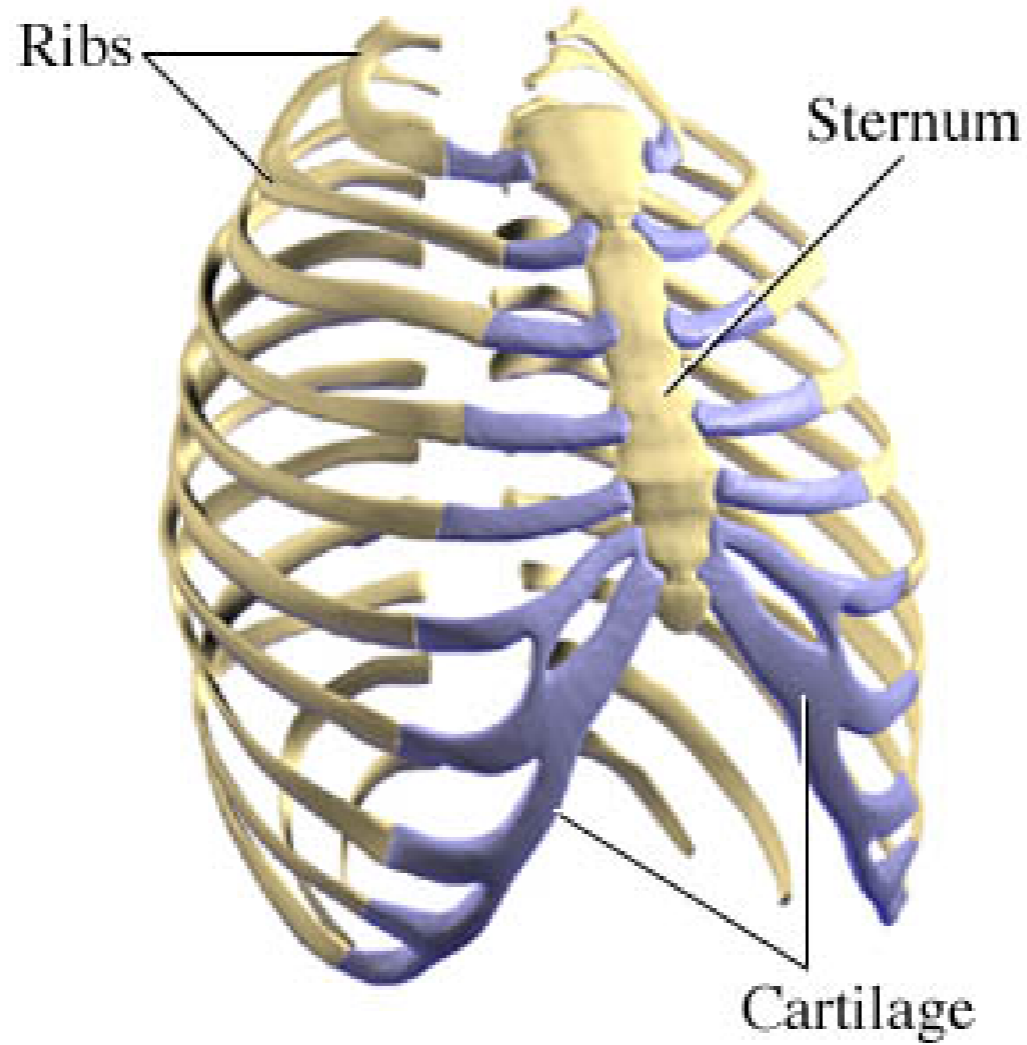
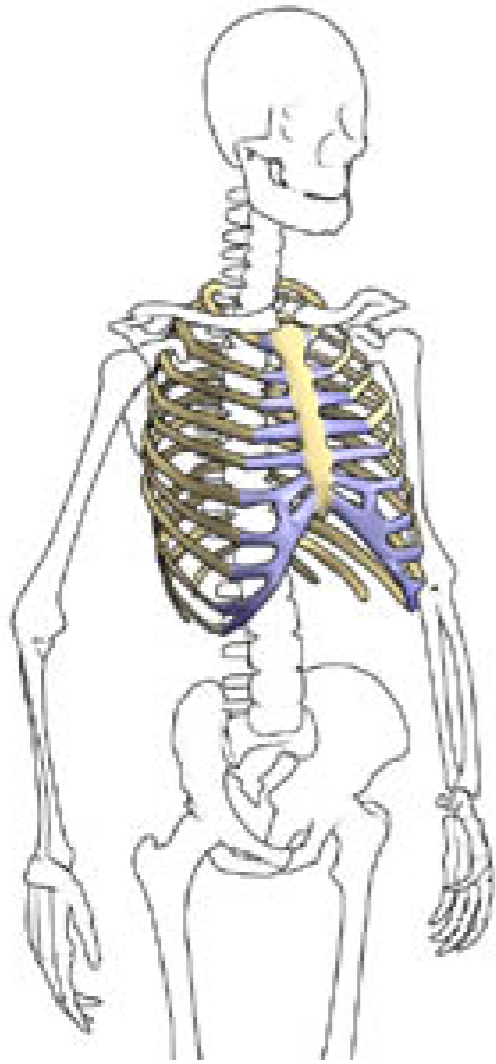
# 3D gradient echo imaging



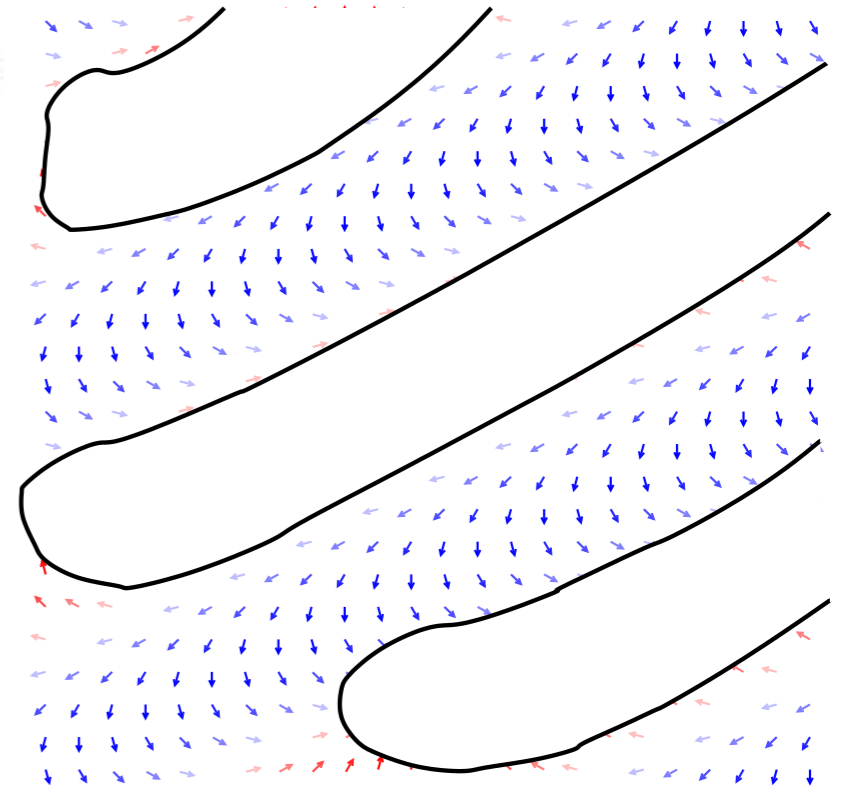
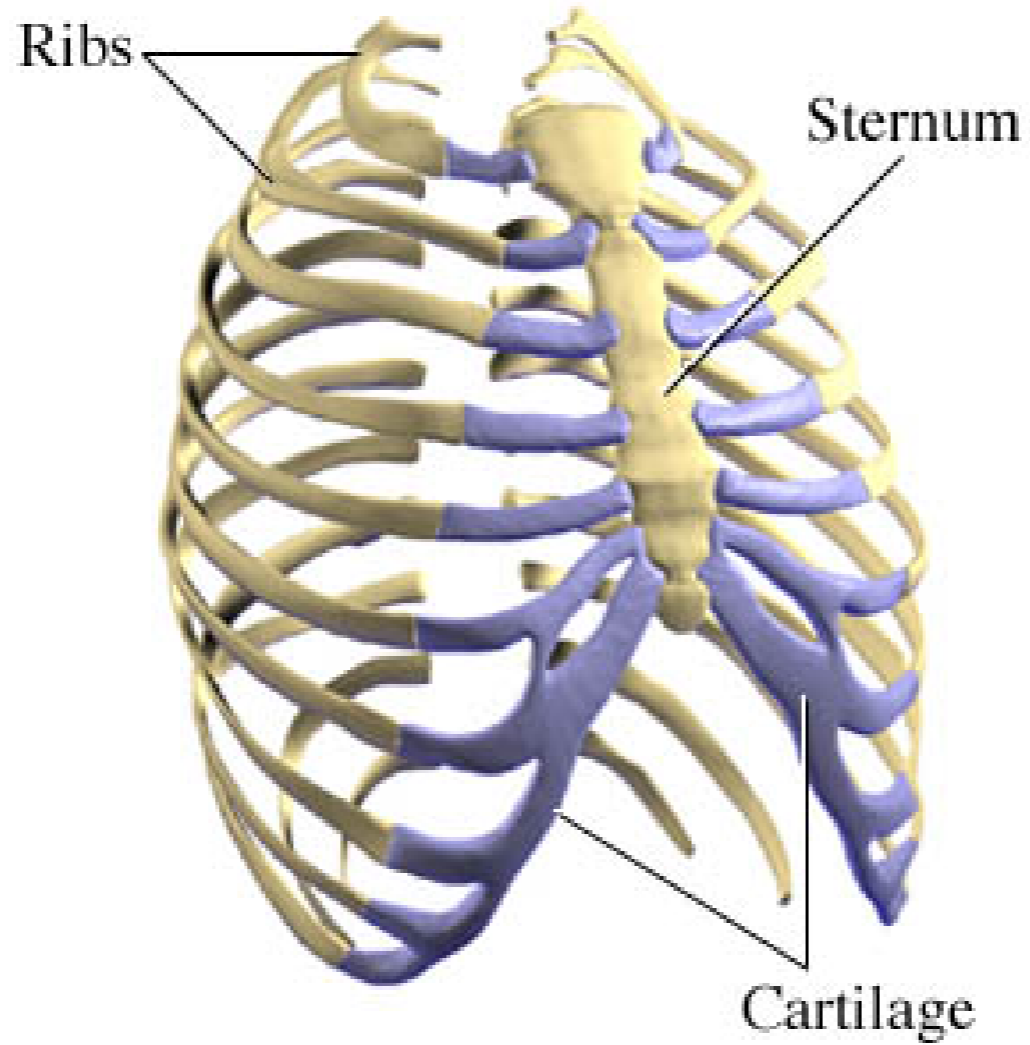
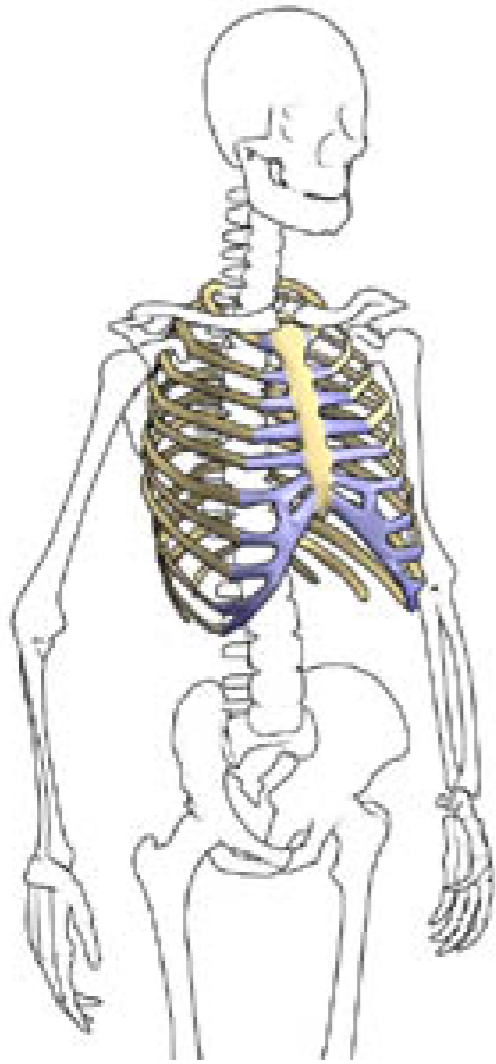
High resolution in all dimensions

More time consuming

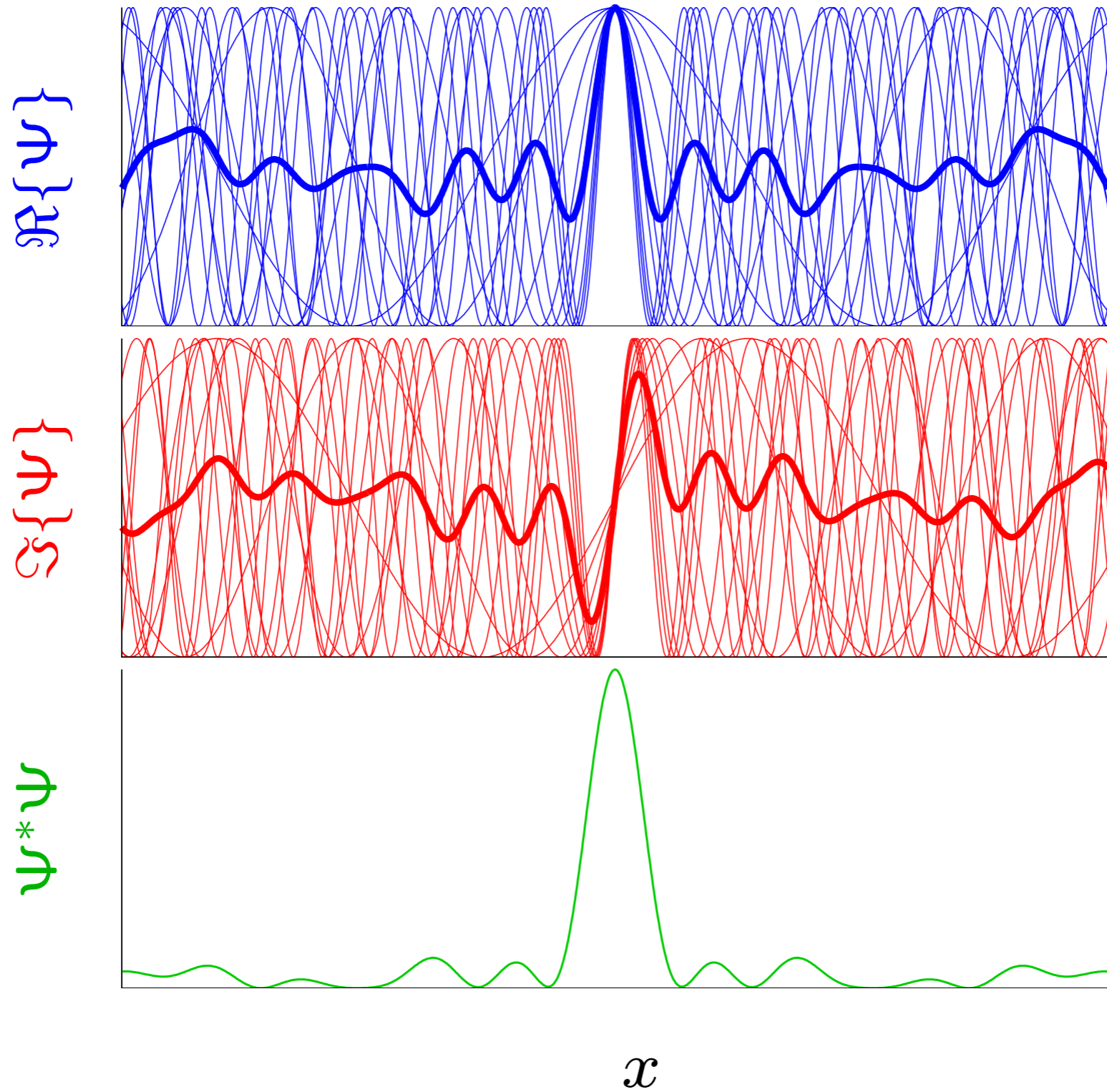
# Regular patterns create signal



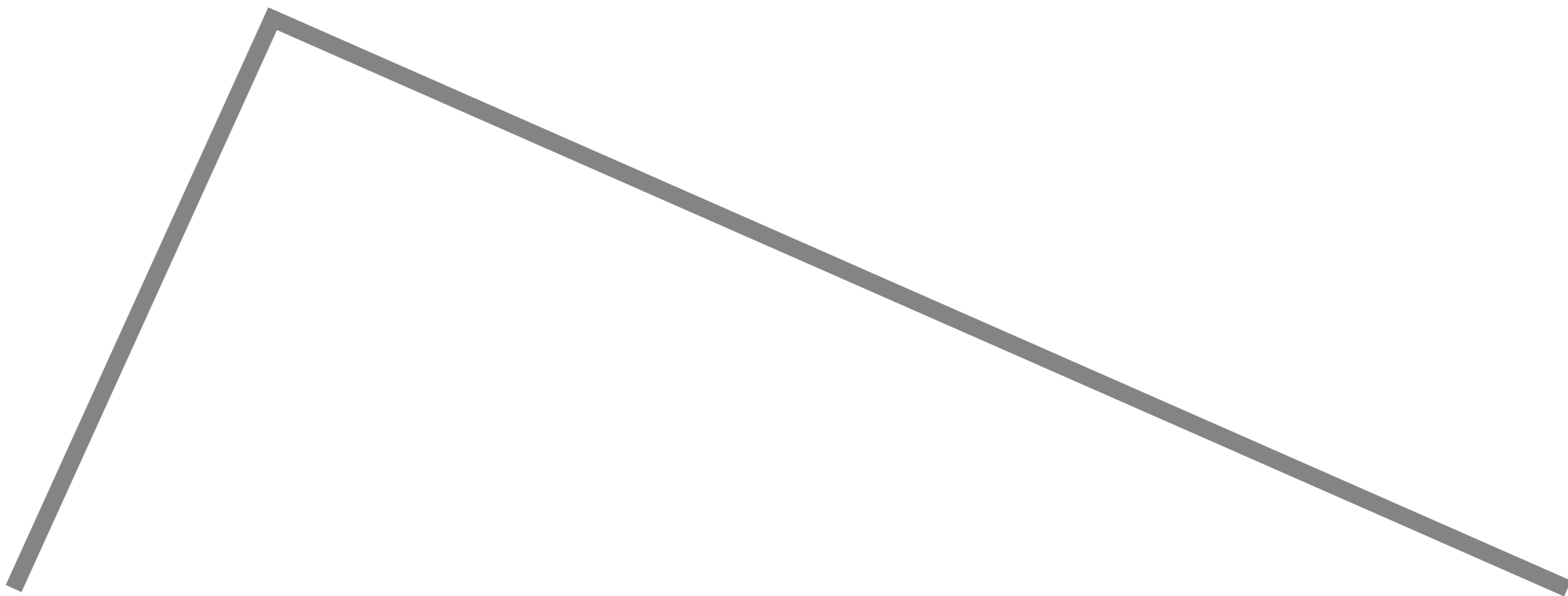
# Regular patterns create signal



# Unique shape as superposition of patterns

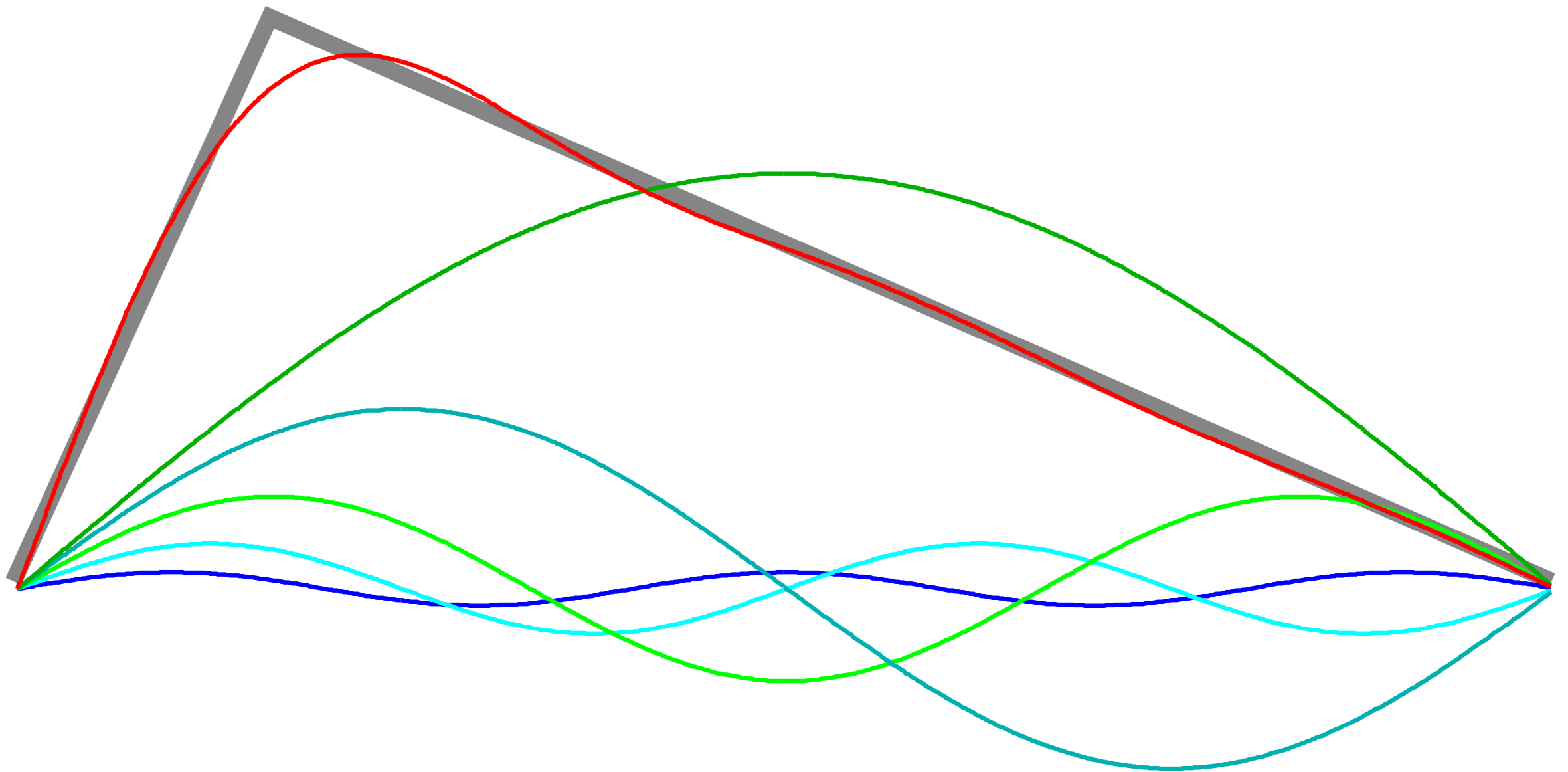


# Unique shape as superposition of patterns

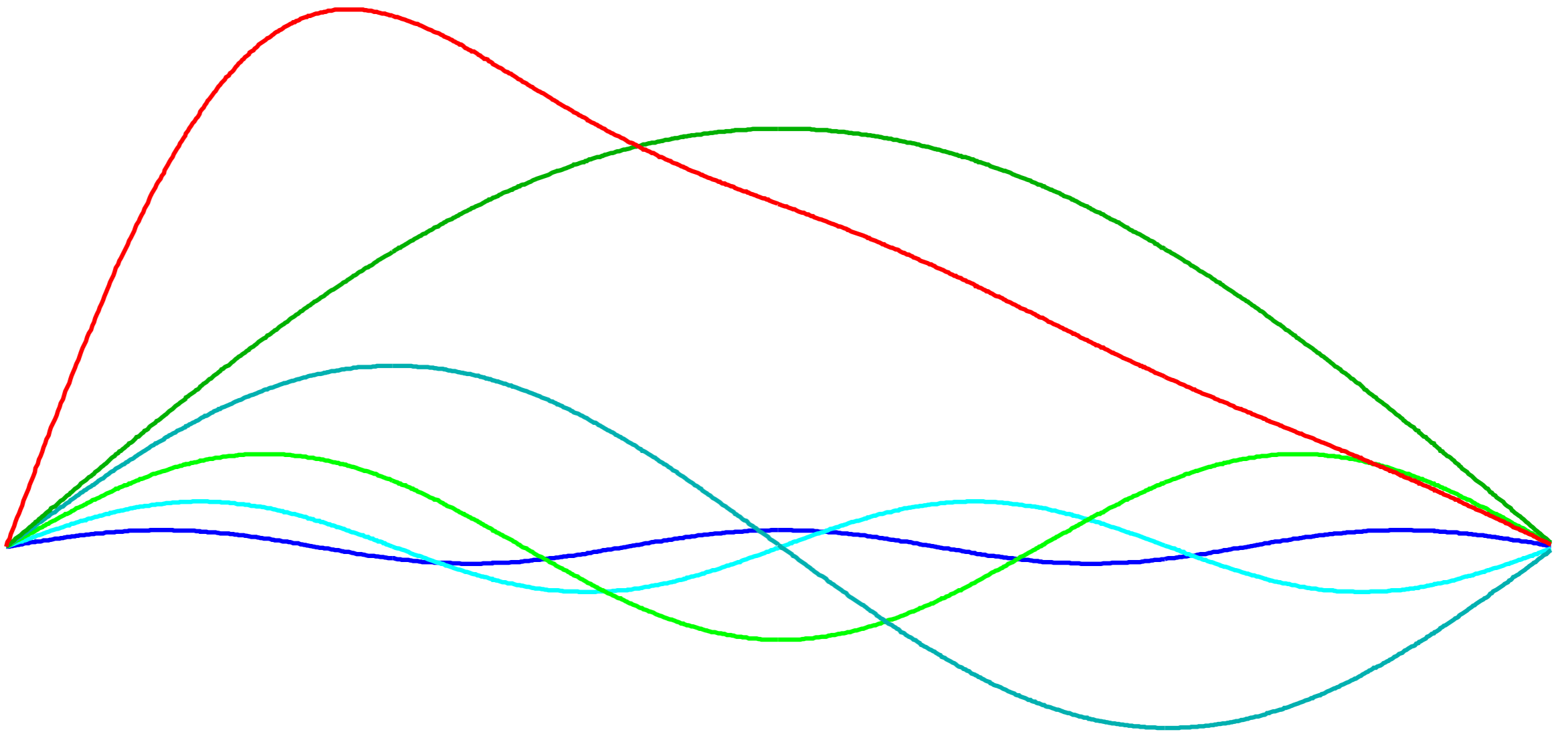




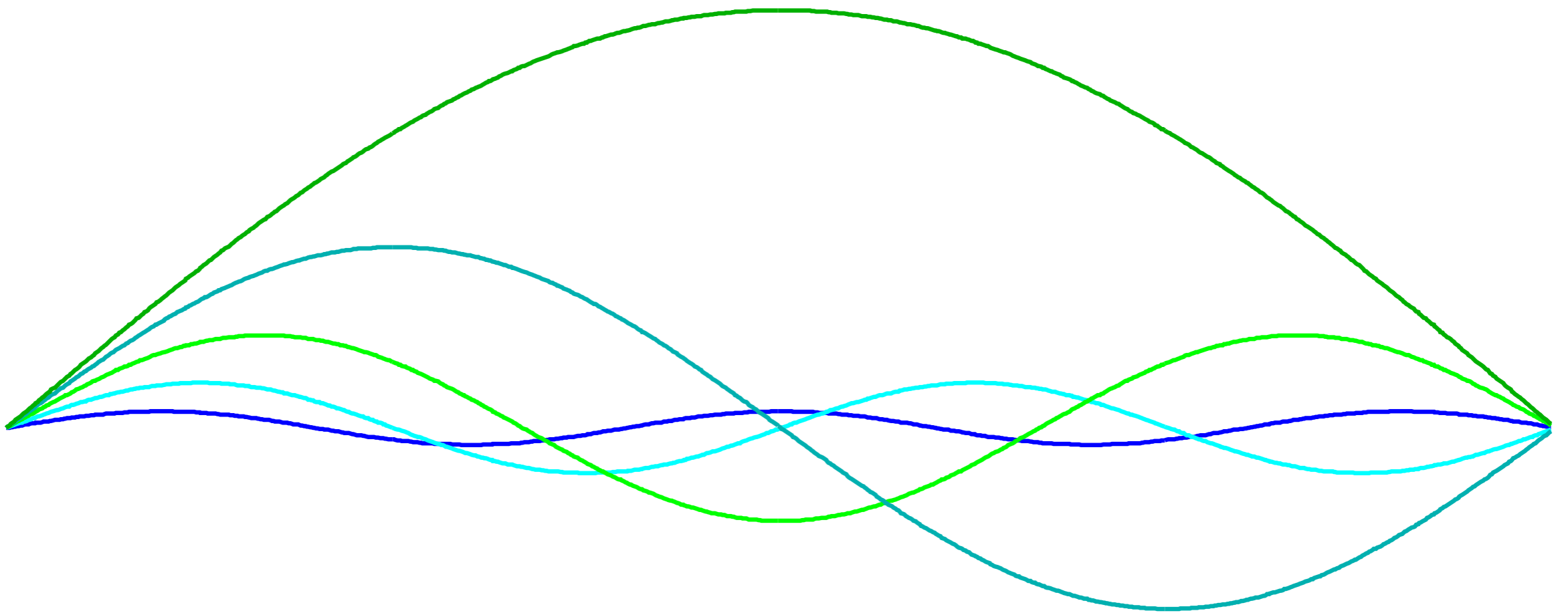
# Unique shape as superposition of patterns



# Unique shape as superposition of patterns



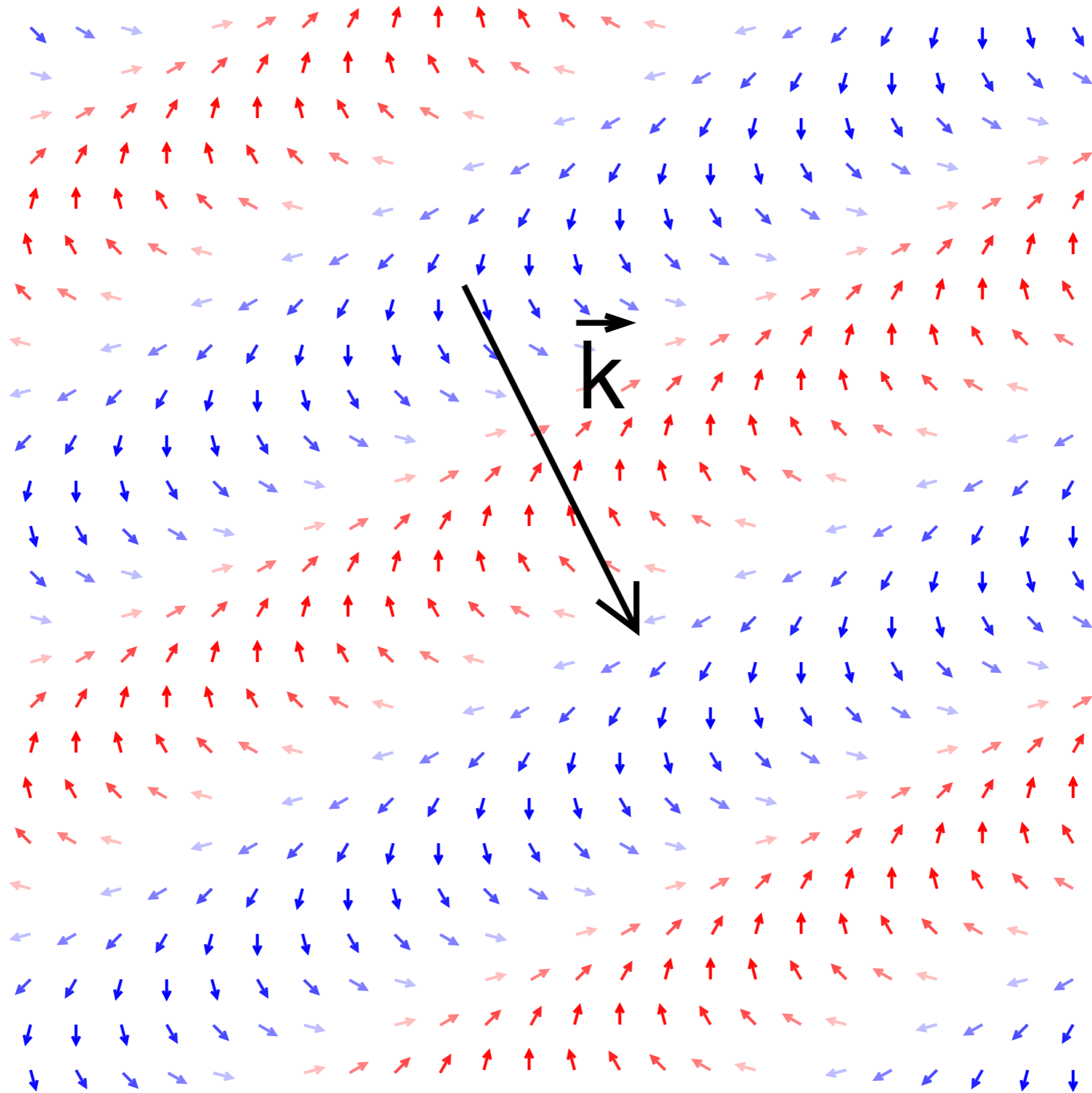
# Unique shape as superposition of patterns



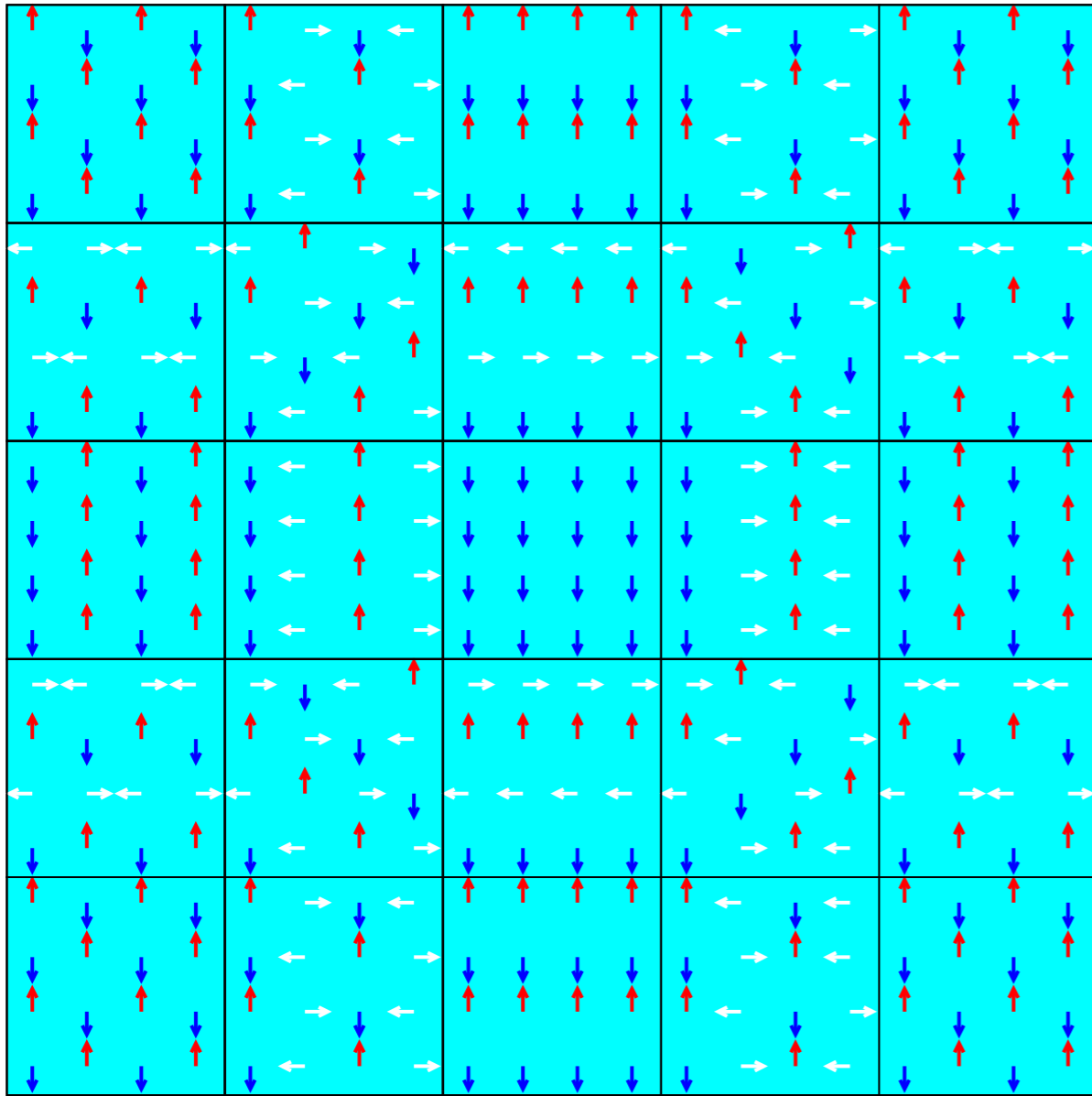
# Image reconstruction

- resembles diffraction methods (crystallography)
- wavelength of the phase patterns generated by gradients
- wavelength of the radio waves is irrelevant (but starts to interfere at high field, where it approaches the body dimensions)
- $\Omega$  assumed to be identical  
differences must be corrected to avoid artifacts

$k$  space

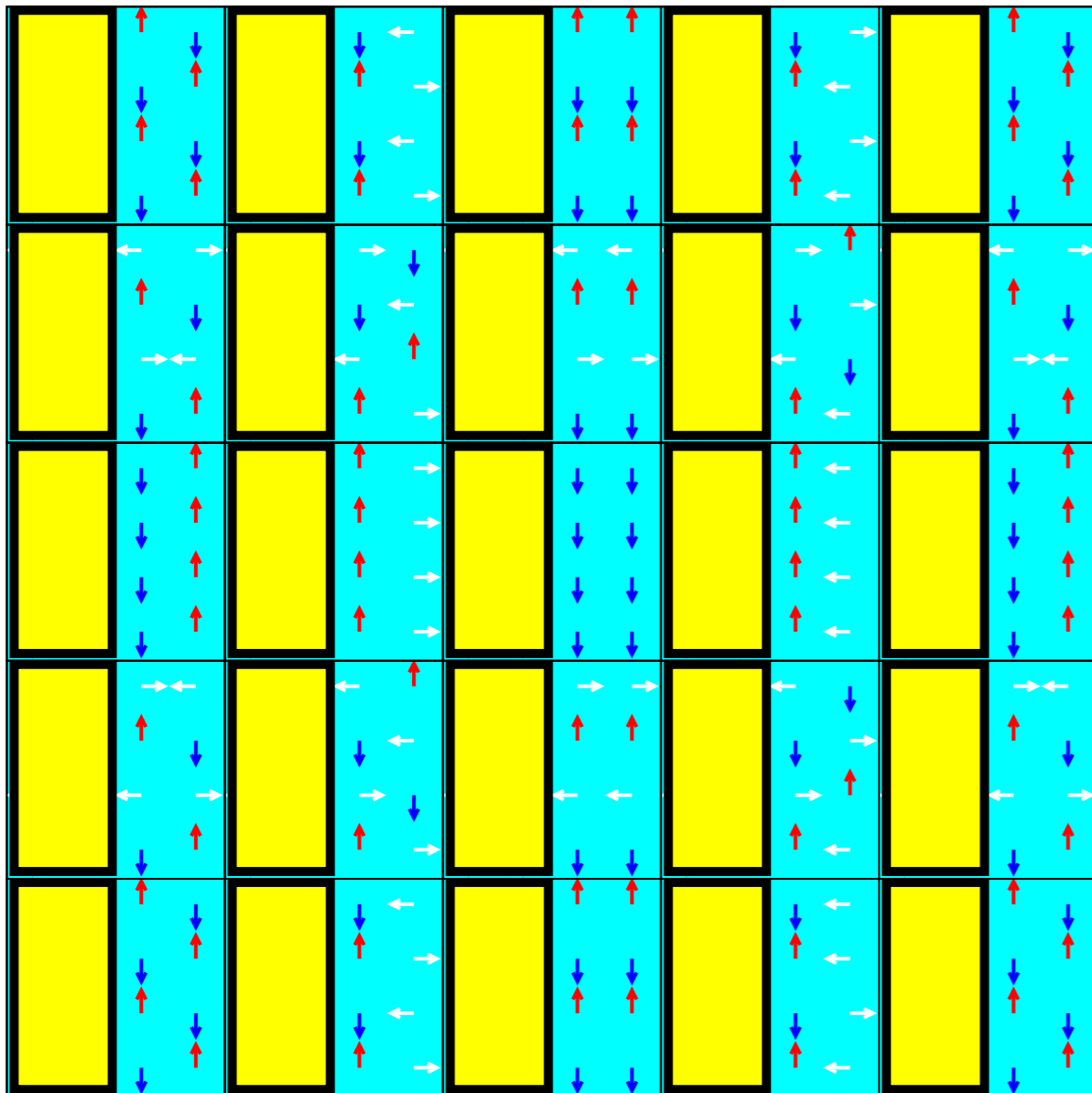


$k$  space



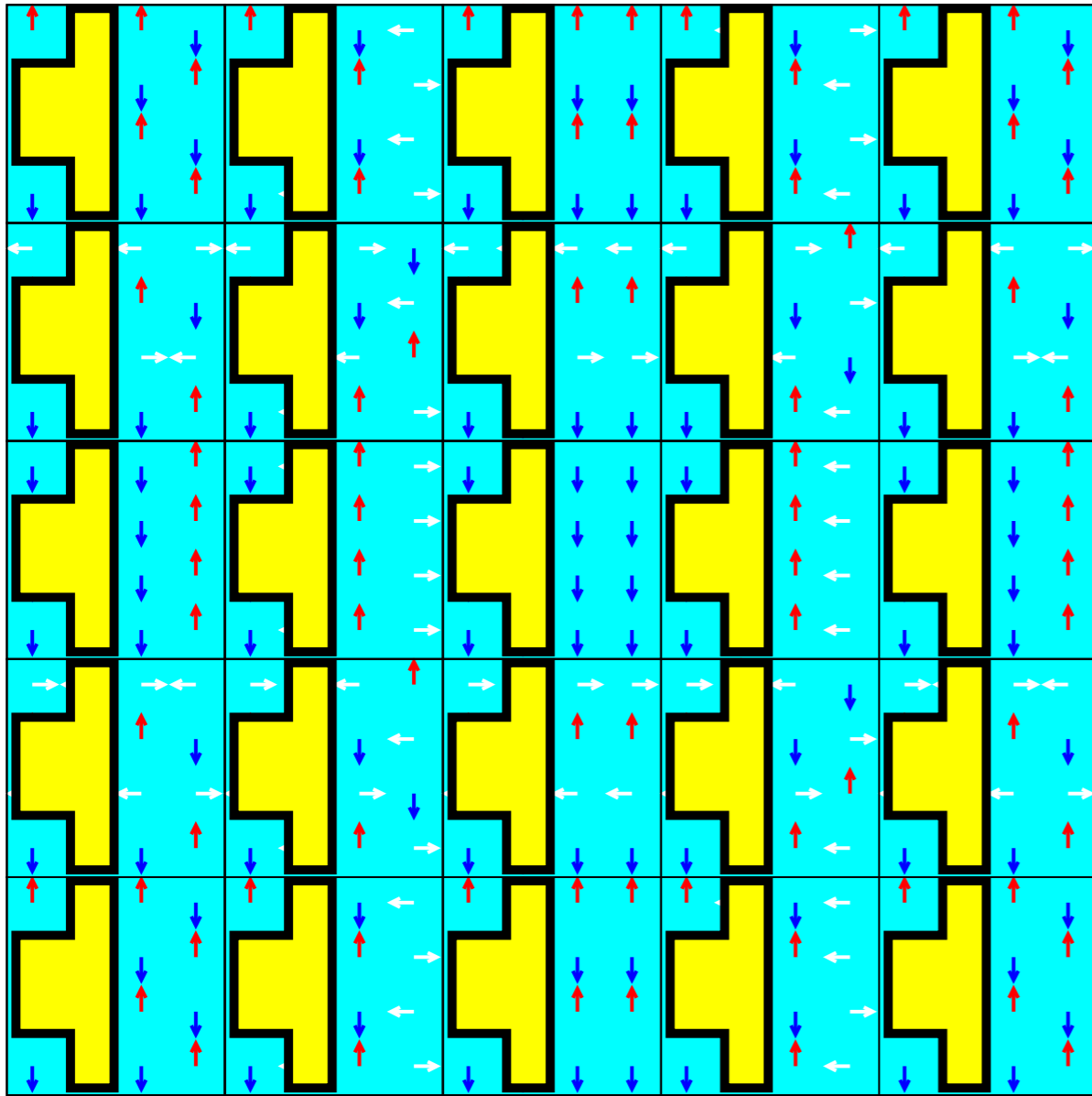
0	0	0	0	0
0	0	0	0	0
0	0	16	0	0
0	0	0	0	0
0	0	0	0	0

$k$  space



0	0	0	0	0
0	0	0	0	0
0	-4	8	-4	0
0	0	0	0	0
0	0	0	0	0

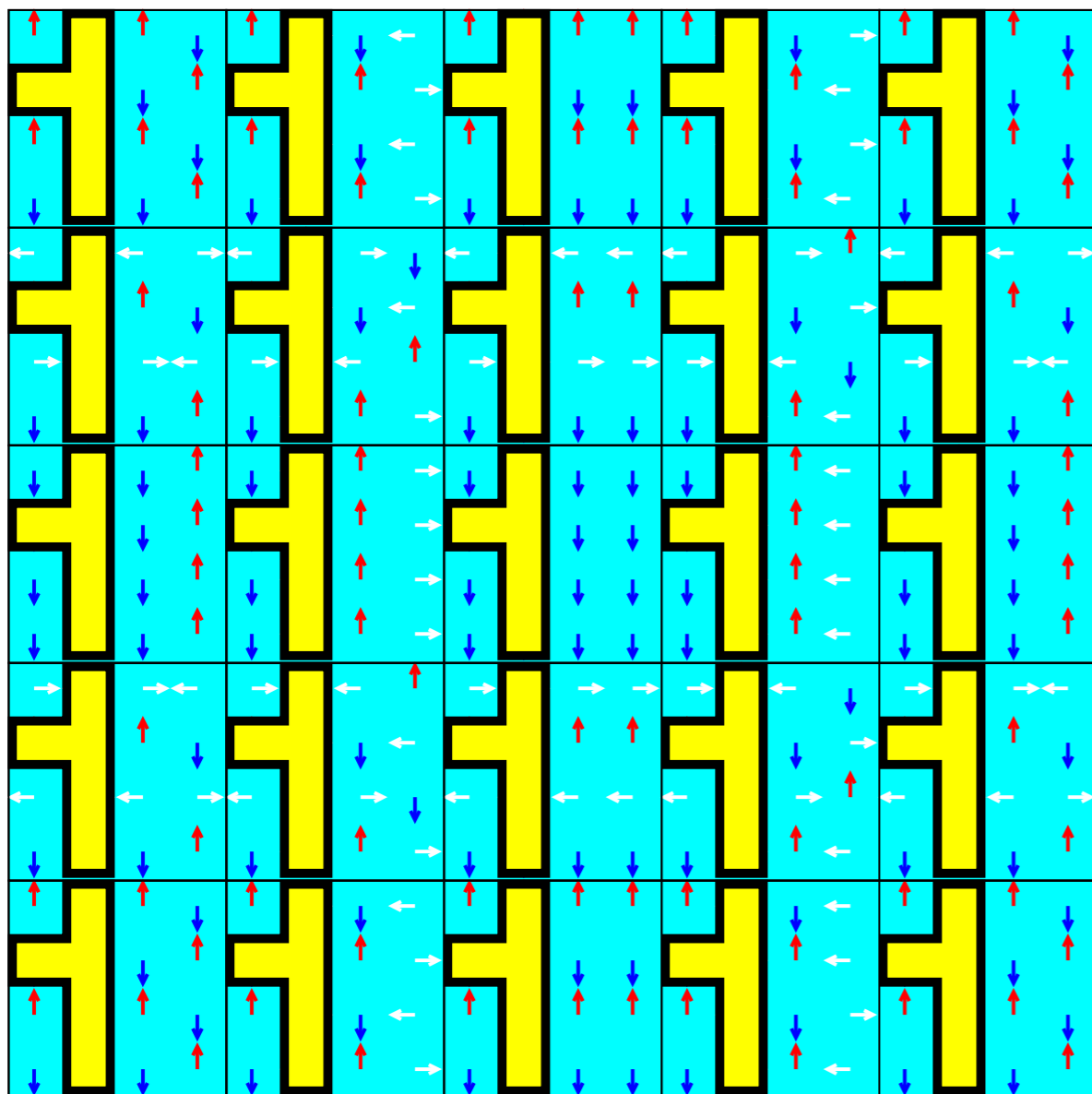
$k$  space



0	0	0	0	0
+1	+1	+1	+1	+1
+2	-2	10	-2	+2
+1	+1	+1	+1	+1
0	0	0	0	0



$k$  space



-1	-1	-1	-1	-1
+1	+1	+1	+1	+1
+3	-1	<b>11</b>	-1	+3
+1	+1	+1	+1	+1
-1	-1	-1	-1	-1

**See Figure 15 in**

[https://eprints.drcmr.dk/37/1/MRI\\_English\\_a4.pdf](https://eprints.drcmr.dk/37/1/MRI_English_a4.pdf)

